

EKG Übungen: ventrikuläre Arrhythmien

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Introduction

Use of the 12-lead ECG recorded during VT to regionalize its origin was first described by Josephson in 1981. ¹

Seven years later, reported by the same group of investigators, proved that the origin of the VT exit site could be accurately identified based on an analysis of the 12-lead ECG. ²

the 4 investigators pinpointed the 182 VTs to 1 of 10 approximately equal specific anatomic regions of the LV and demonstrated a remarkable 93% site concordance in site designation for all 4 investigators. ²

1. Josephson ME, Horowitz LN, Waxman HL, Spielman SR, Greenspan AM, Cain ME, Marchlinski FE, Ezri MD. Sustained ventricular tachycardia: role of the 12-lead electrocardiogram in localizing site of origin. *Circulation* 1981;64:257–272.

2. Miller JM, Marchlinski FE, Buxton AE, Josephson ME. Relationship between the 12-lead electrocardiogram during ventricular tachycardia and endocardial site of origin in patients with coronary artery disease. *Circulation* 1988;77:759–766.

Introduction

It should be emphasized that the spatial resolution of the 12-lead ECG is limited, and similar 12-lead QRS complexes can be obtained during pacing at sites up to 5 cm apart with similar ECG patterns confirmed over $> 8 \text{ cm}^2$ during pace-mapping in at least 10% of VTs.

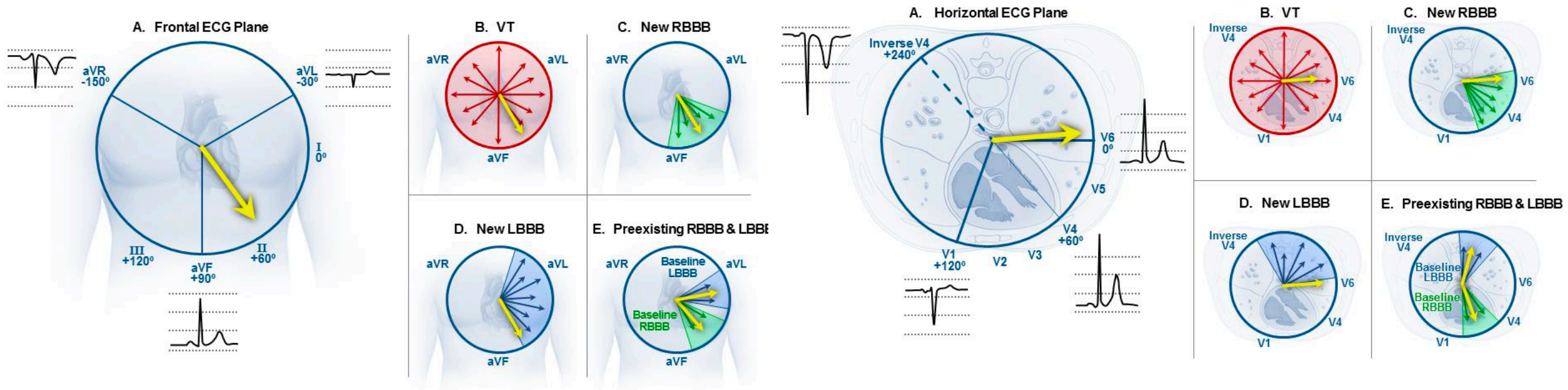
Given that the LV has an end-diastolic area of about $80\text{--}100 \text{ cm}^2$, it makes more sense to divide it into no more than 10–12 approximately equal segments when localizing a region of interest using the 12-lead ECG of the VT to limit overlapping information

Gopal AS, Keller AM, Rigling R, King DL, King DL. Left ventricular volume and endocardial surface area by three-dimensional echocardiography: comparison with two-dimensional echocardiography and nuclear magnetic resonance imaging. J Am Coll Cardiol 1993;22:258–270.

ECG features

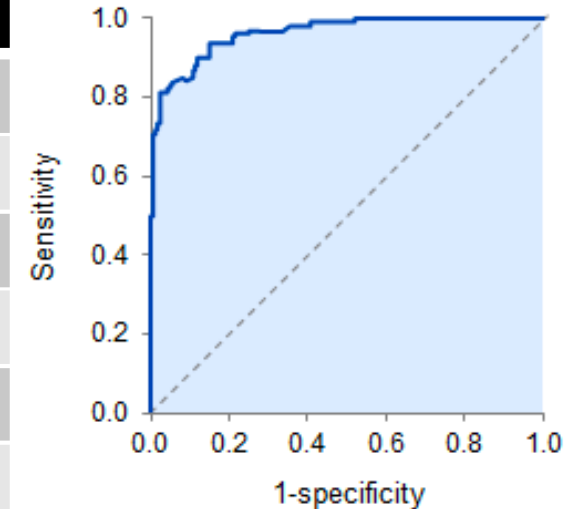
... significant variation may result from several factors, such as body habitus, lead placement and shifts in the relationship of the heart to the chest wall.

WCT formula: A novel algorithm designed to automatically differentiate wide-complex tachycardias



WCT formula: A novel algorithm designed to automatically differentiate wide-complex tachycardias

	SWCT (n = 160)	VT (n = 157)	P value
Baseline QRS duration (ms)	135.9 (28.1)	147.5 (44.0)	0.03
Baseline QTc duration (ms)	483.2 (43.4)	500.4 (63.2)	0.07
WCT QRS duration (ms)	144.4 (18.1)	177.1 (32.4)	< 0.001
QRS duration change (ms)	18.1 (22.4)	45.1 (34.3)	< 0.001
QRS axis change (°)	24.9 (32.6)	82.2 (56.7)	< 0.001
Frontal PAC (%)	34.9 (28.2)	124.2 (87.1)	< 0.001
Horizontal PAC (%)	44.8 (25.2)	115.3 (62.9)	< 0.001



AOC: 96.6%

Patient:

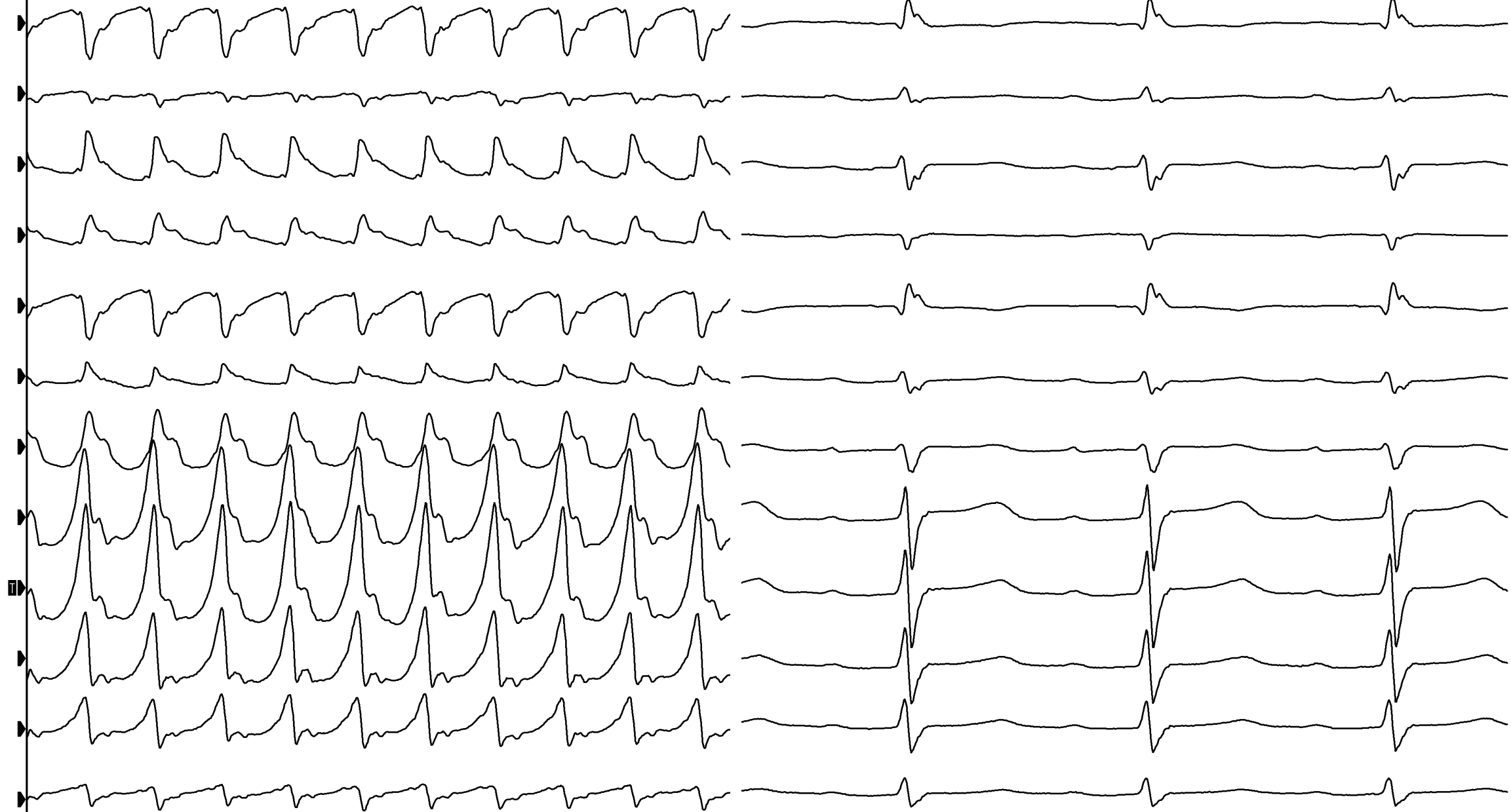
79y ♂

Palpitation

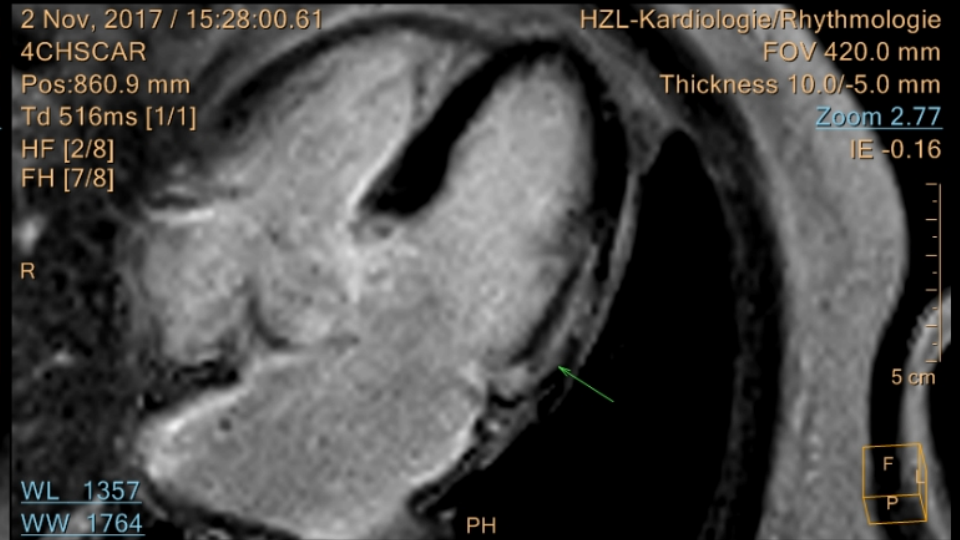
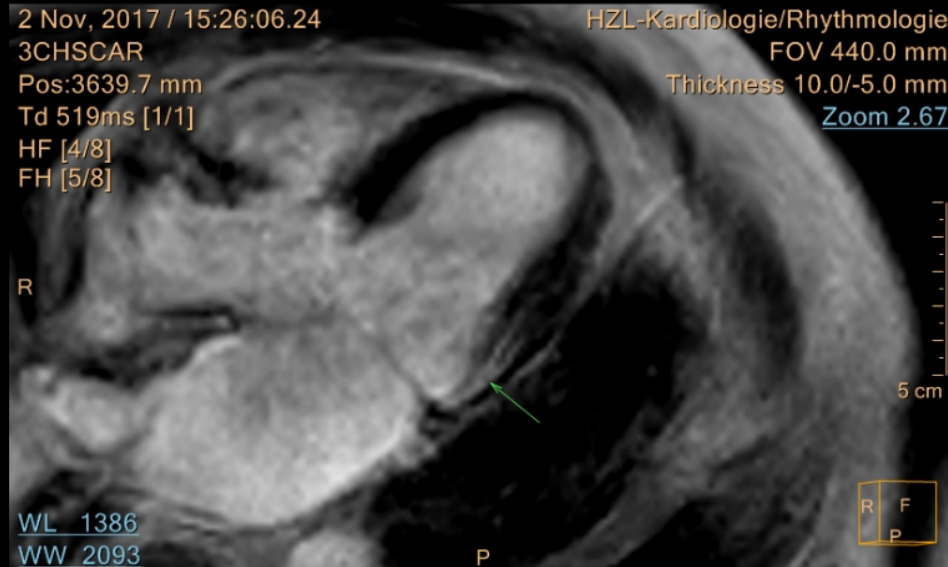
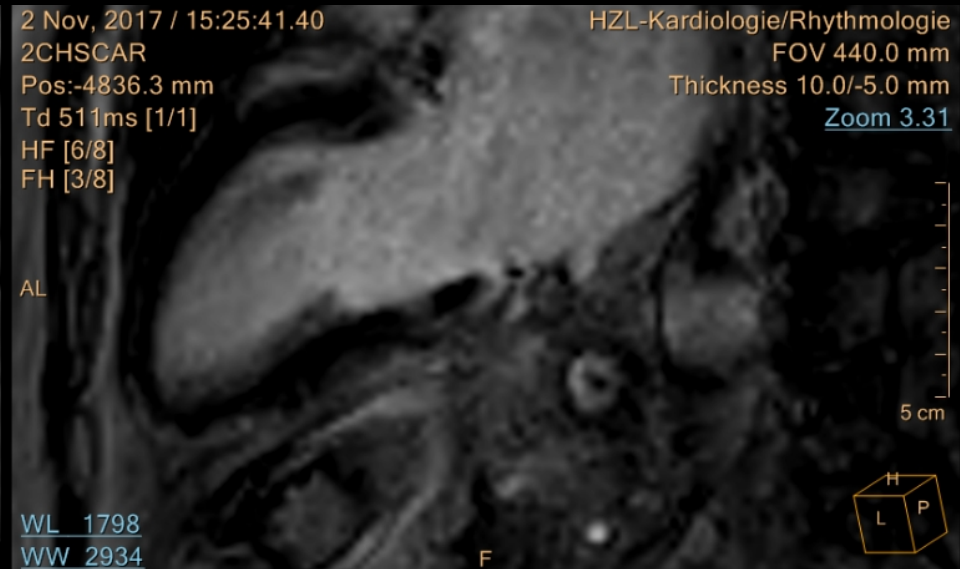
LVEF: 63%, no WMA,

CA: Normal.

CL: 250 ms



08:17:38 08:17:39 08:17:40 07:57:32 07:57:33 07:57:34

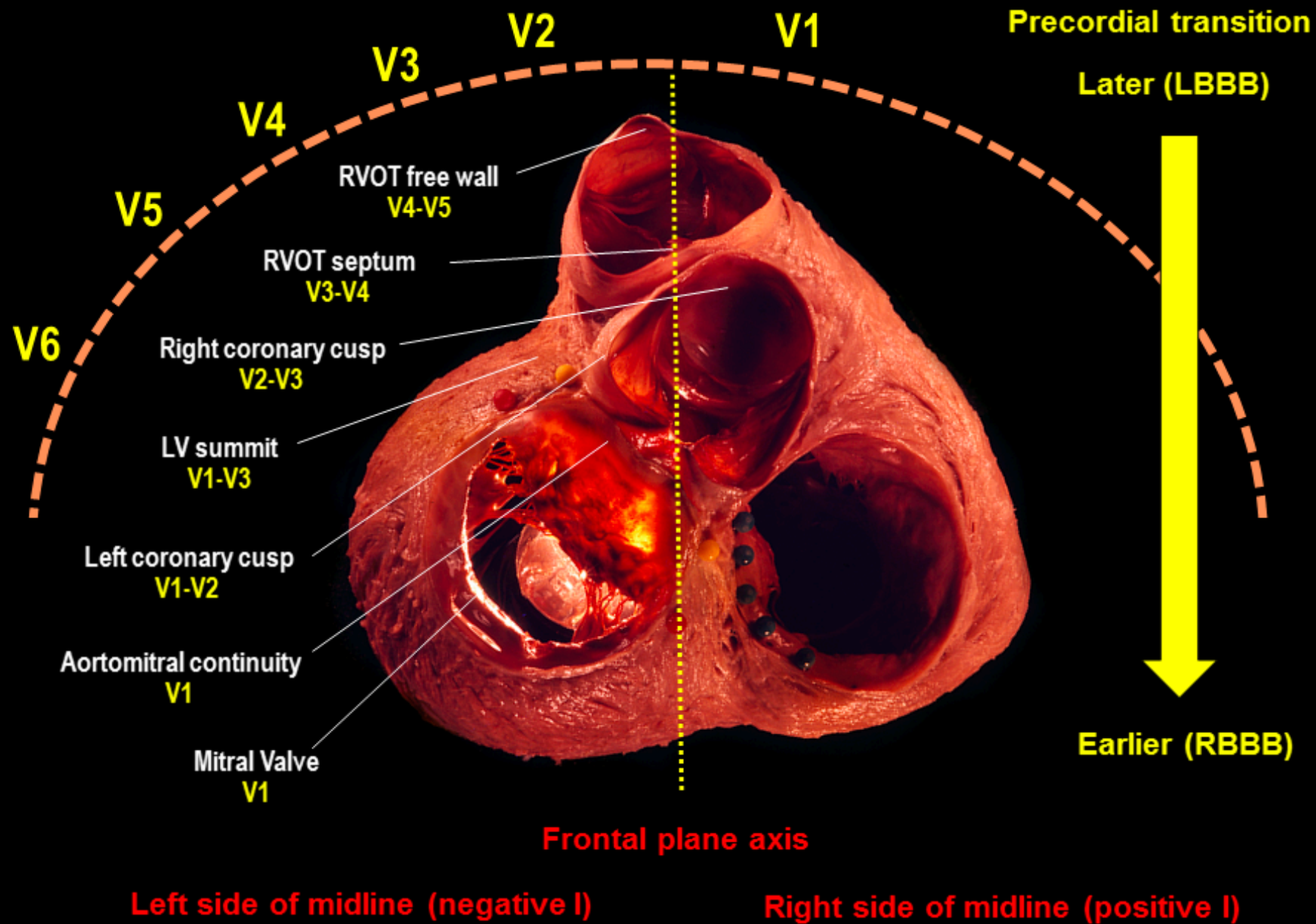


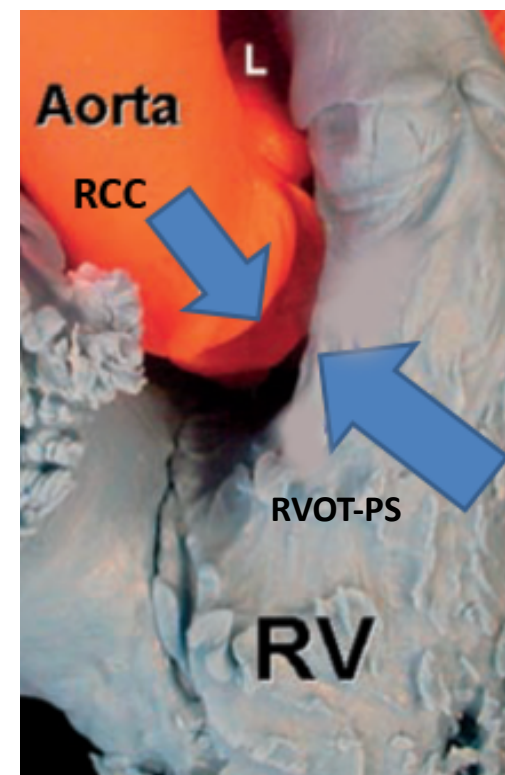
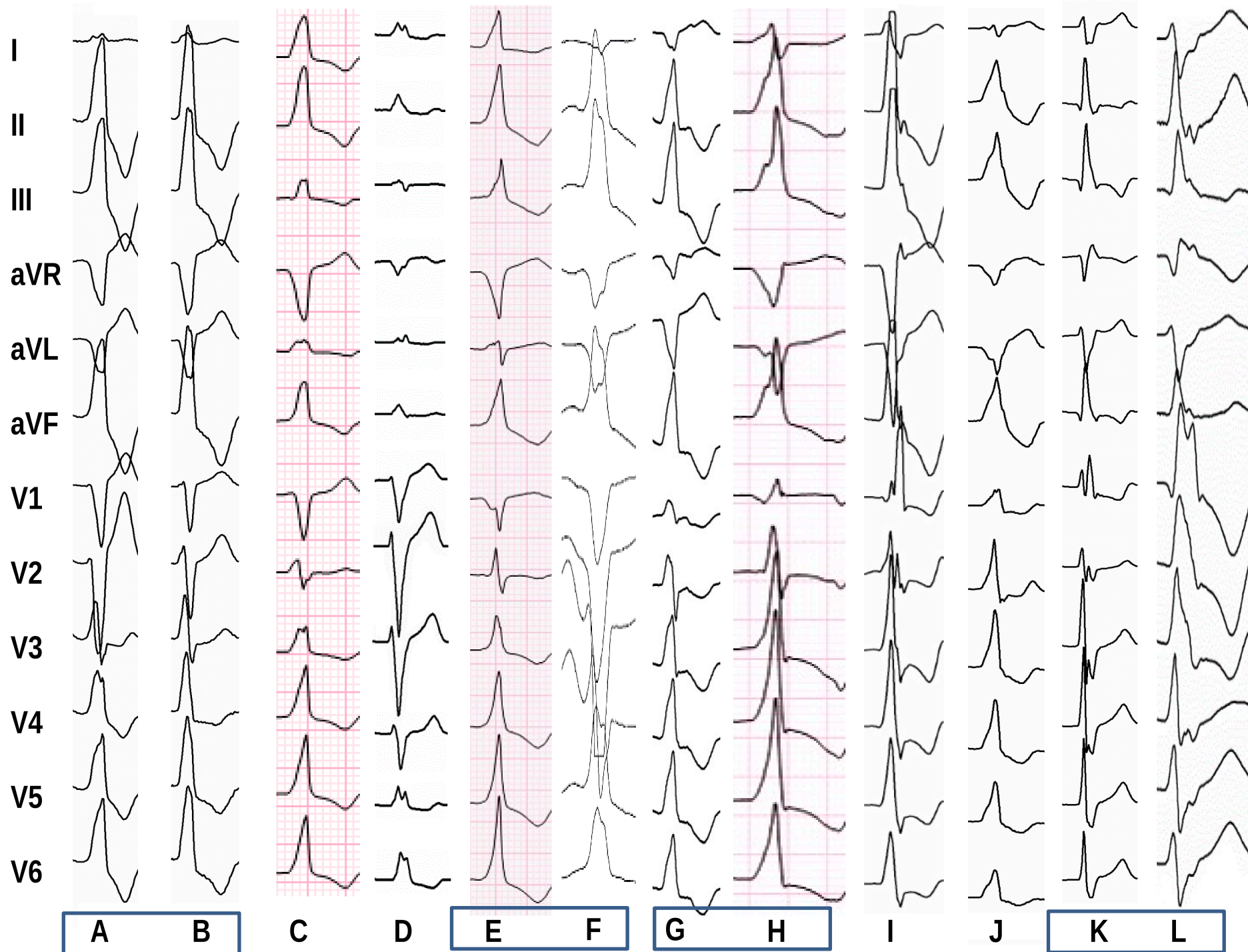
MRT 02.11.2017

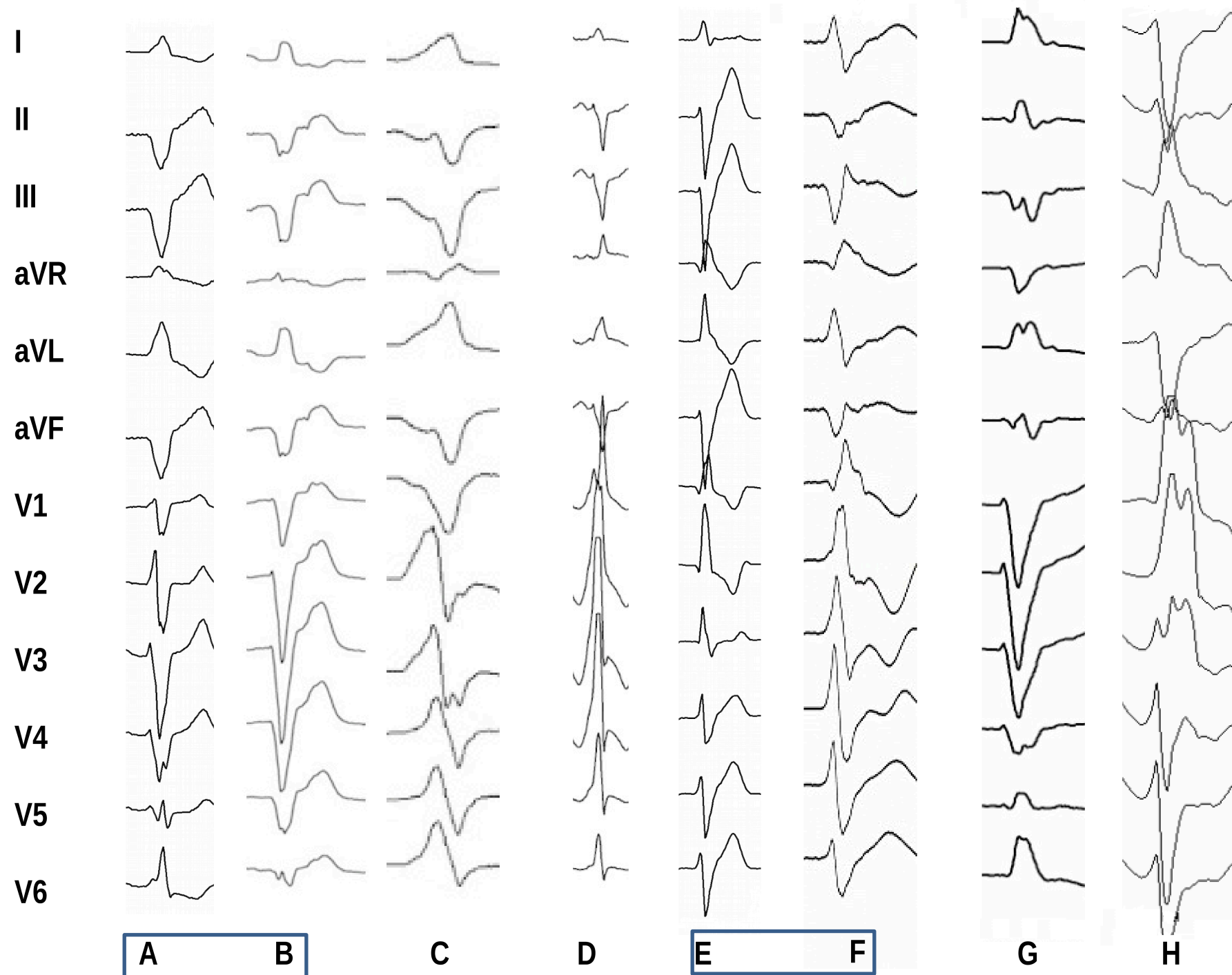
ECG features

Several ECG features are relevant for localization of a particular VA. The most important are:

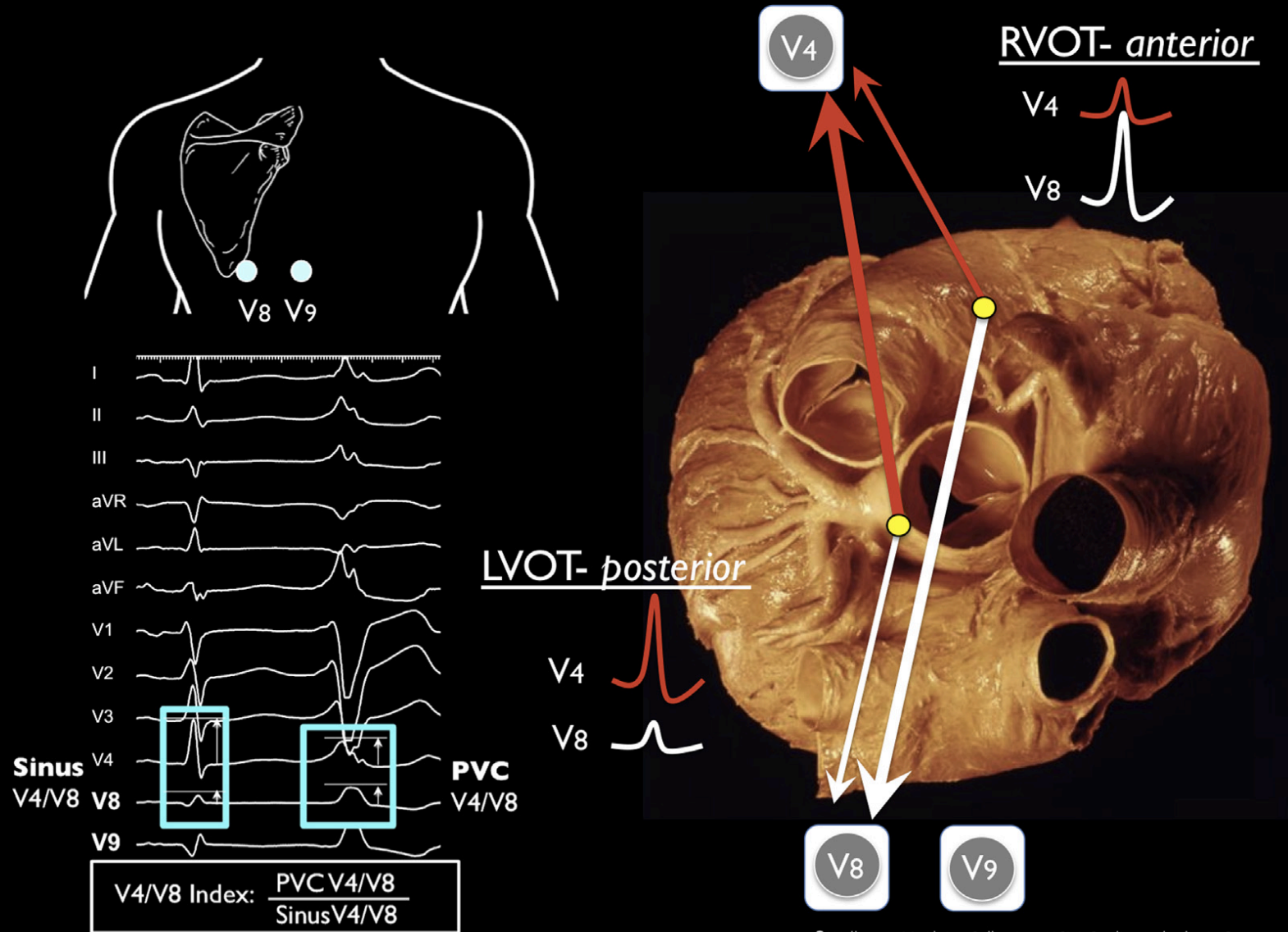
- (1) QRS axis (both a vertical (superior-inferior) and horizontal (right-left))
- (2) Bundle branch block pattern
- (3) Precordial transition
- (4) QRS width







Value of Posterior ECG Leads



©Wallace A. McAlpine Collection- UCLA Cardiac Arrhythmia Center

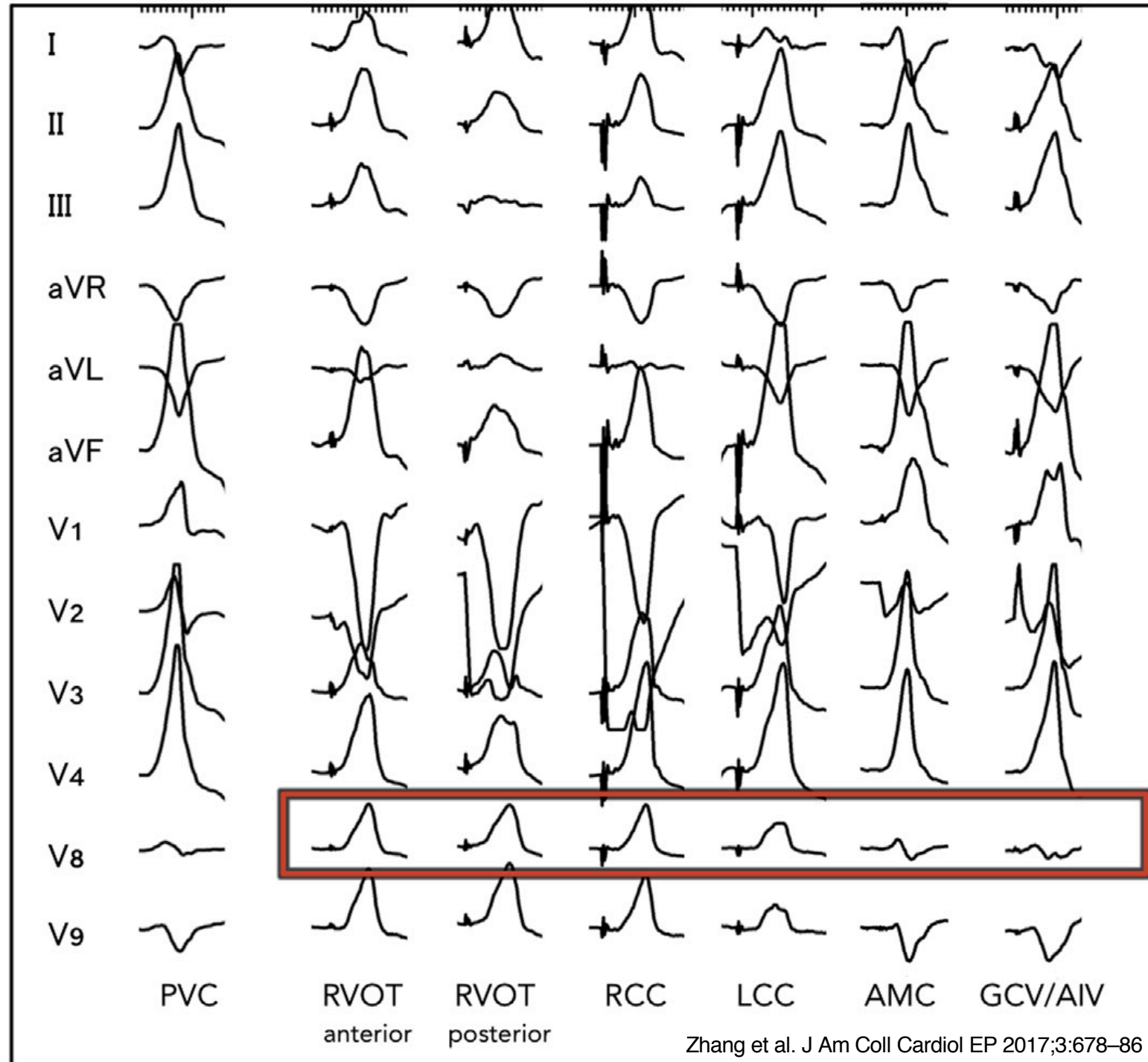
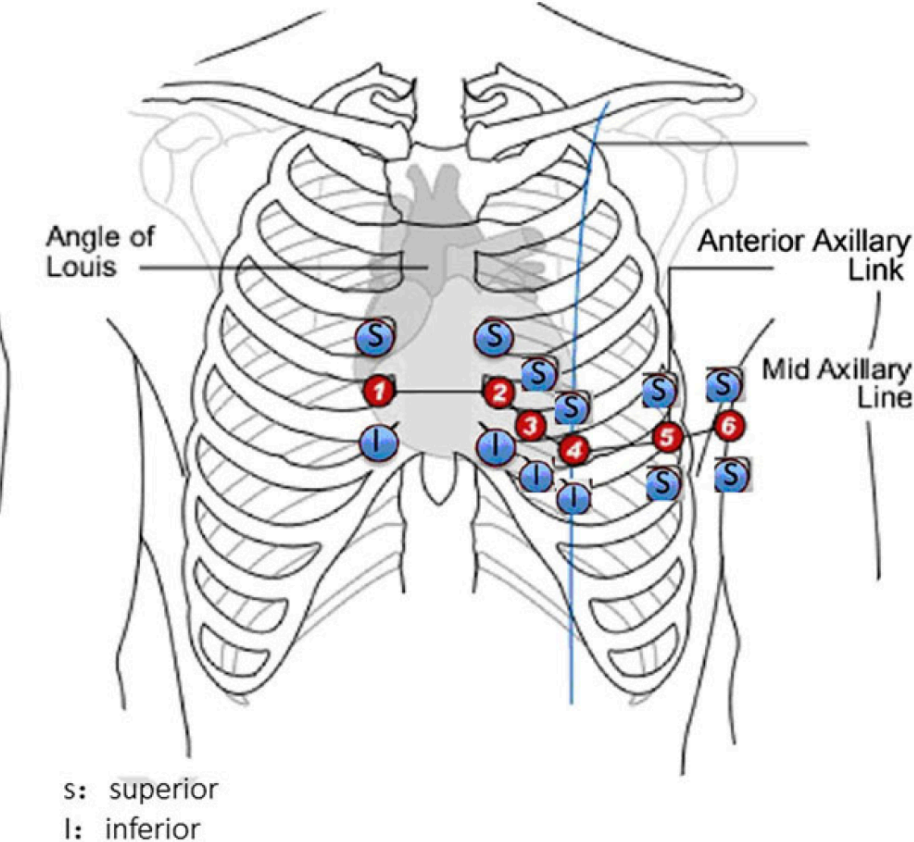


TABLE 3 Test Characteristics

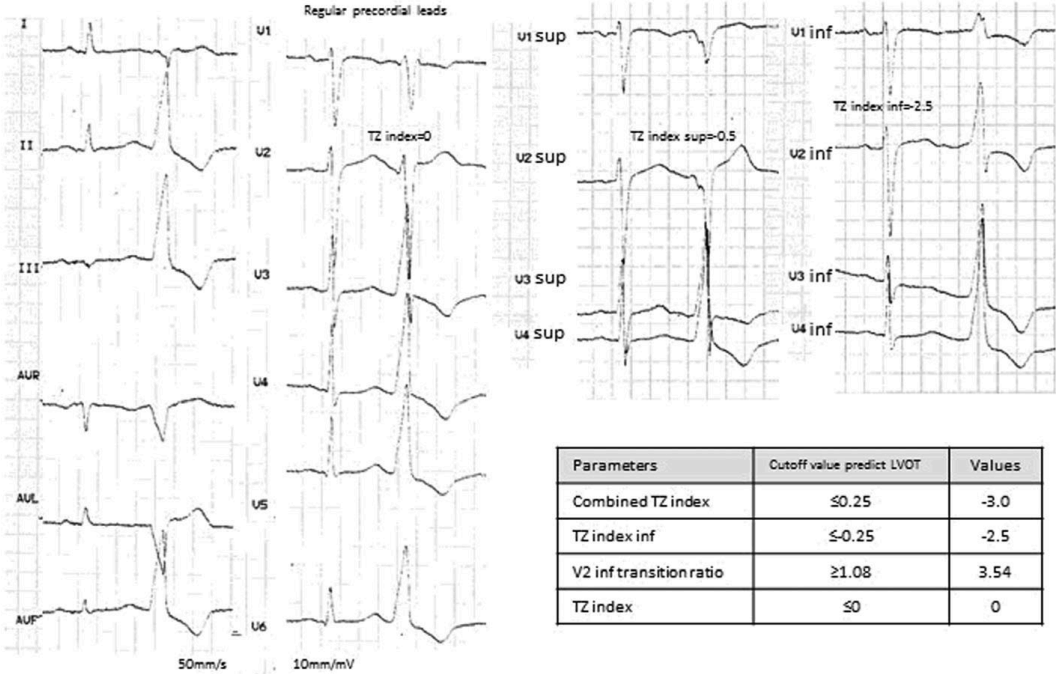
	Sensitivity	Specificity	PPV	NPV
Predictive of left-sided location in the prospective cohort				
V ₄ /V ₈ ratio >3	75	82	64	89
V ₄ /V ₈ index >2.28	67	96	89	87
V ₂ transition ratio ≥0.6	67	67	47	82
V _{2S} /V _{3R} ≤1.5	36	71	33	74
PVC with a V ₃ precordial transition (n = 19)				
V ₄ /V ₈ ratio >3	67	81	57	87
V ₄ /V ₈ index >2.28	67	100	100	87
V ₂ transition ratio ≥0.6	50	54	33	70
V _{2S} /V _{3R} ≤1.5	40	62	29	73
Values are %.				
NPV = negative predictive value; PPP = positive predictive value.				
Zhang et al. J Am Coll Cardiol EP 2017;3:678–86				

Multiple Intercostal Space Electrocardiogram Allows Accurate Localization of Outflow Tract Ventricular Arrhythmia Origin

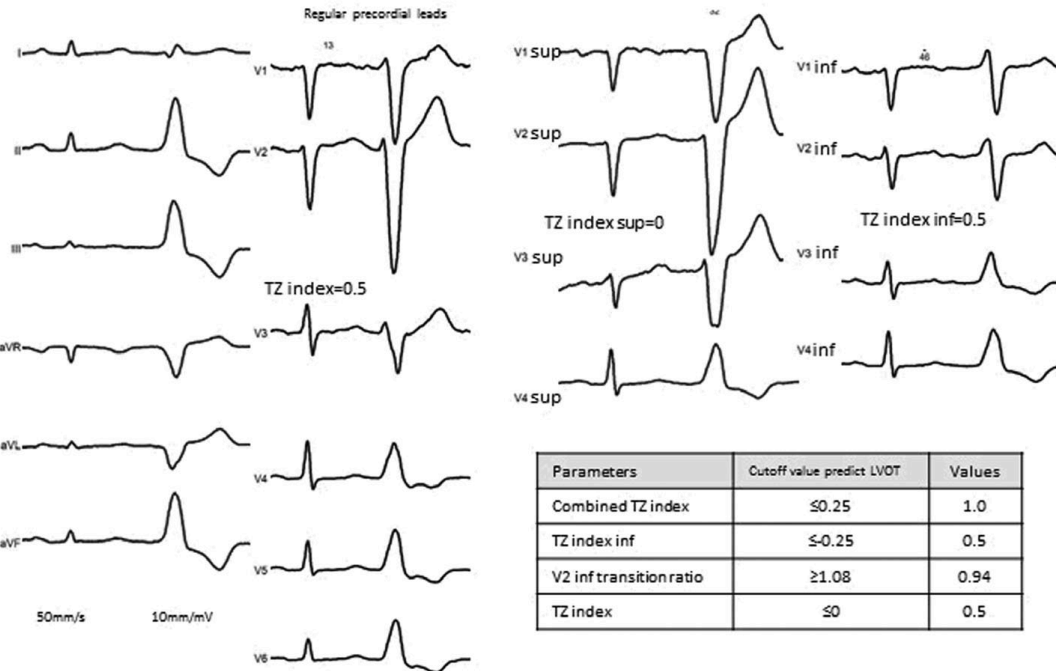


The combined TZ index outperformed other ECG criteria to differentiate left from right OT-VA origins.

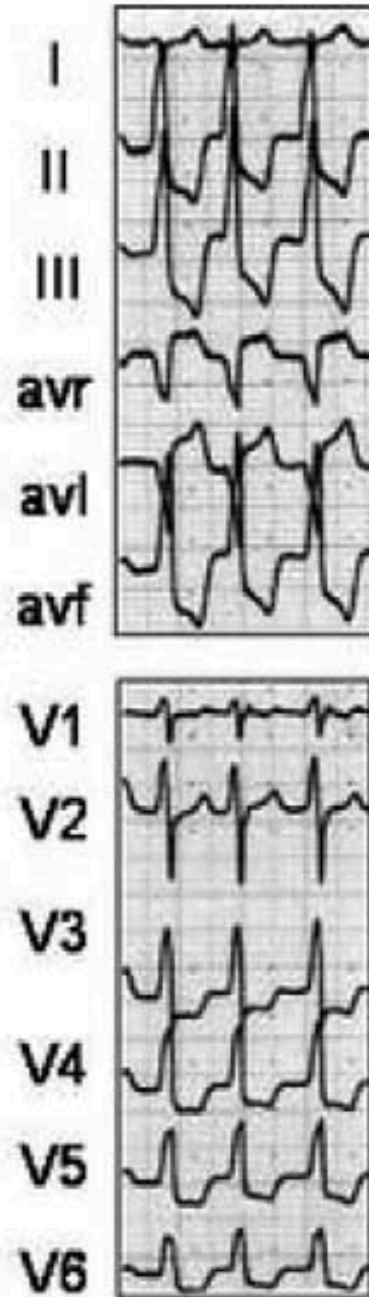
Aortic coronary cusp



RVOT



LVOT ↑
RVOT ↓



R/S transition V2/V3:

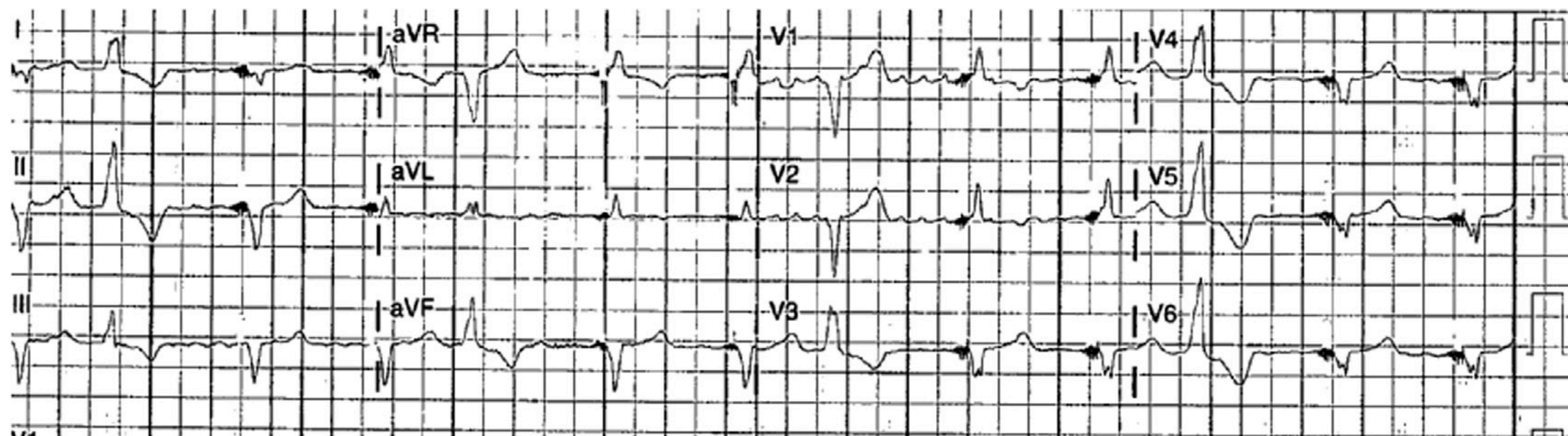
$V2R/V2S > 0.3$

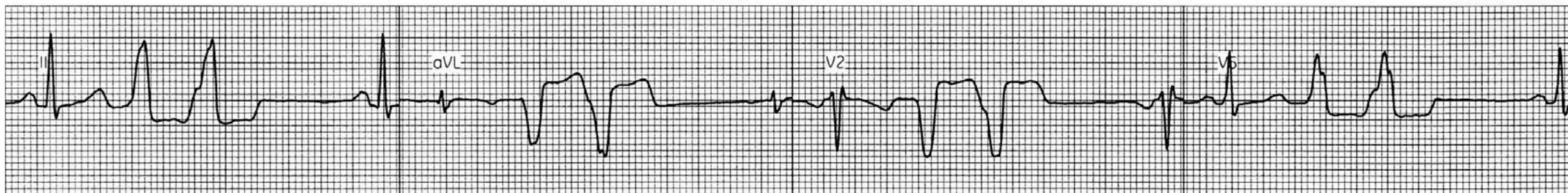
$V2R_{ms}/V2_{ms} > 0.5$

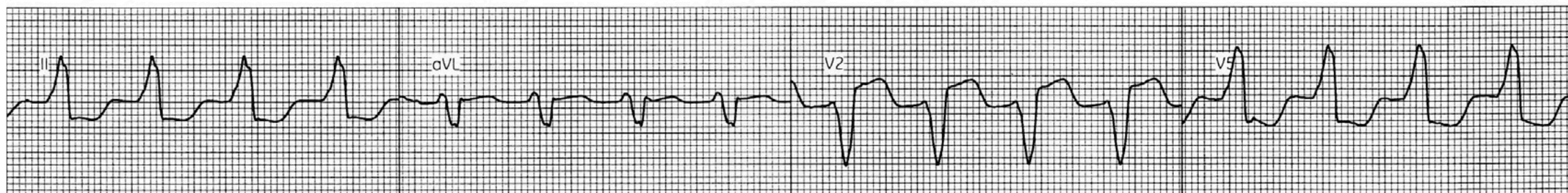
$V2R_{PVC}/V2R_{SR} \geq 0.6$

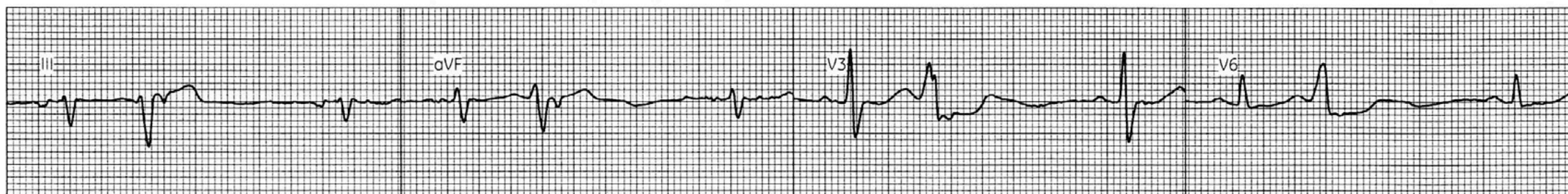
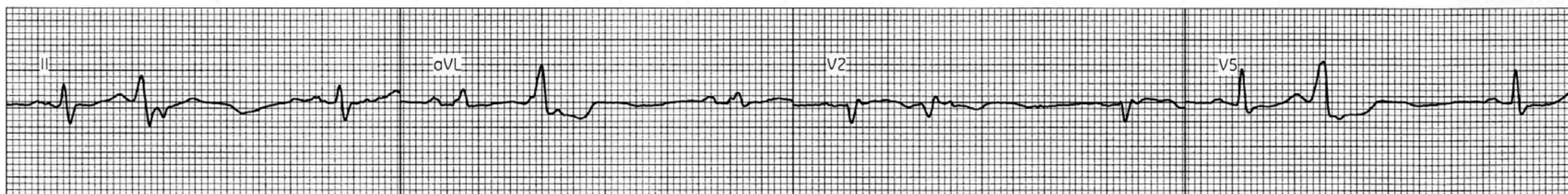
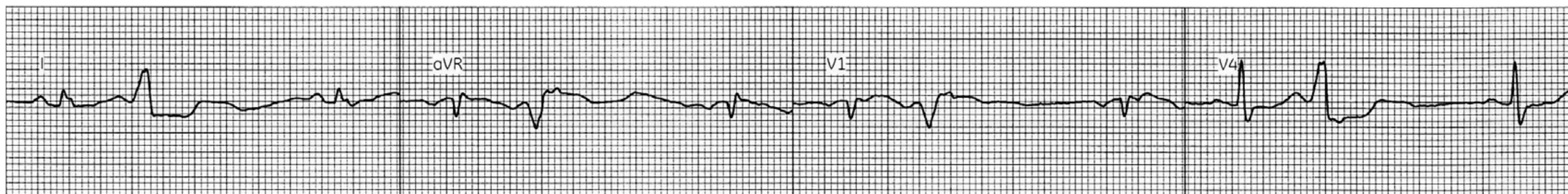
$V2S/V3R \leq 1.5$

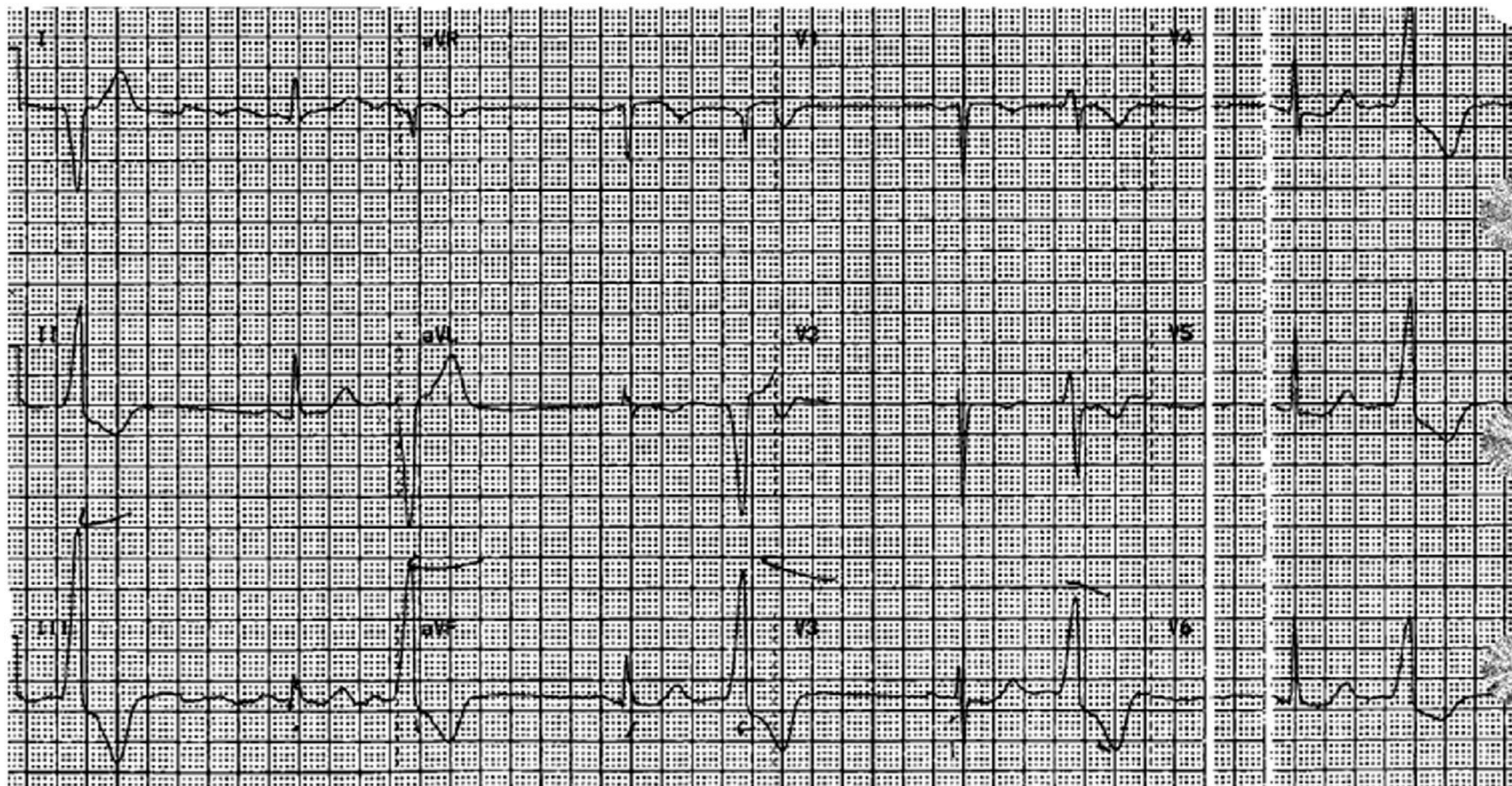
R/S transition in PVC earlier than SR

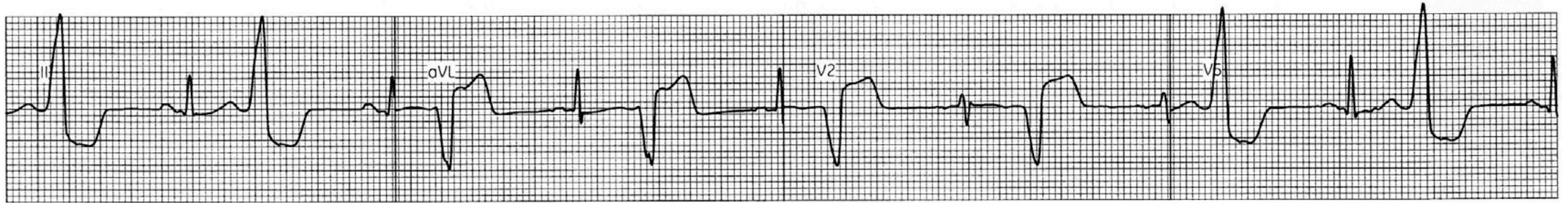
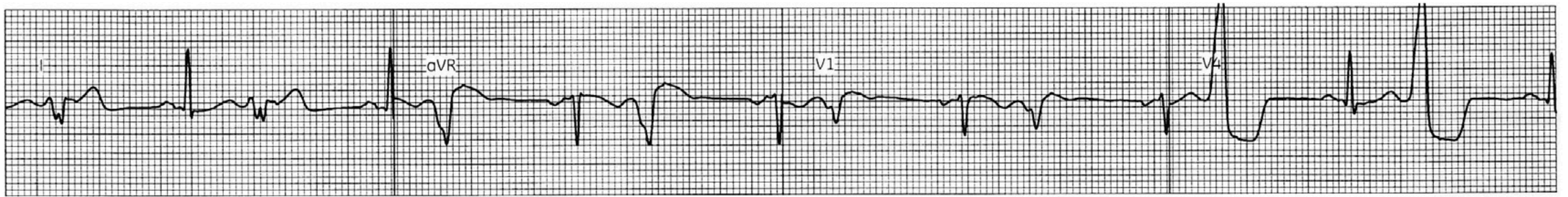


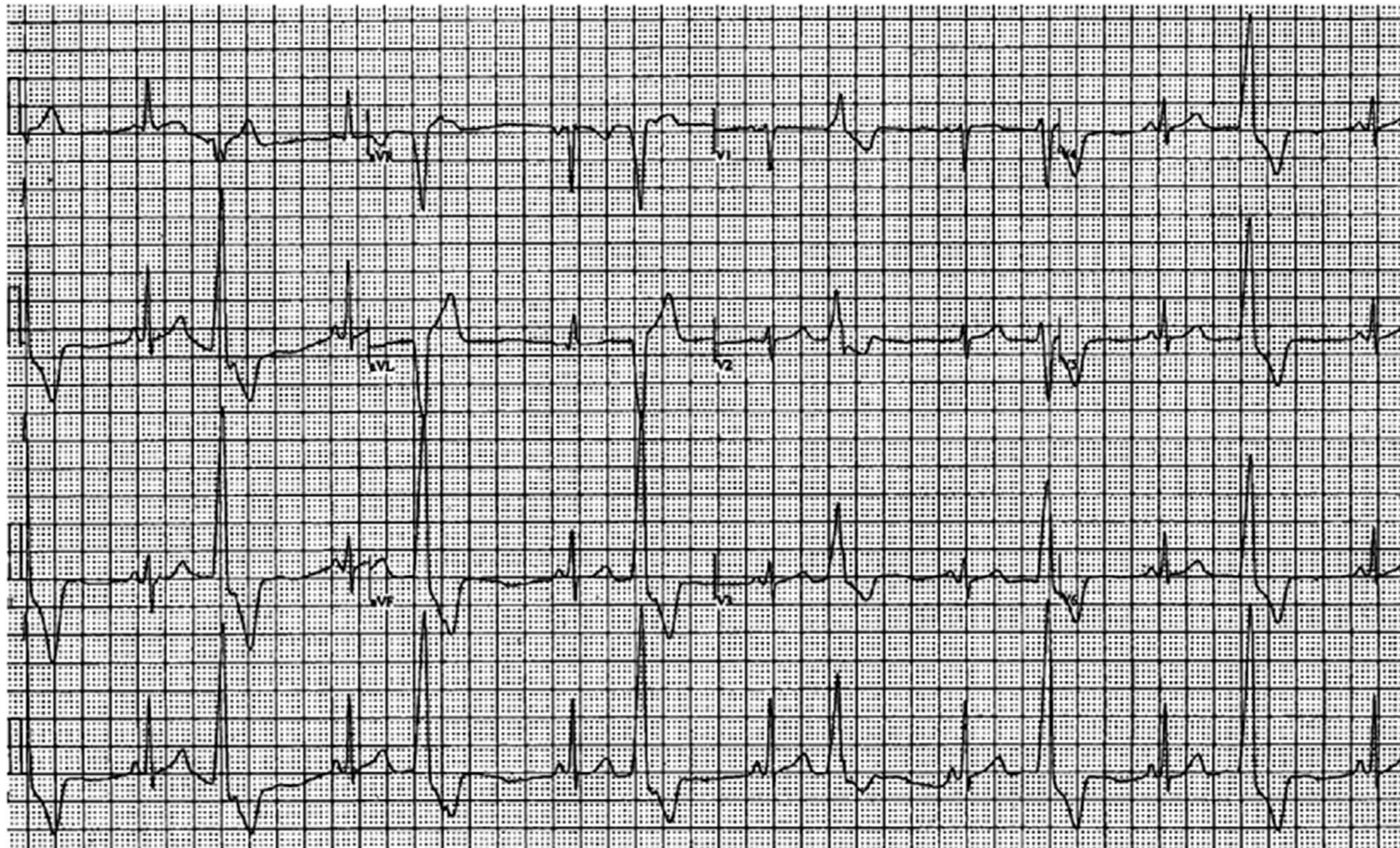


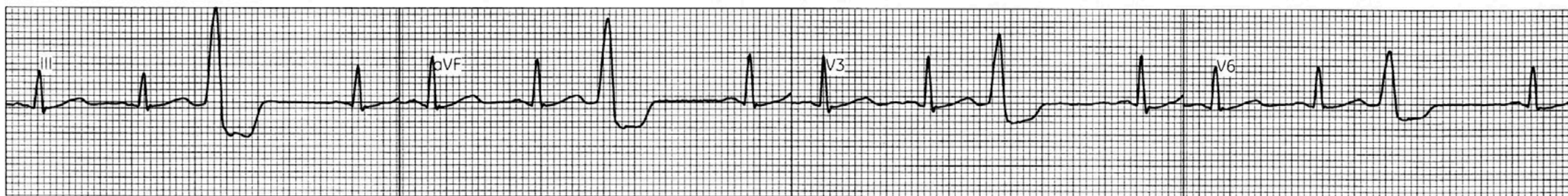
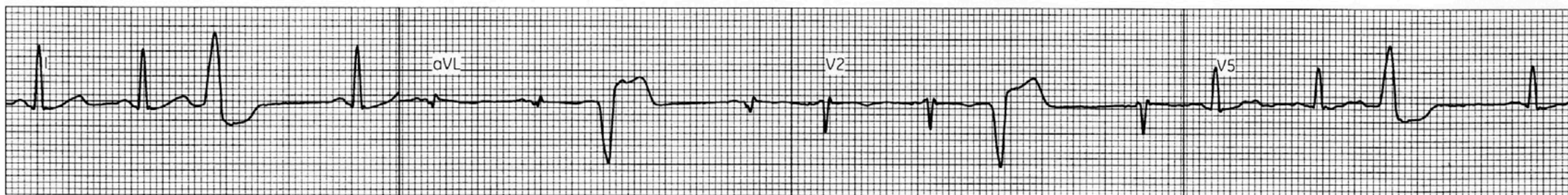
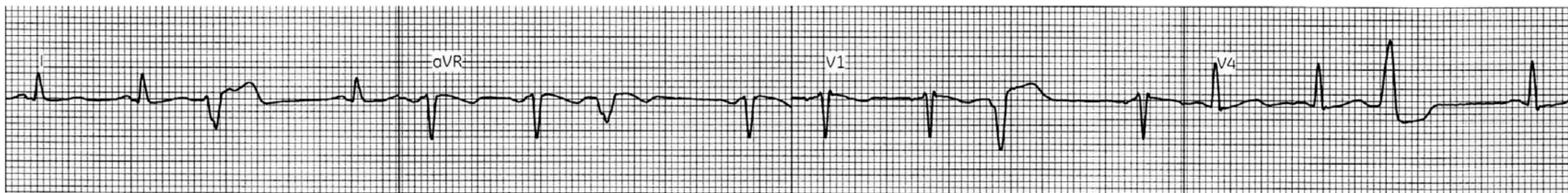




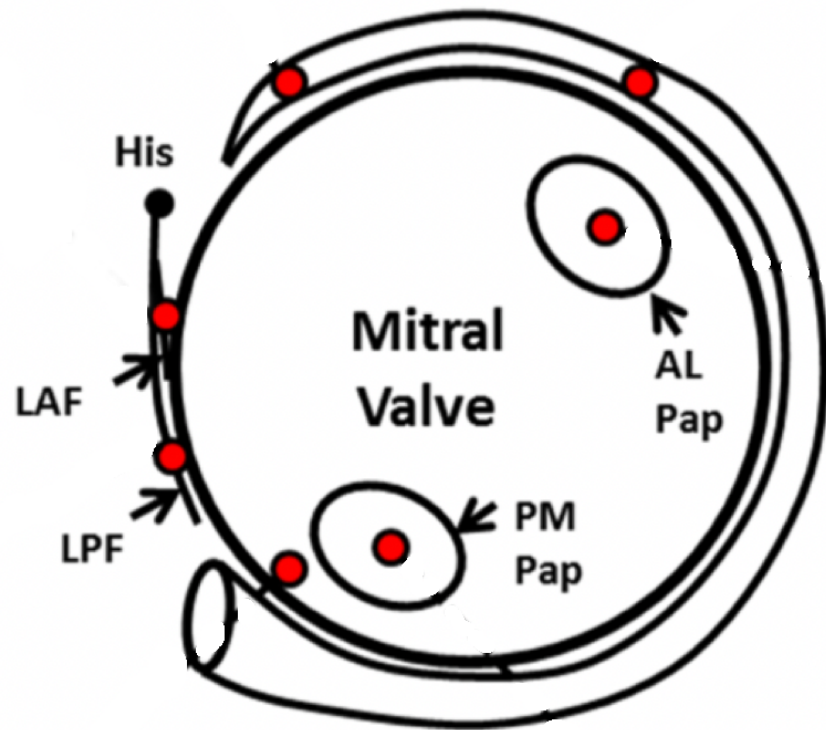




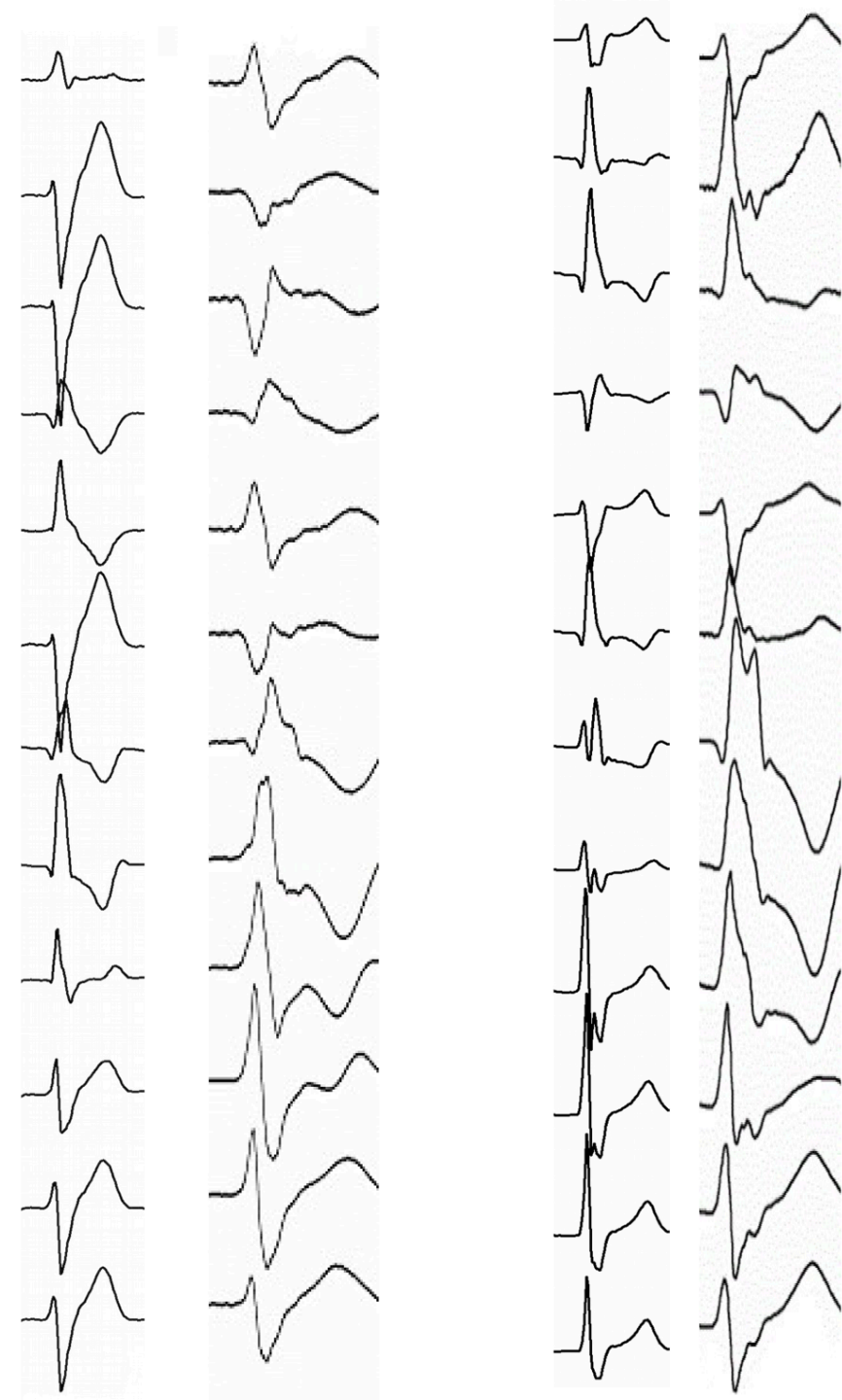




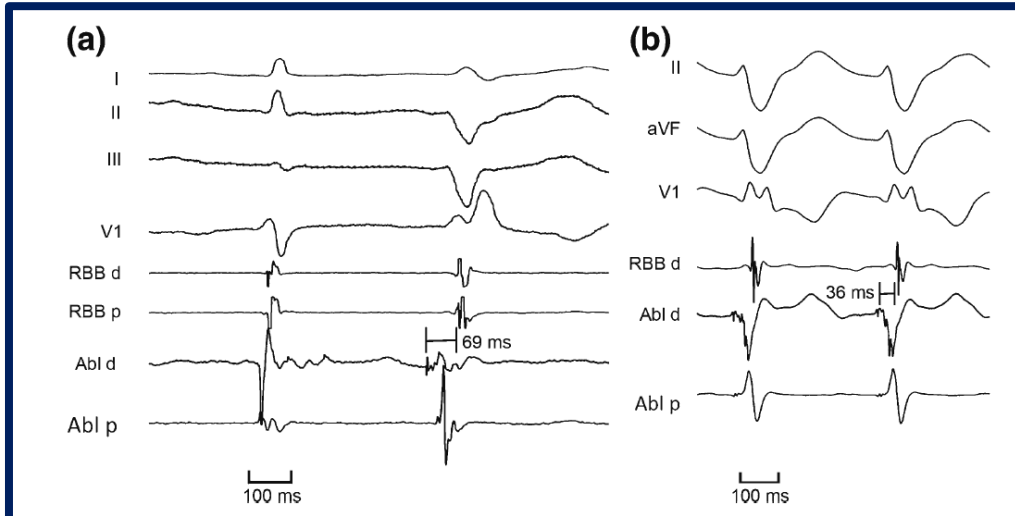
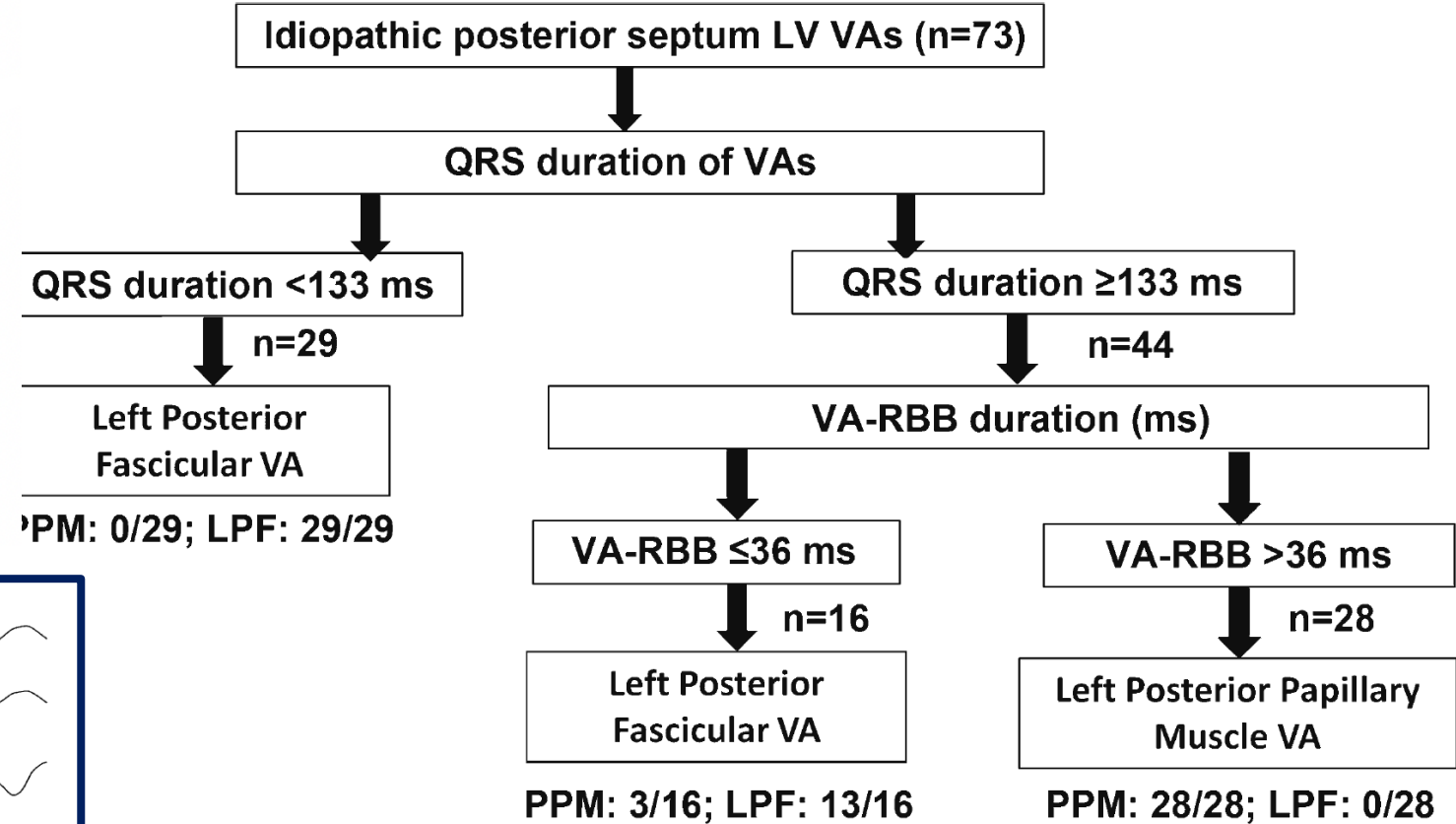
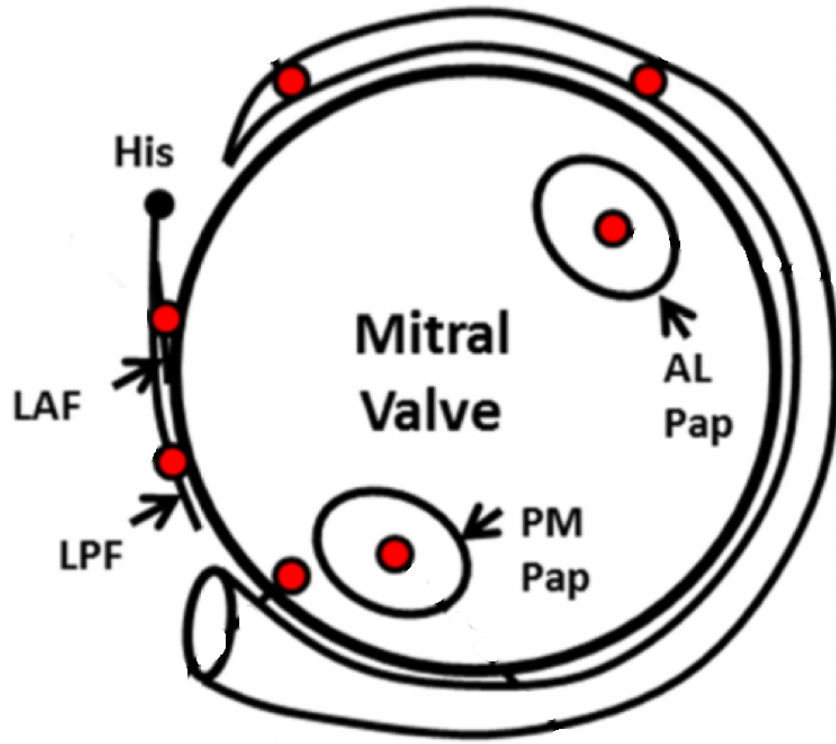
Fascicular or PM VT



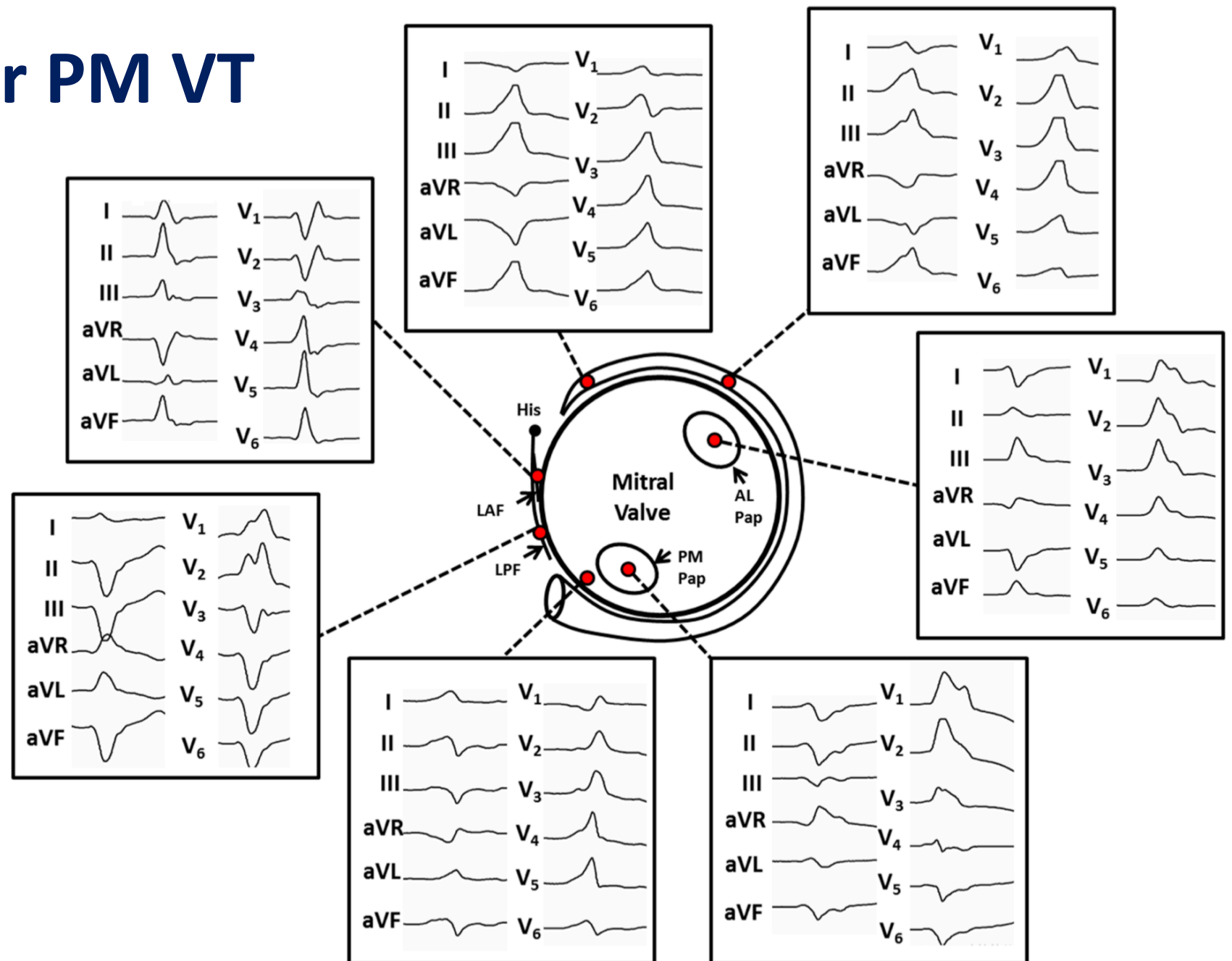
Circ Arrhythm Electrophysiol. 2015;8:616-624.



Fascicular or PM VT



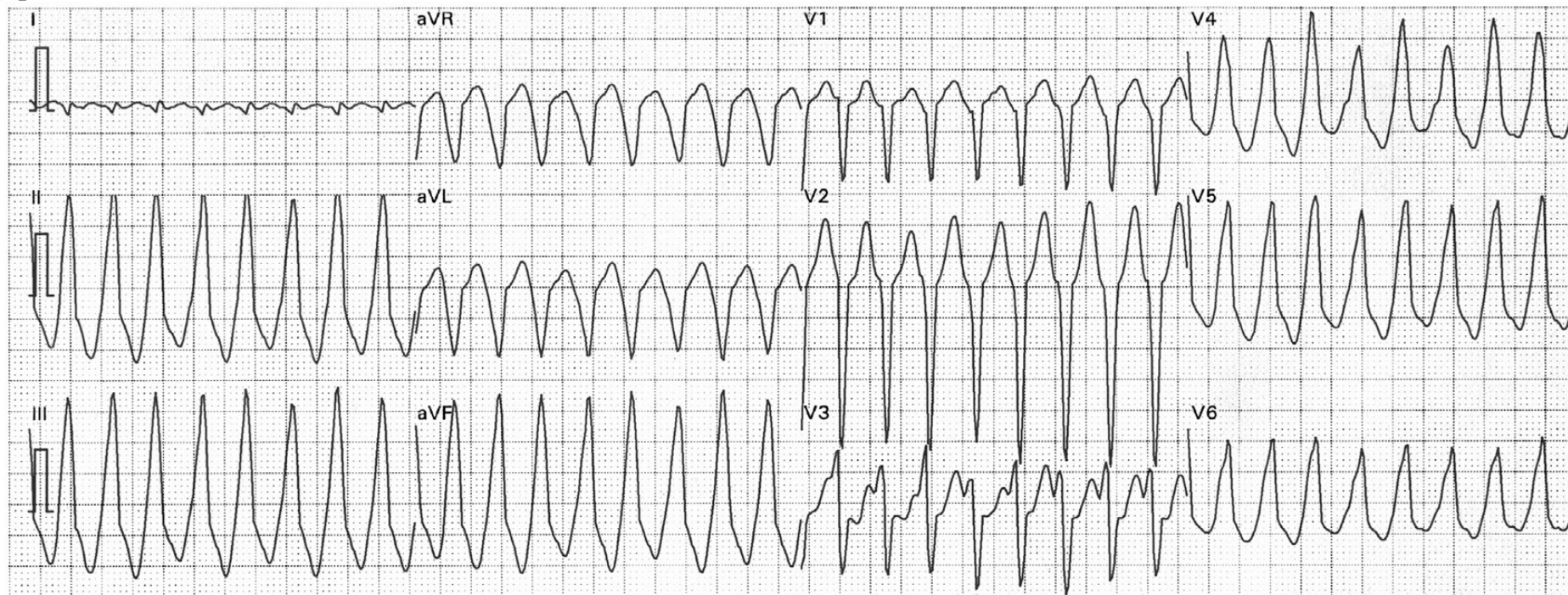
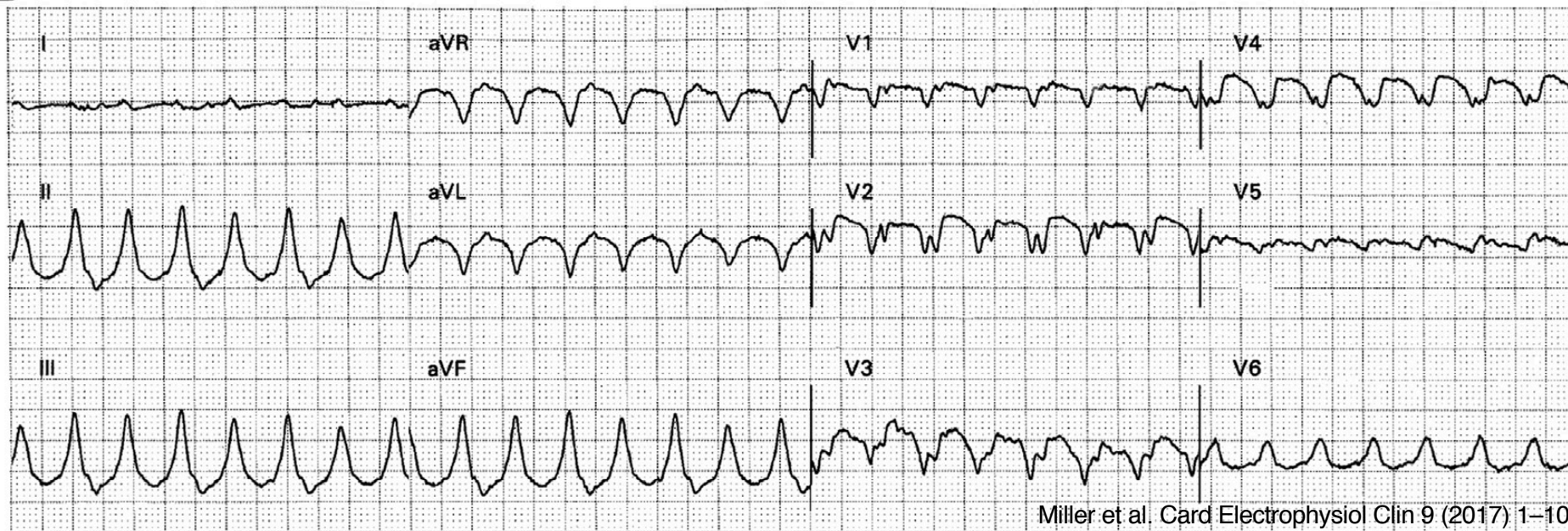
Fascicular or PM VT



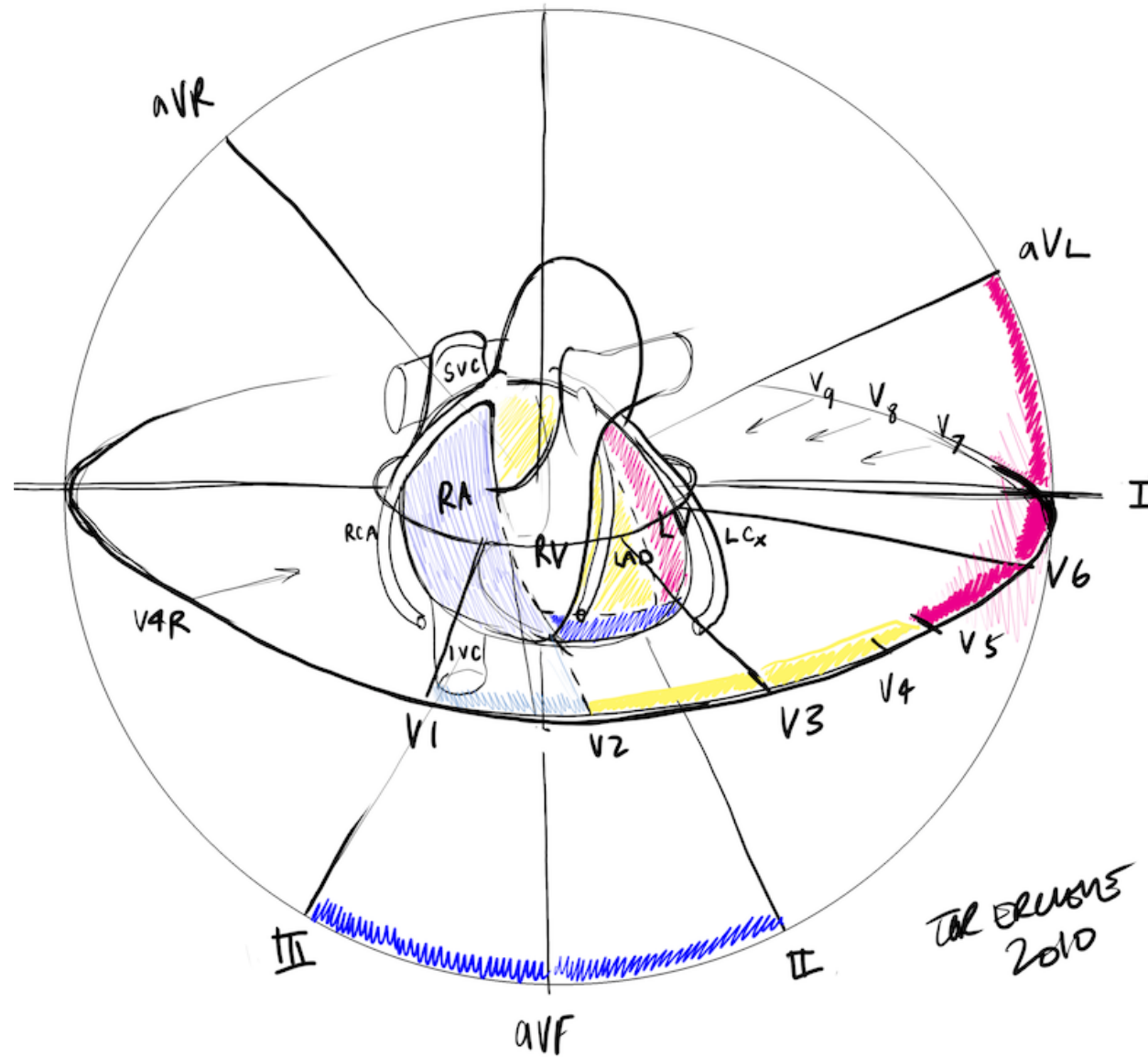
12 lead ECG and ventricular arrhythmias in
patients with structural heart disease

12 lead ECG and ventricular arrhythmias in patients with structural heart disease

- Presence and size of scar
- Intramyocardial fibrosis
- Shape of the heart (e.g. aneurysm) and its position in the chest
- Site of VT origin in the scar area
- Nonuniform anisotropy
- Acute ischemia
- Integrity of His-Purkinje system
- LVH/RVH

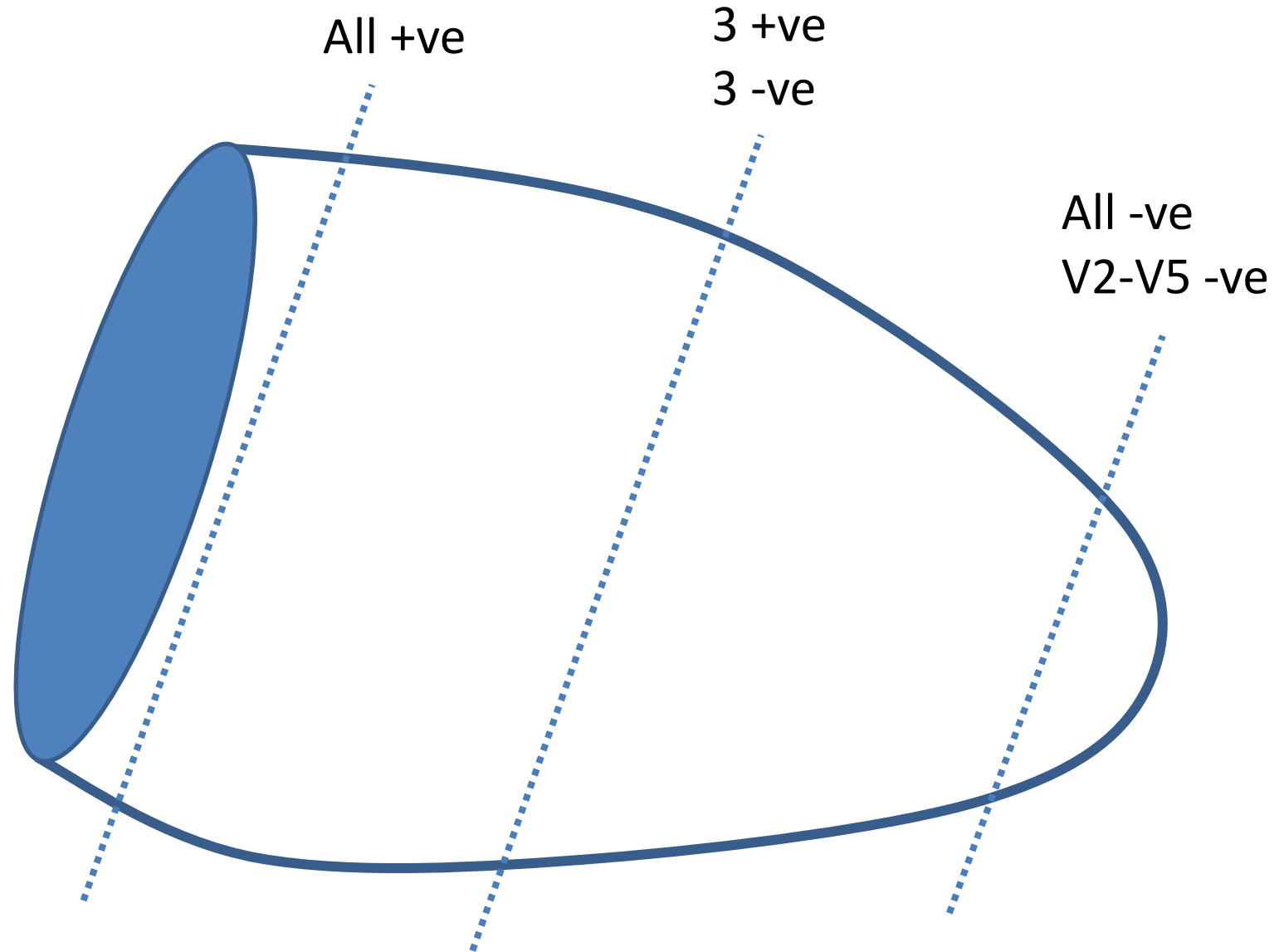
A**B**

STEP1: V1

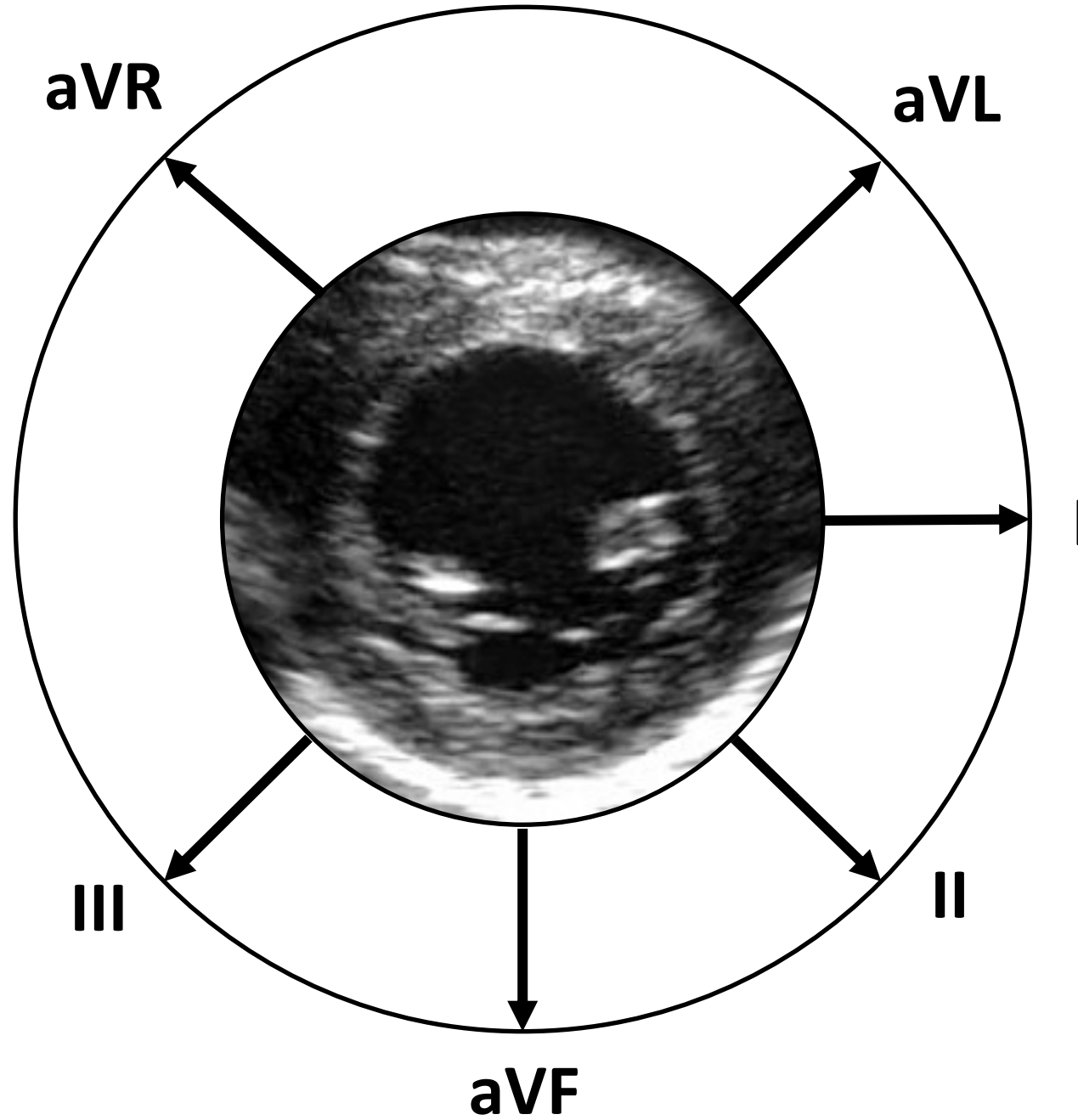


My Simplified Approach

STEP2: V1-V6

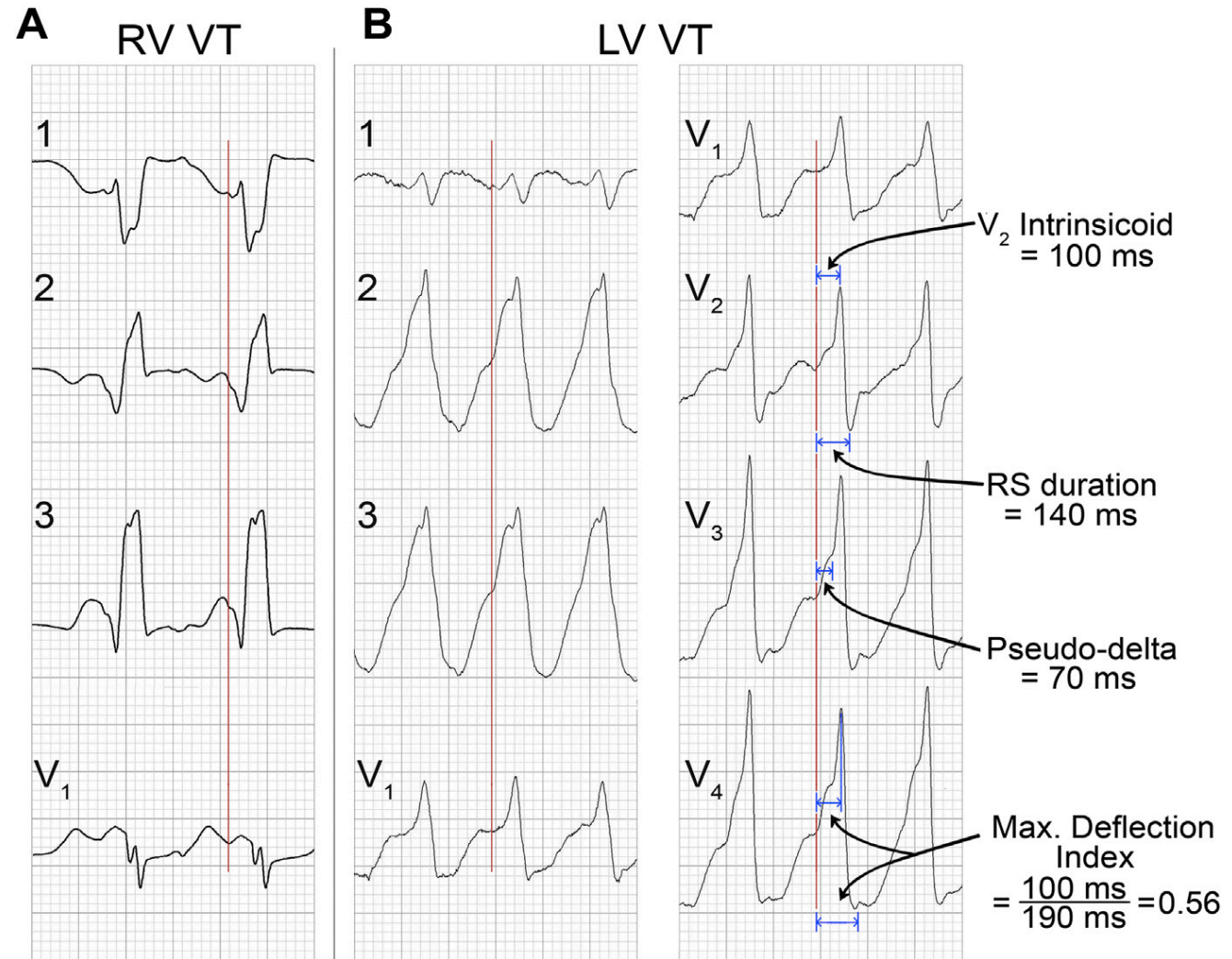


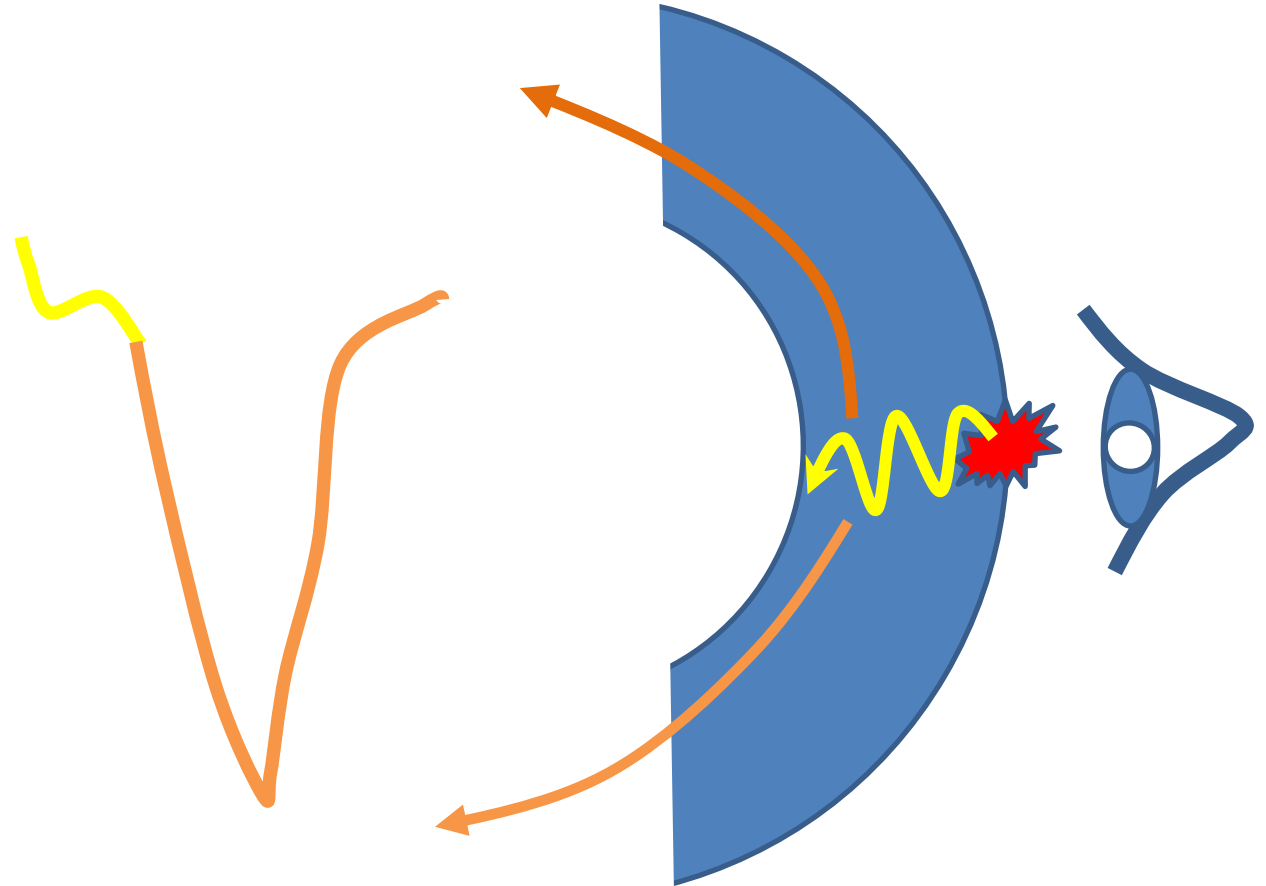
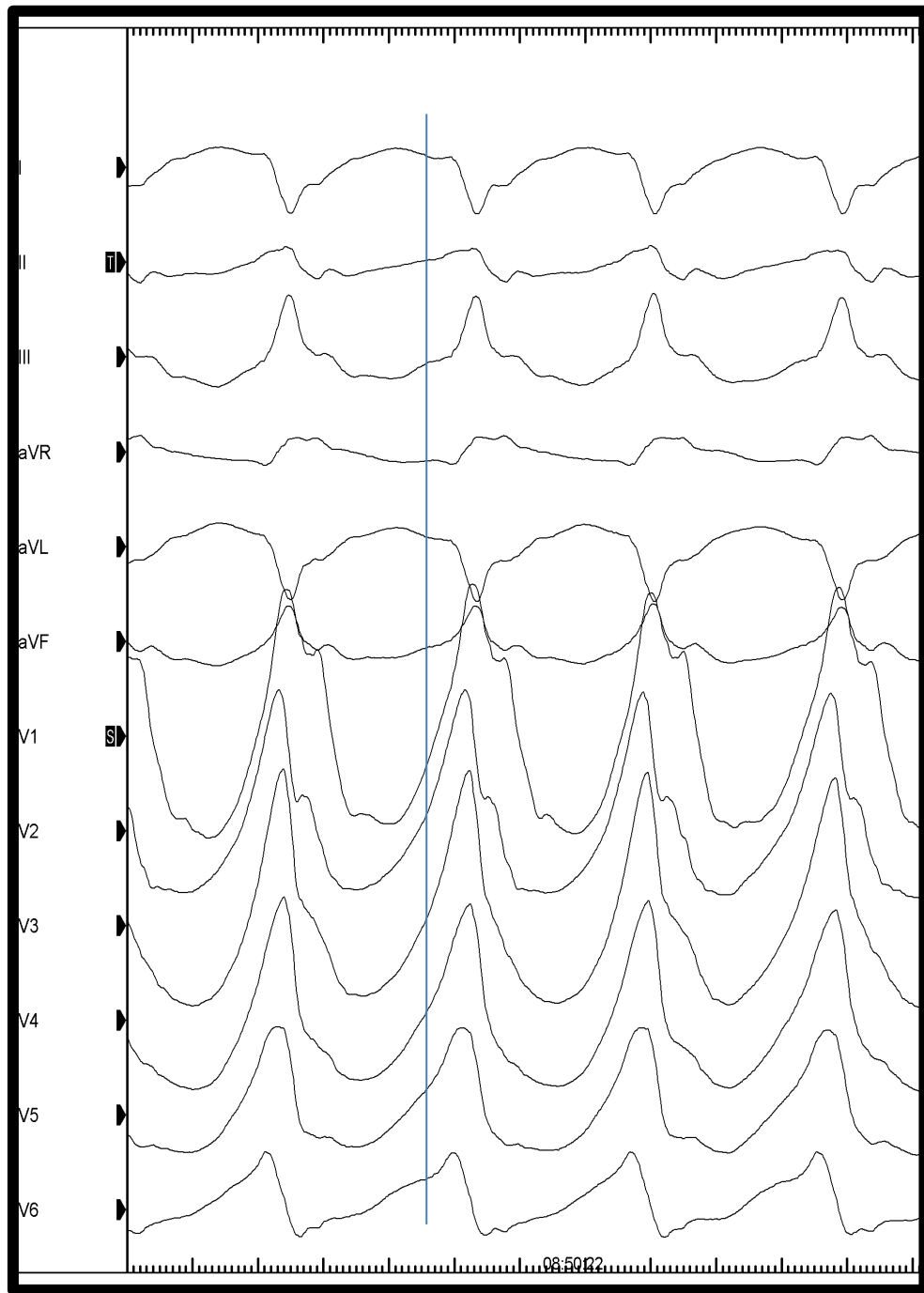
STEP3: Limb Leads

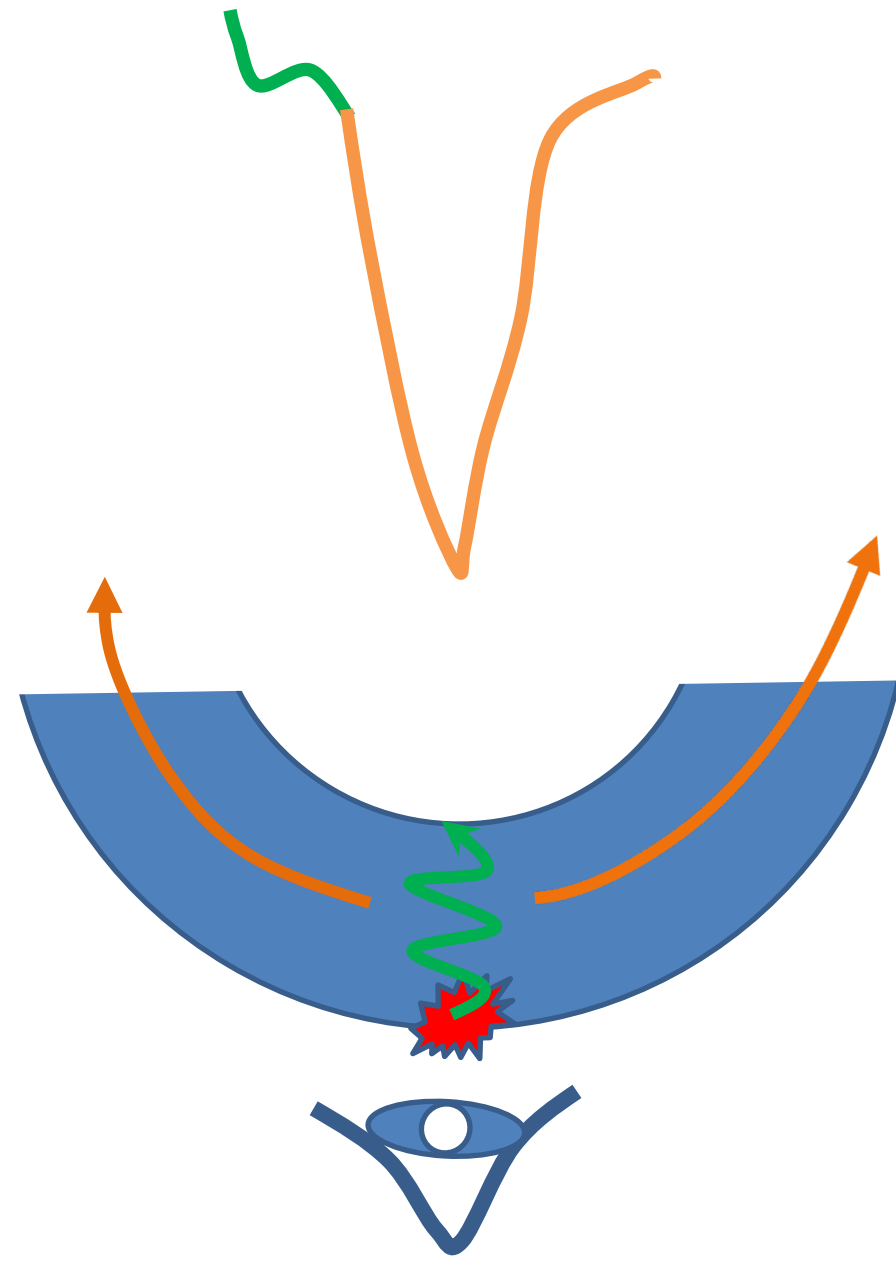
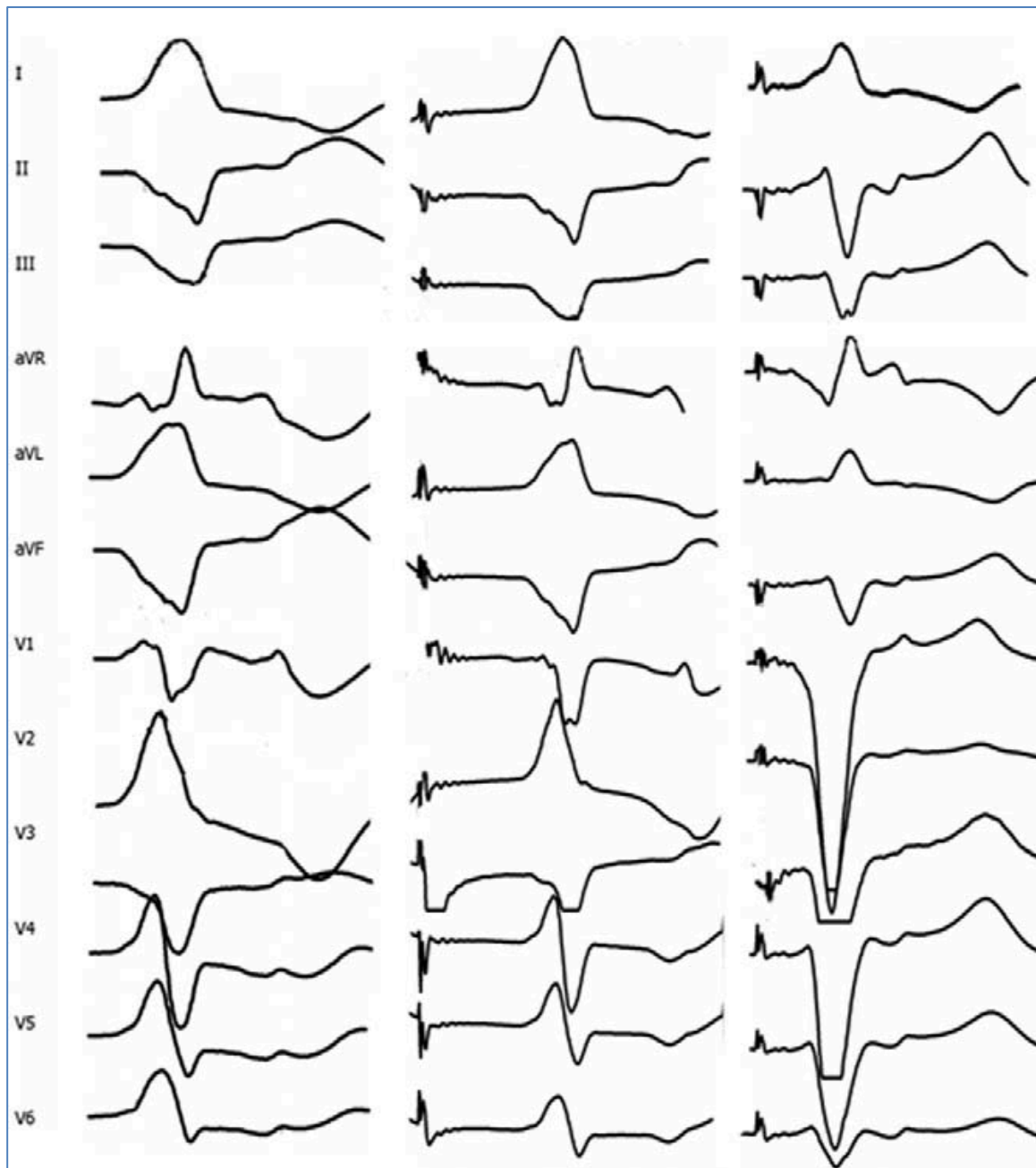


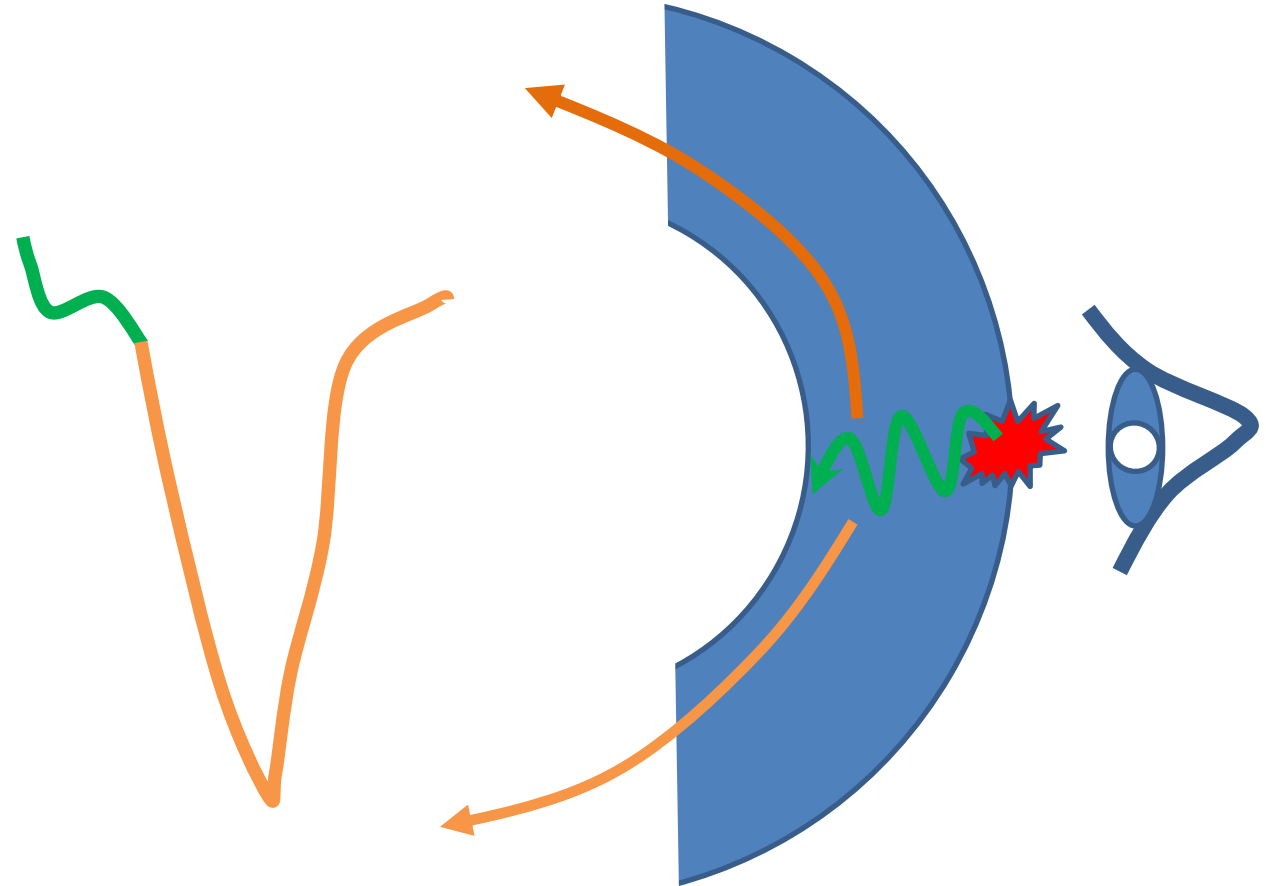
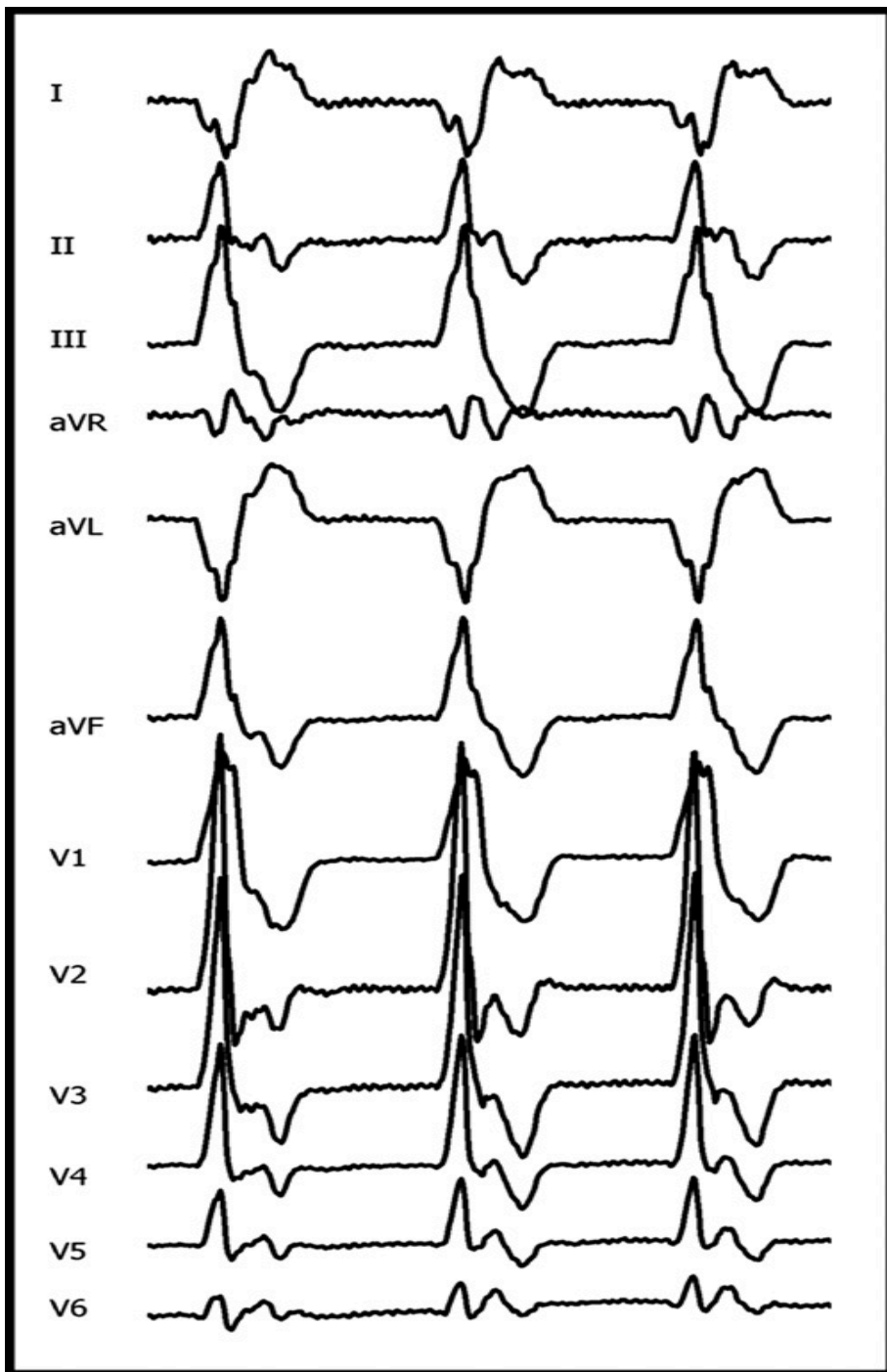
Epicardial Exit

Several criteria have been proposed to identify VTs that require epicardial mapping and ablation; these can be separated into 2 categories, namely, those based on interval/duration and those based on QRS morphologies

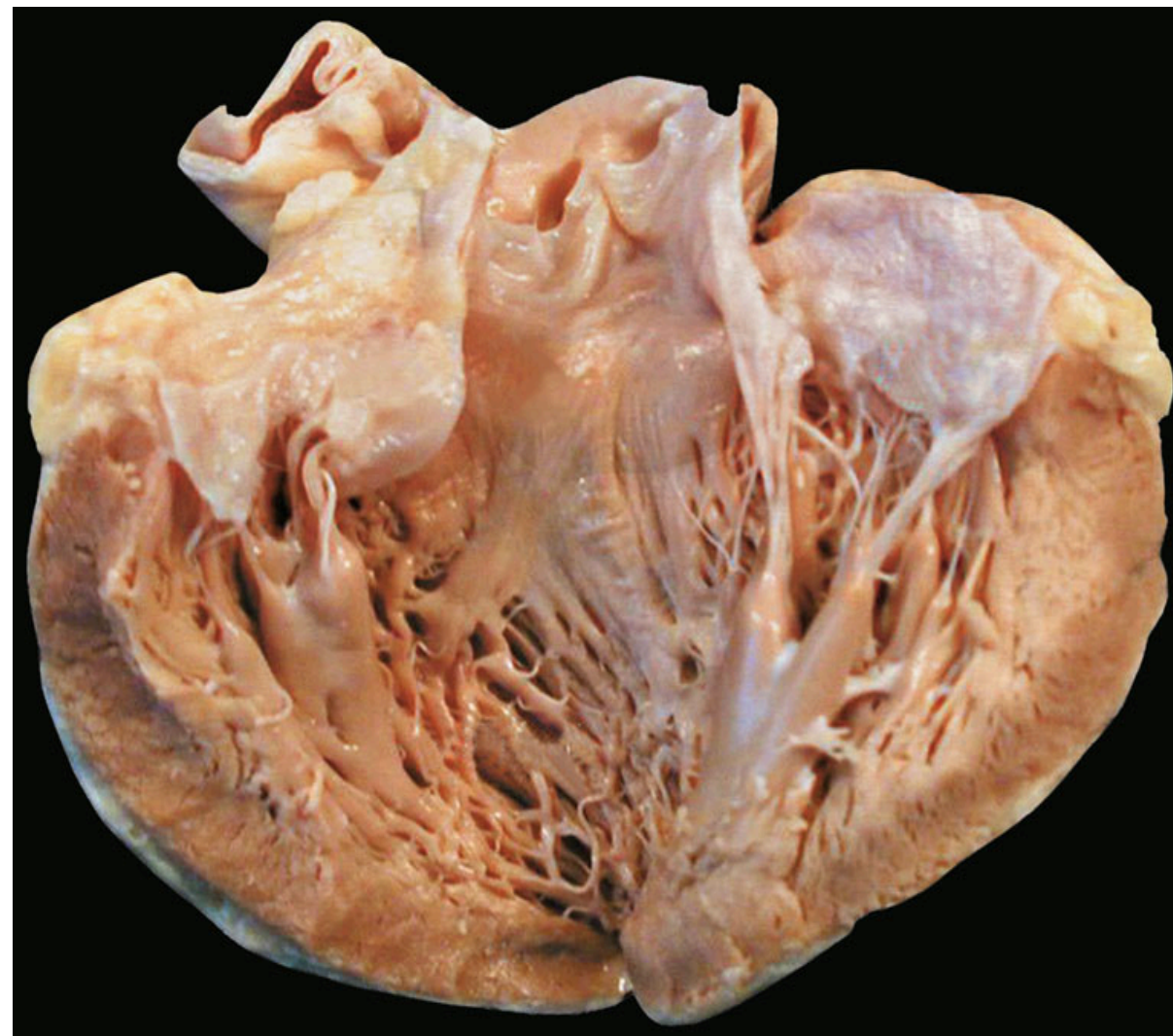
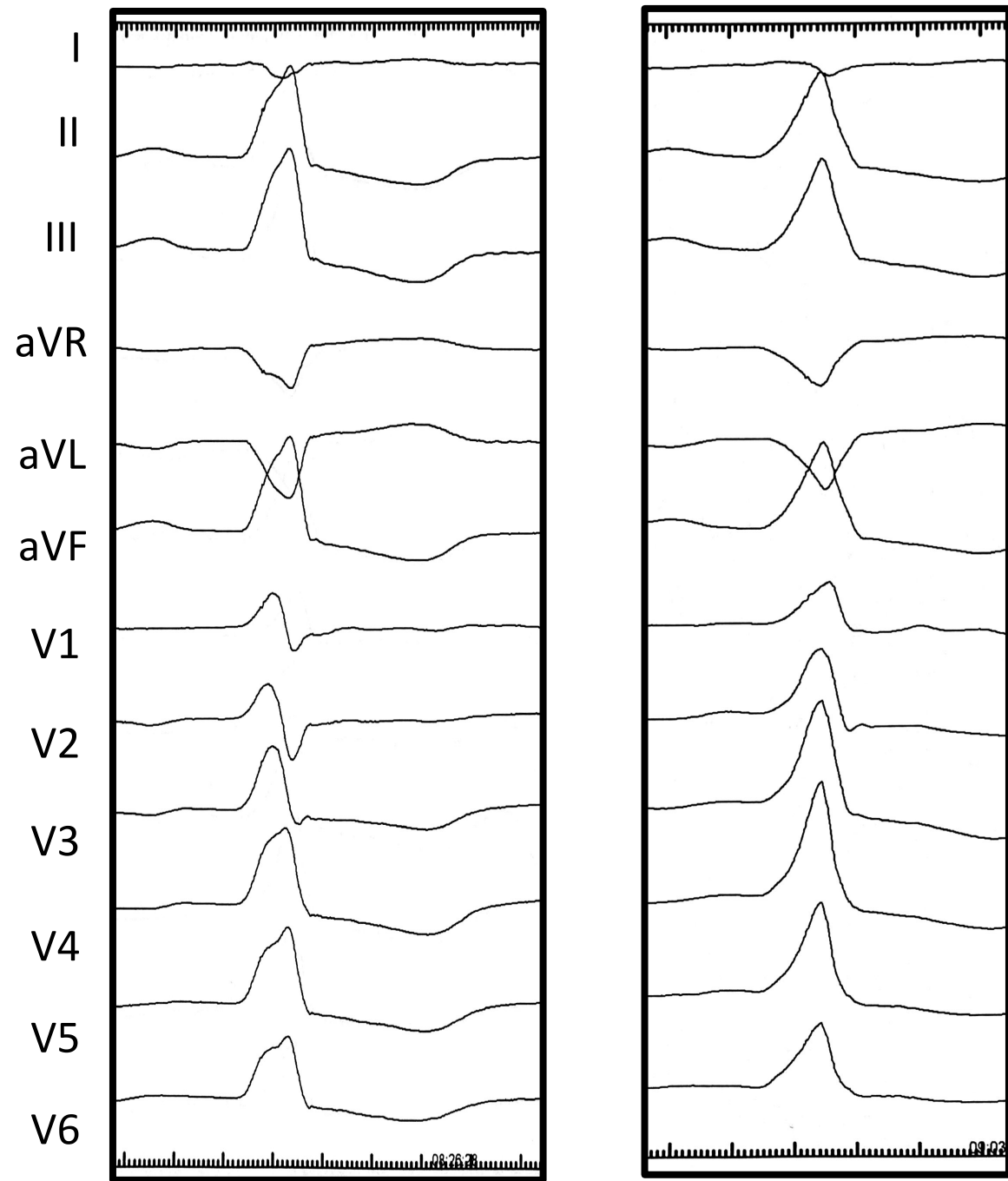


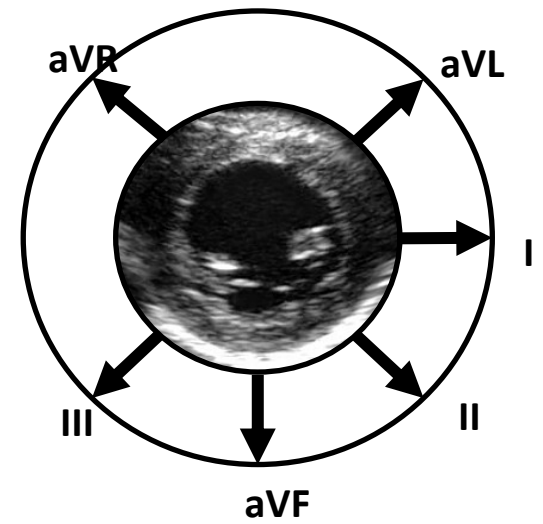
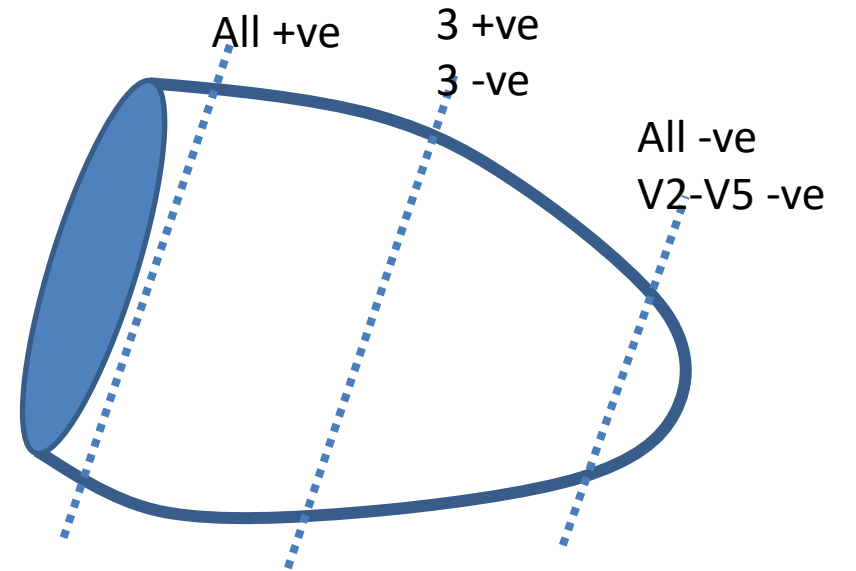
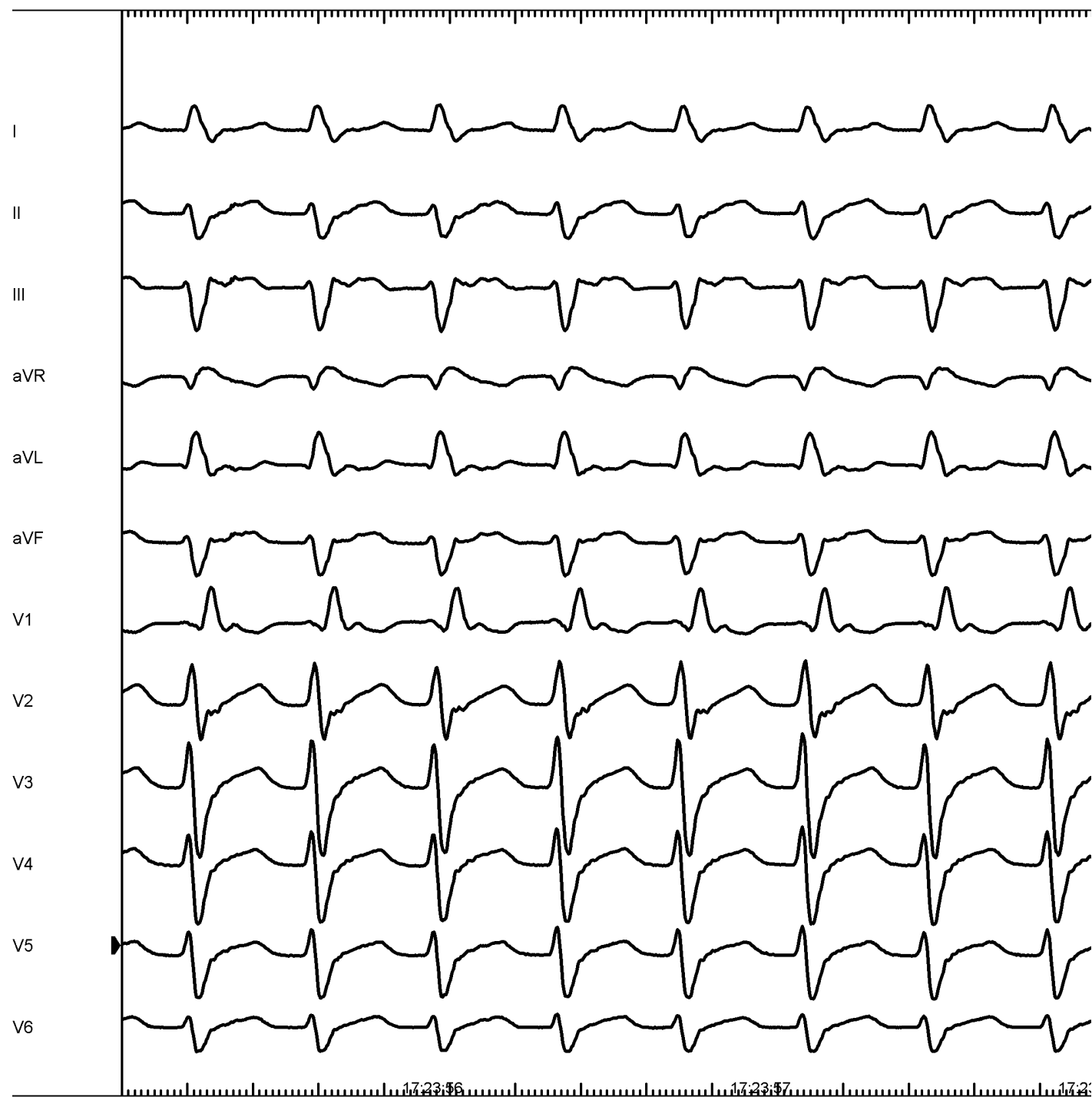






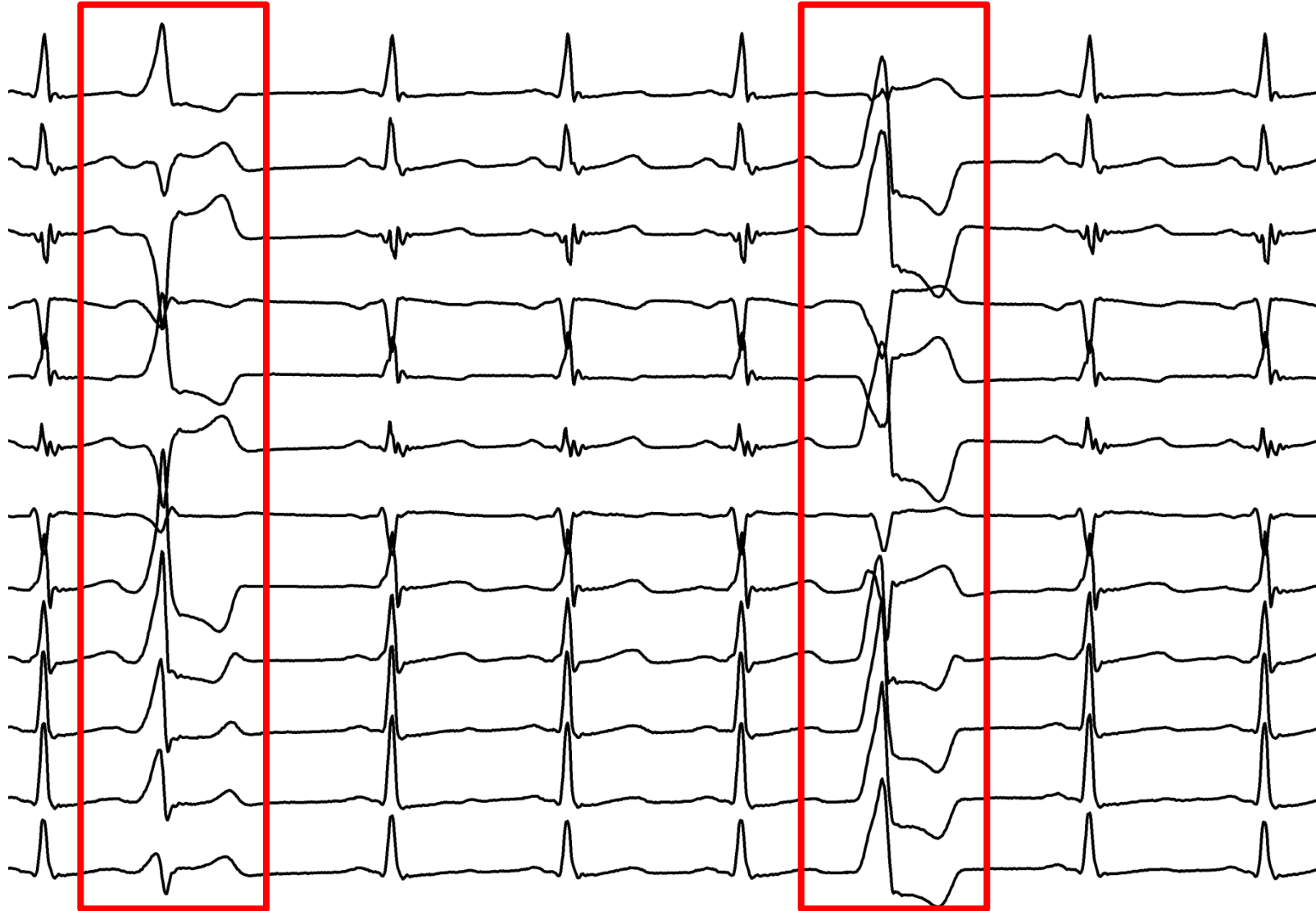
VT Localization: case studies



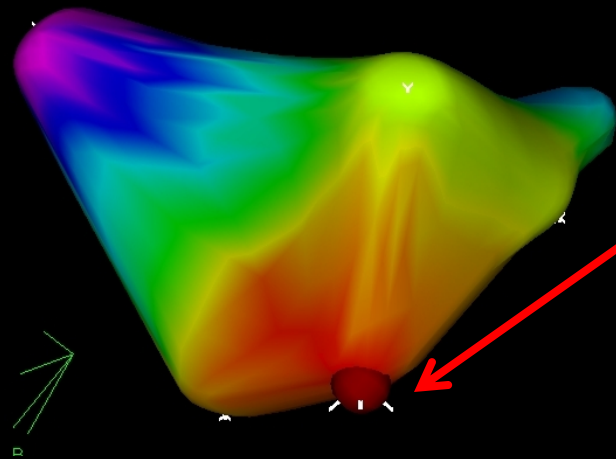


MV

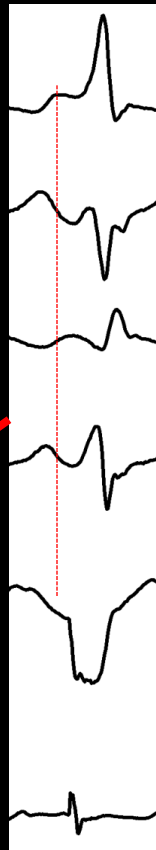
LCC



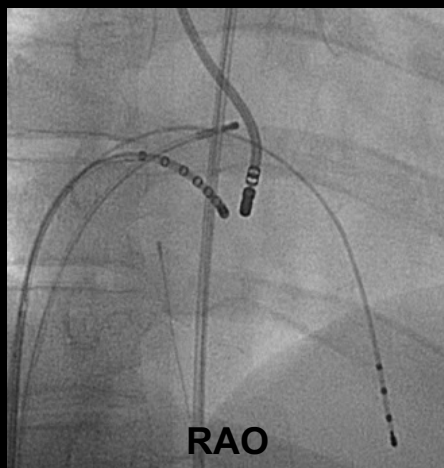
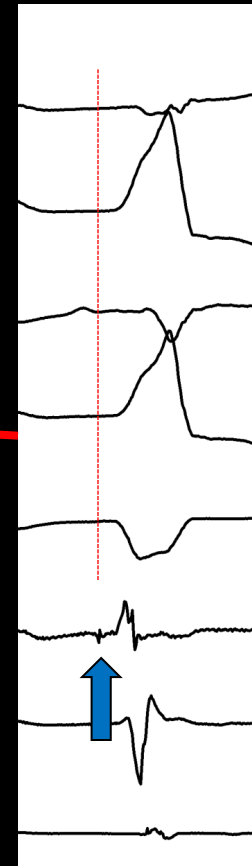
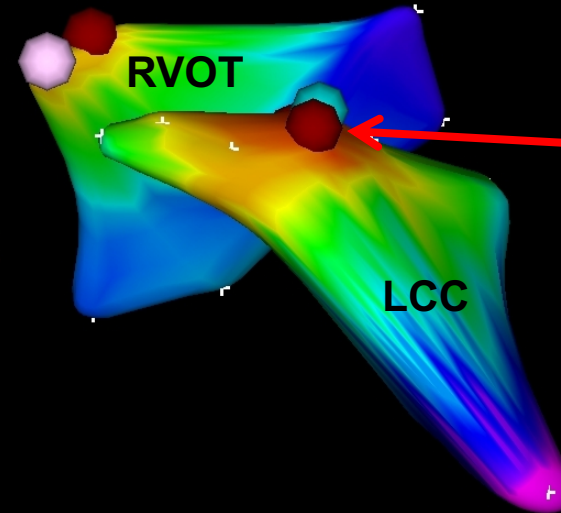
PVC from MA



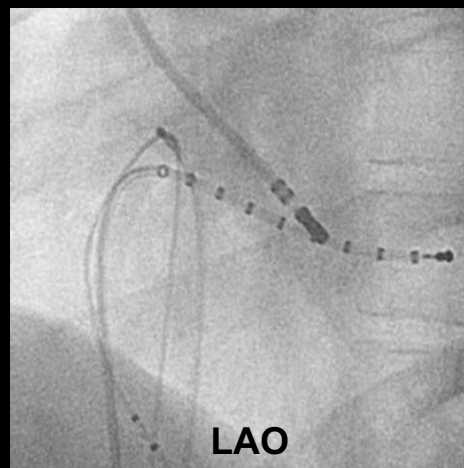
Inferior View



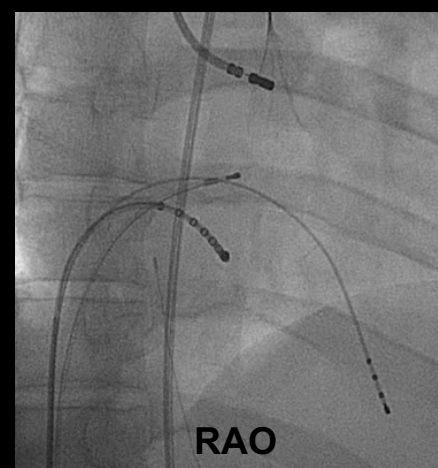
PVC from LCC



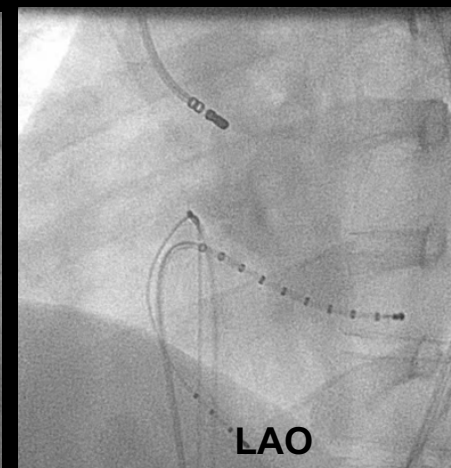
RAO



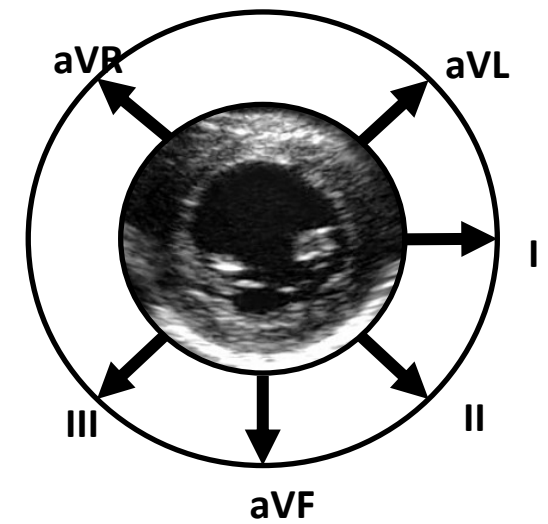
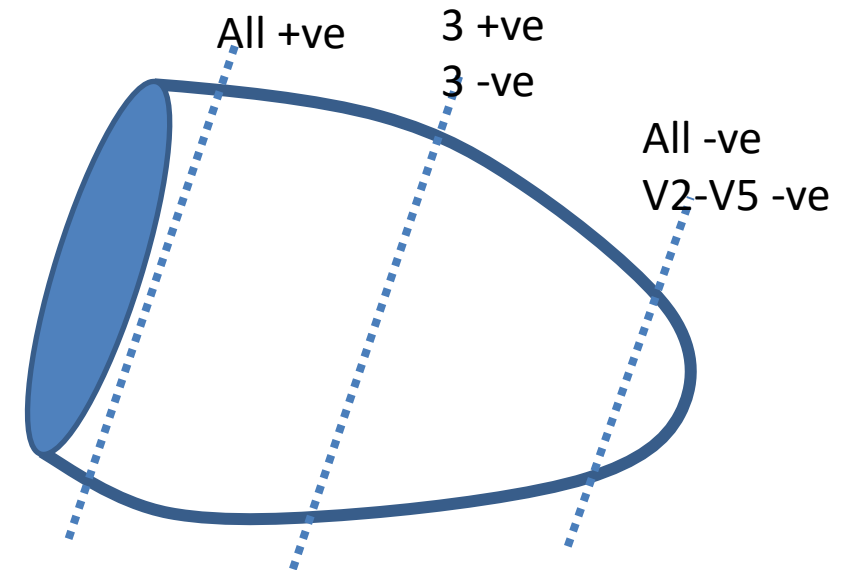
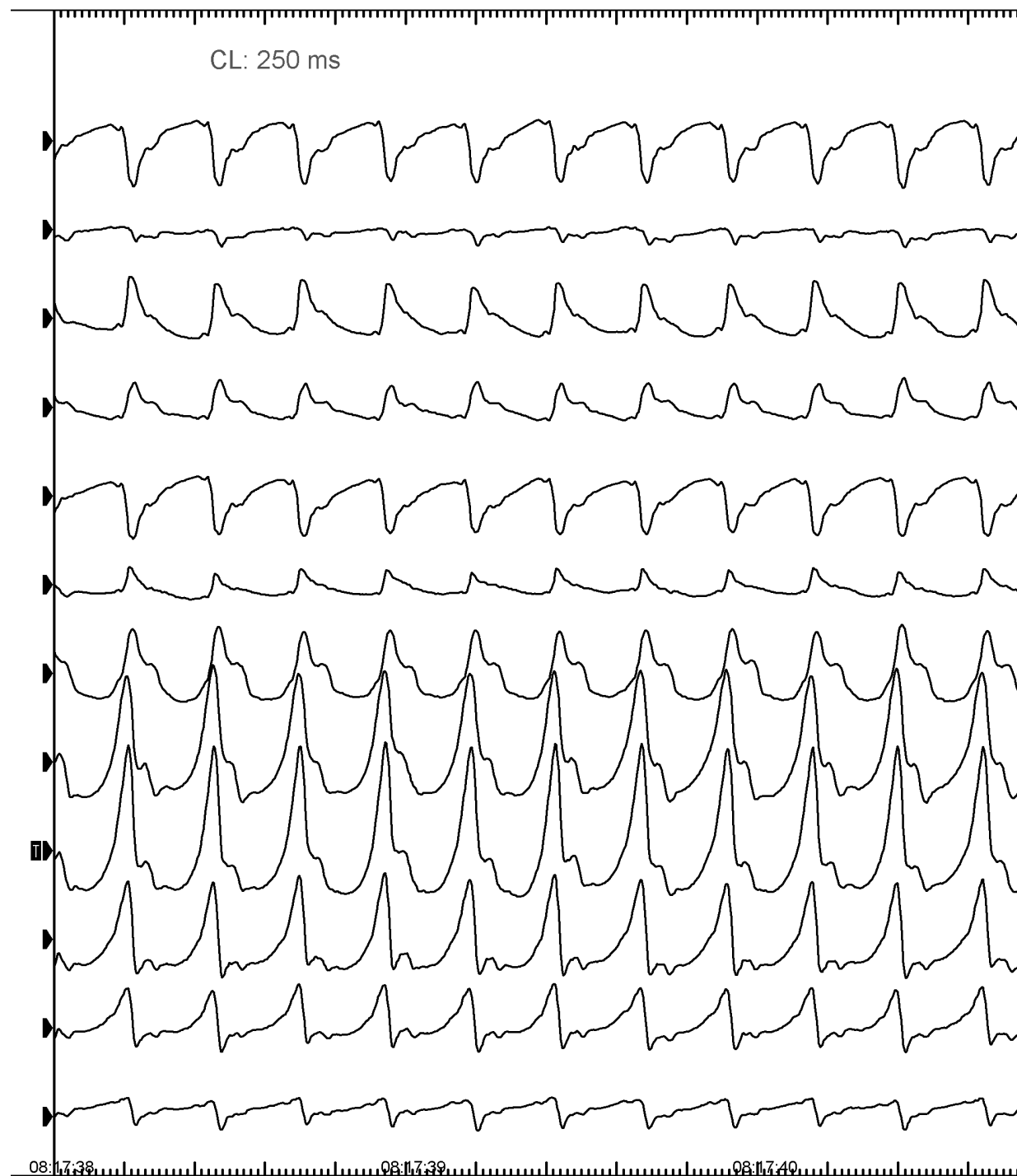
LAO



RAO



LAO





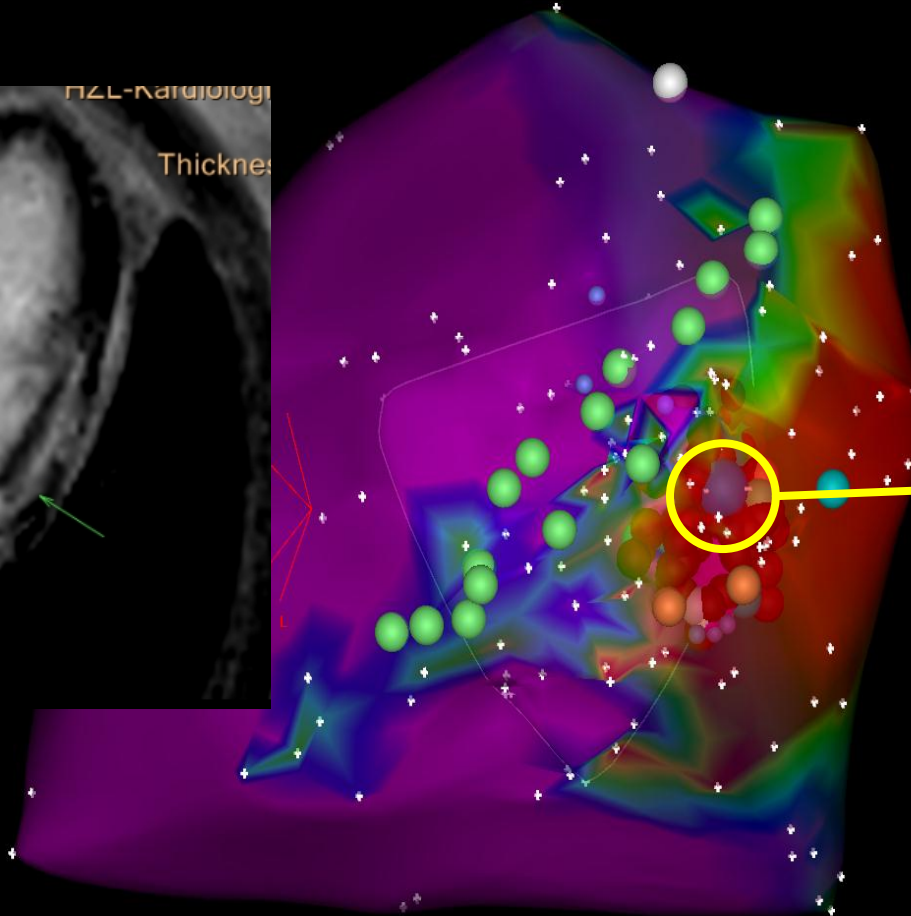
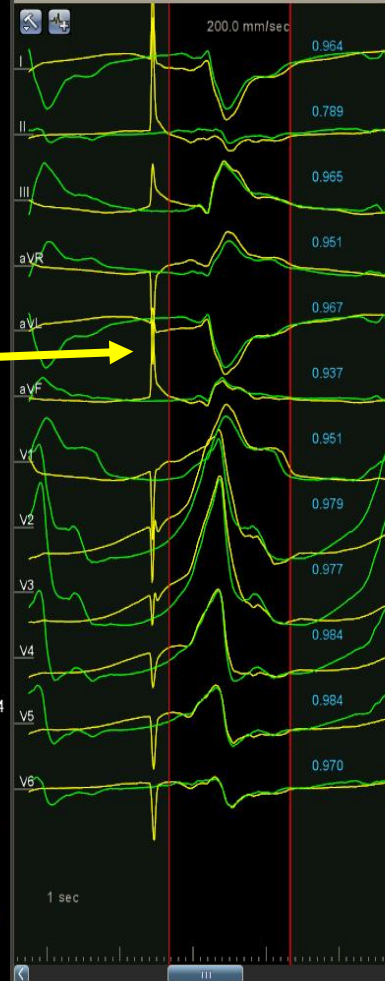
2-endo (137, 0)

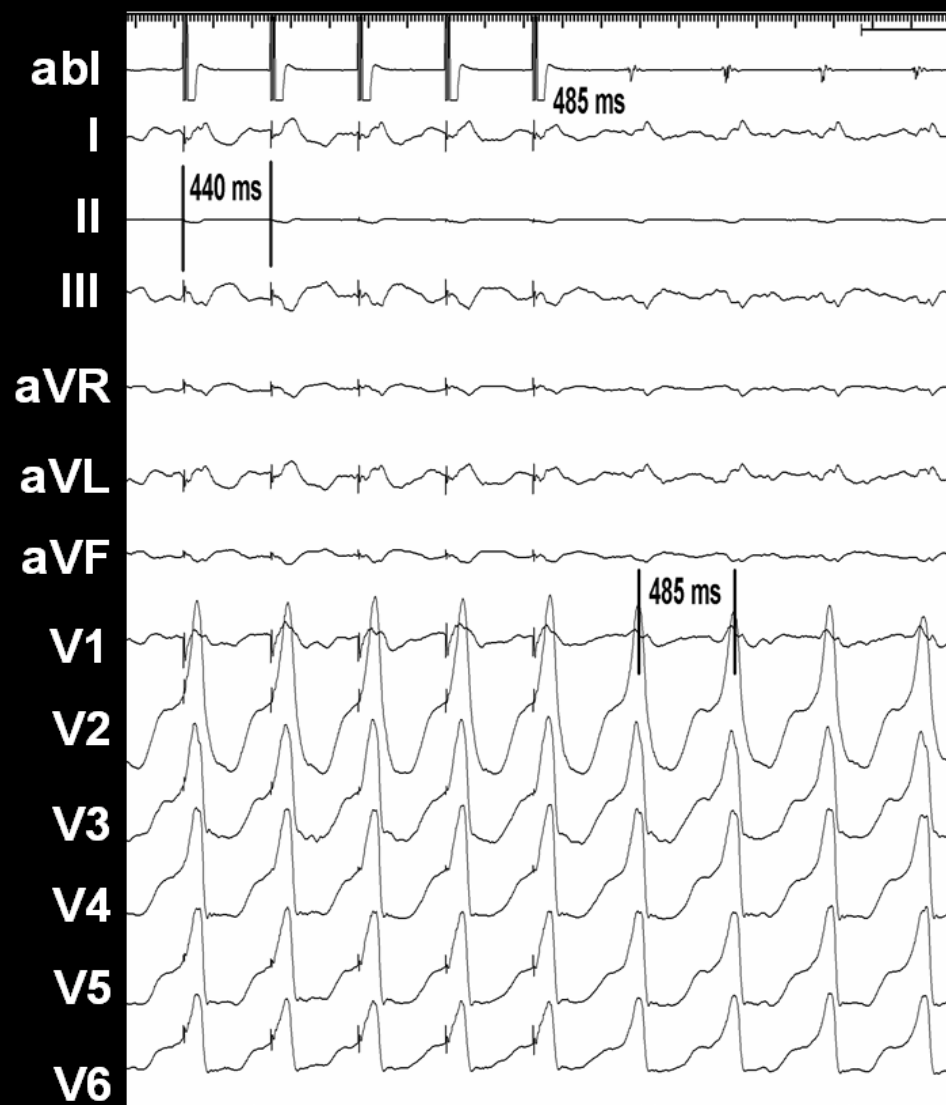
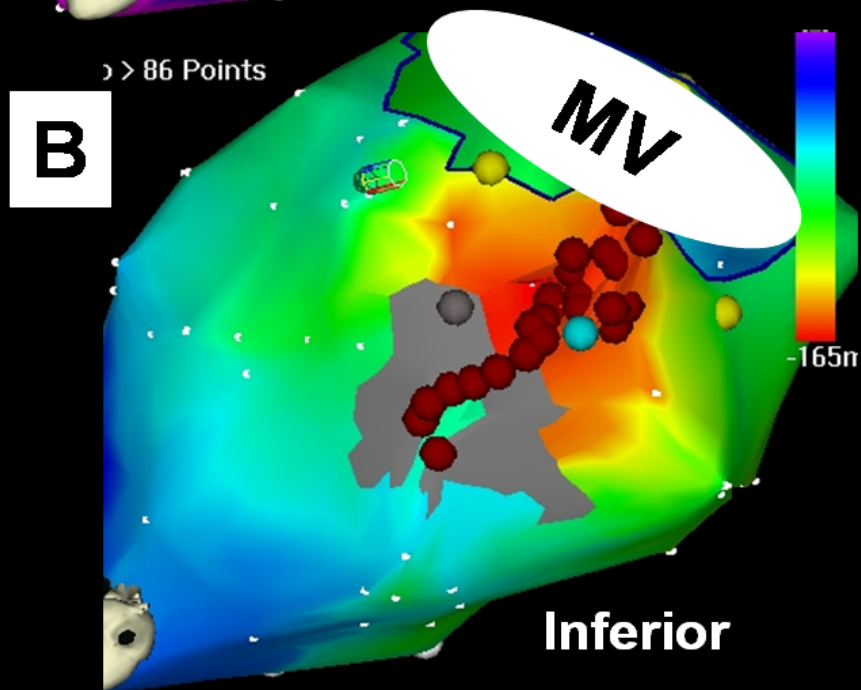
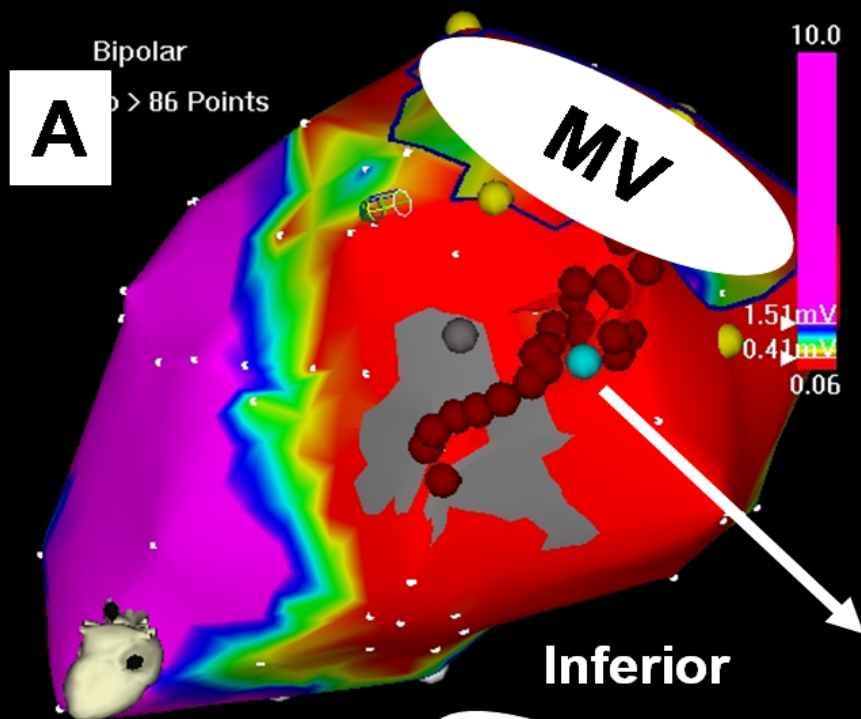
0.50 mV Bi 1.50 mV

Acquisition Correlation

PM/IS Correlation Table

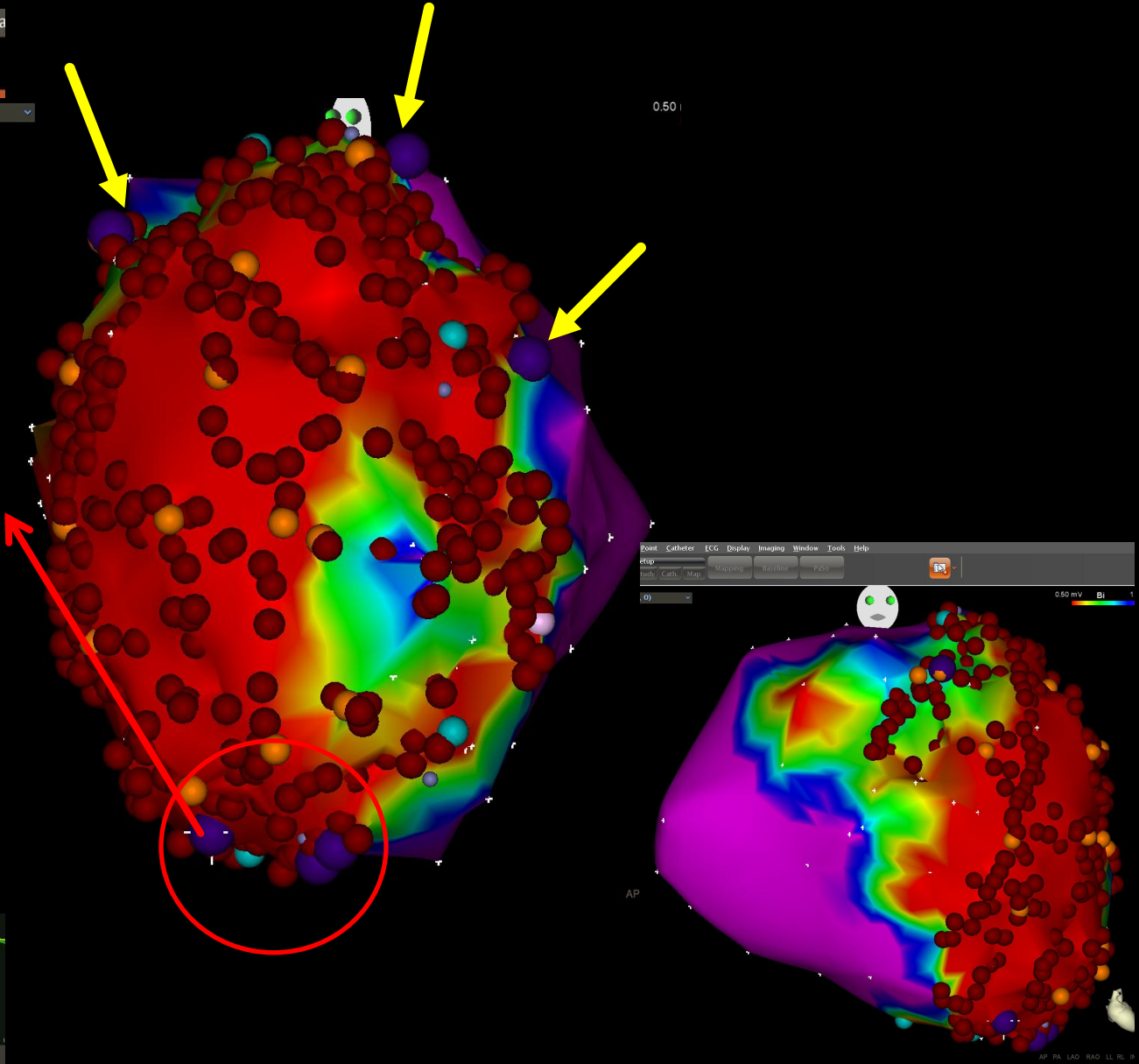
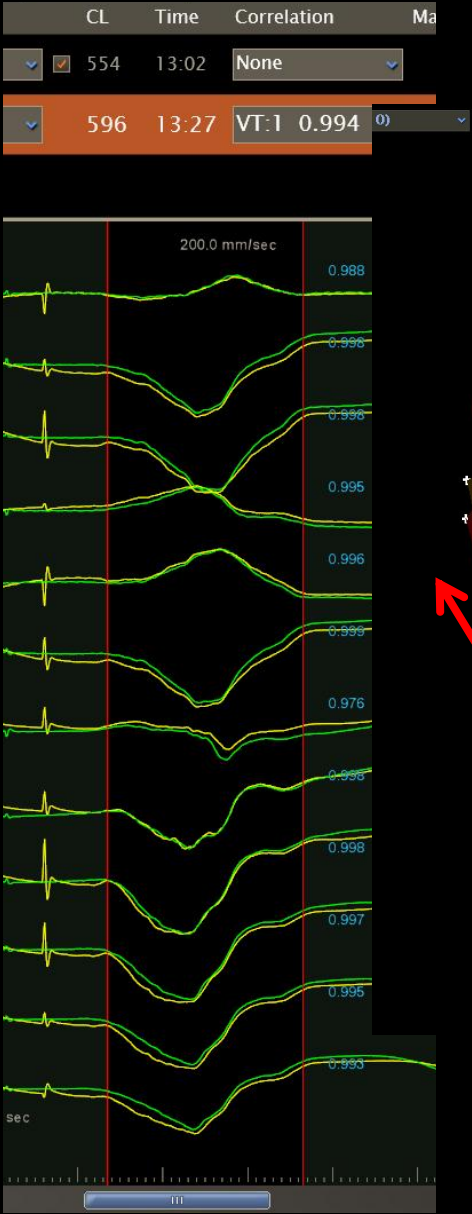
#	PM Name	VES:4	VES:5
18	PM:7	0.834	0.599
19	PM:8	0.840	0.573
21	PM:9	0.915	0.846
23	PM:10	0.952	0.826

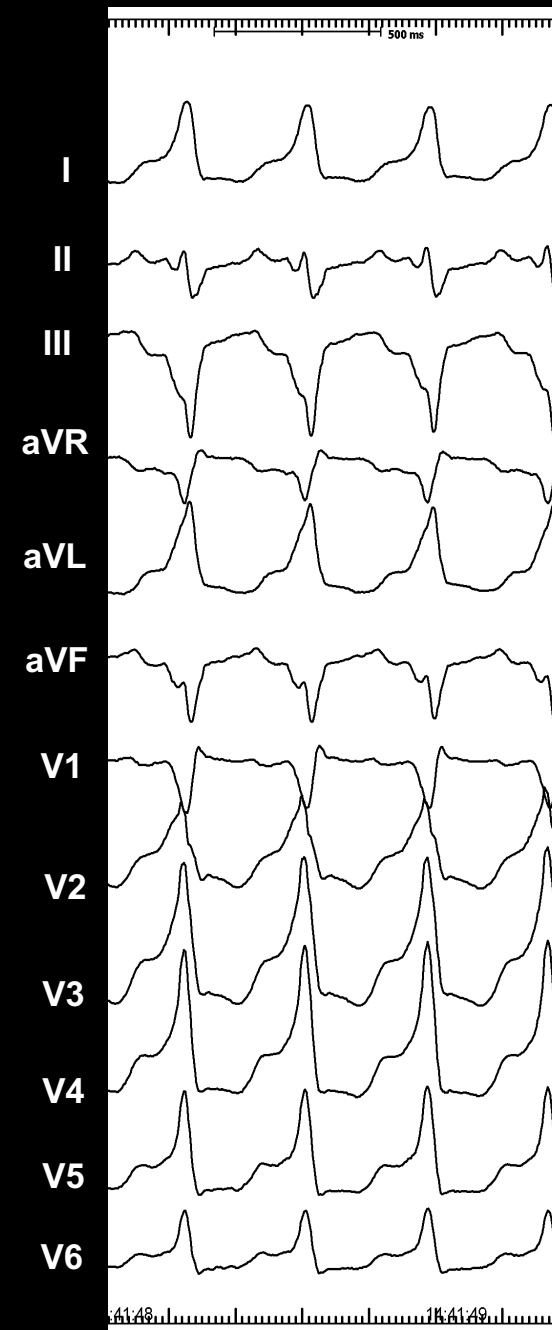
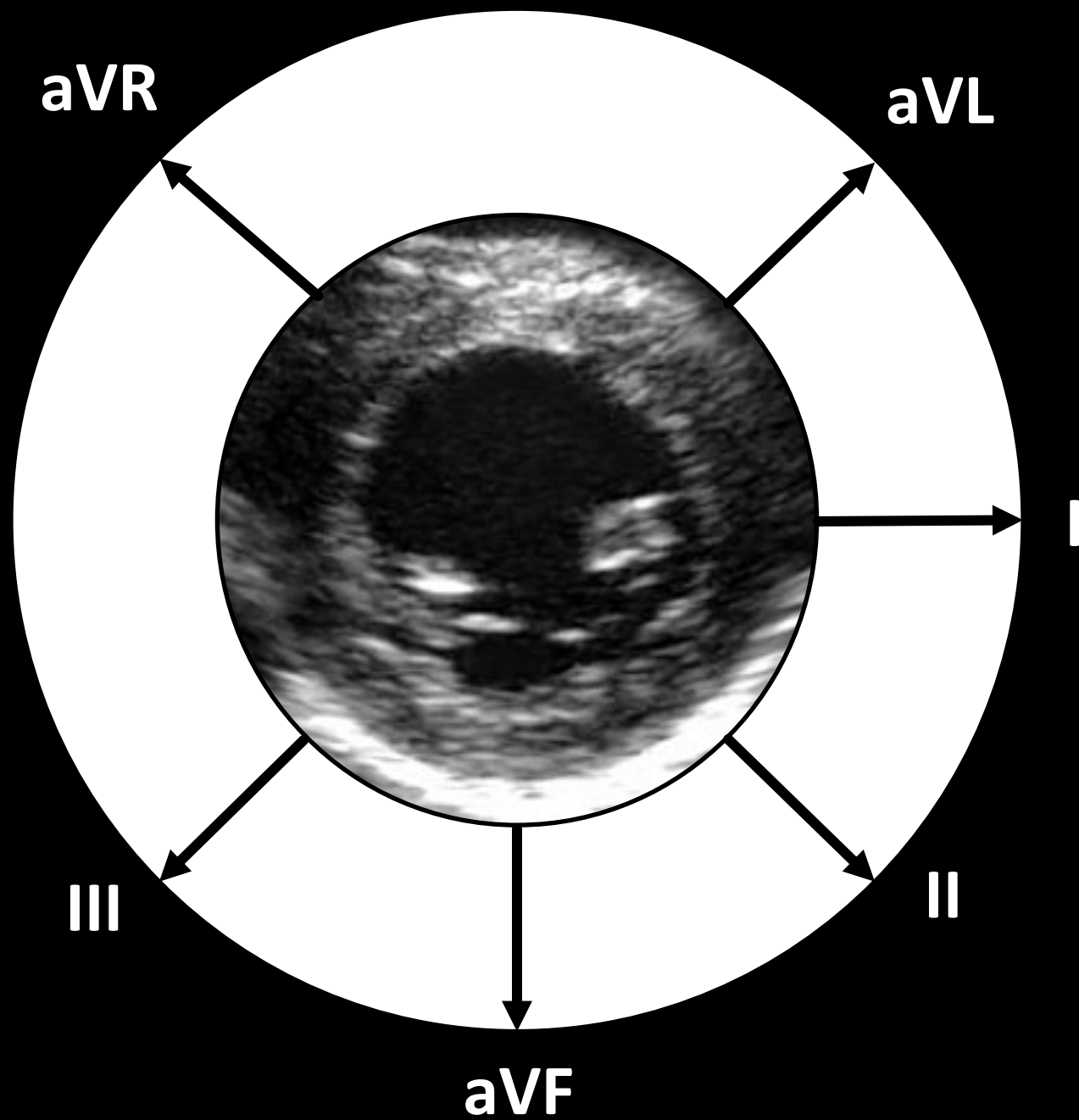




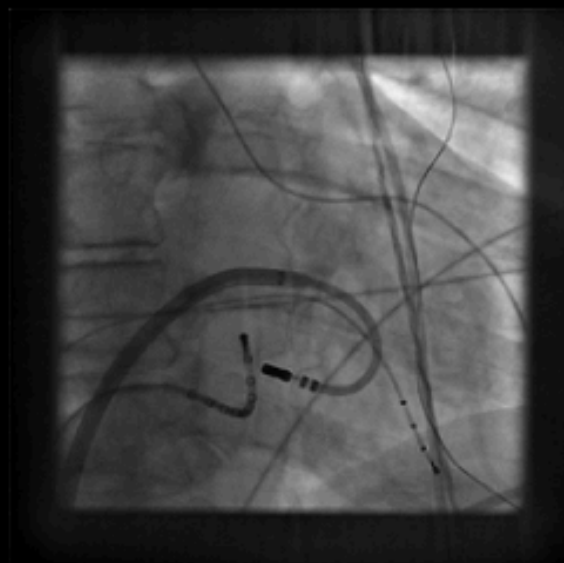
Concealed Entrainment

80J, VWI, EF: 20%, NYHA II

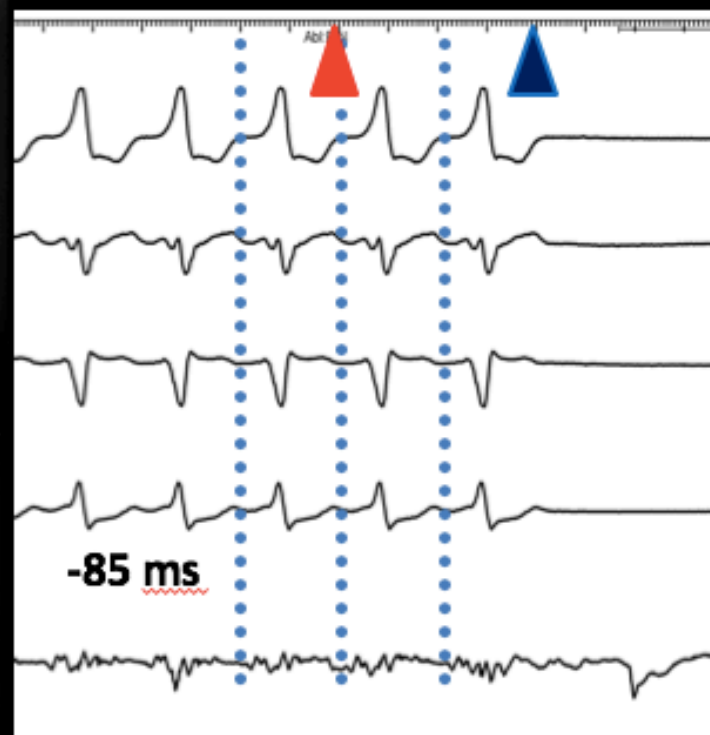
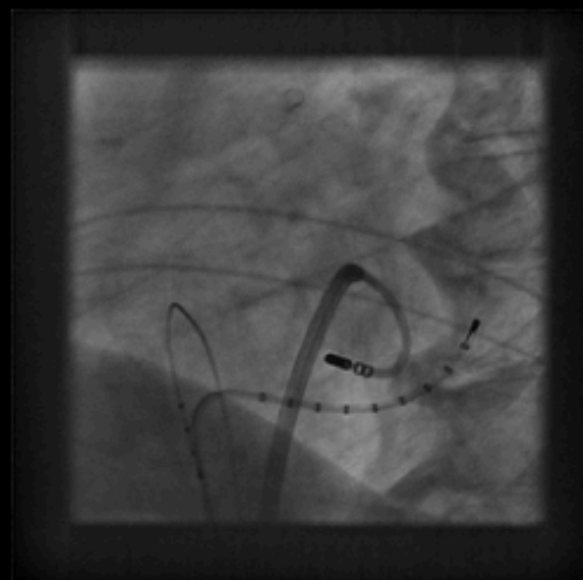




RAO



LAO



I

II

III

aVR

aVL

aVF

V1

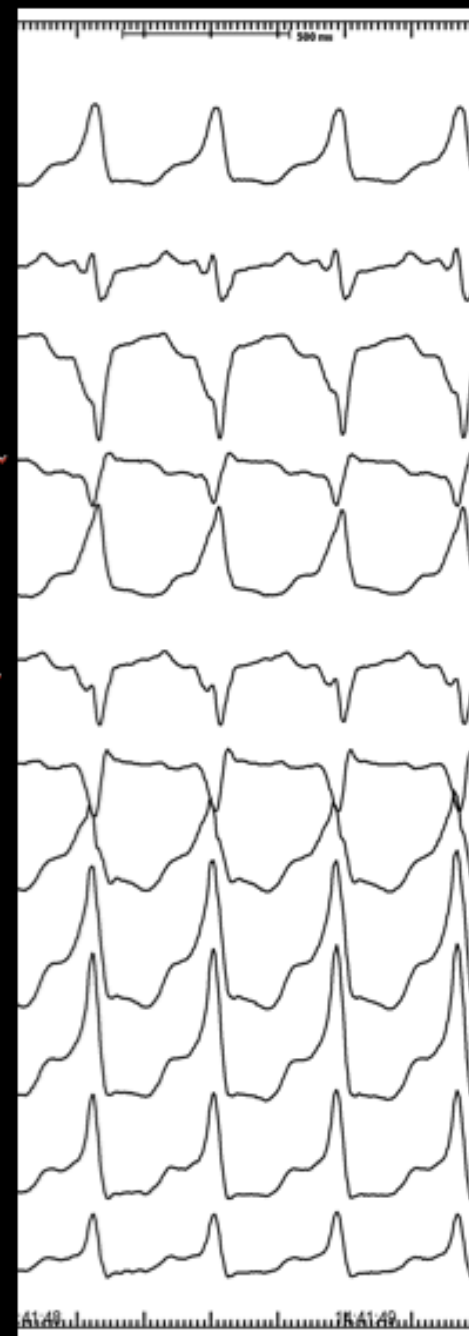
V2

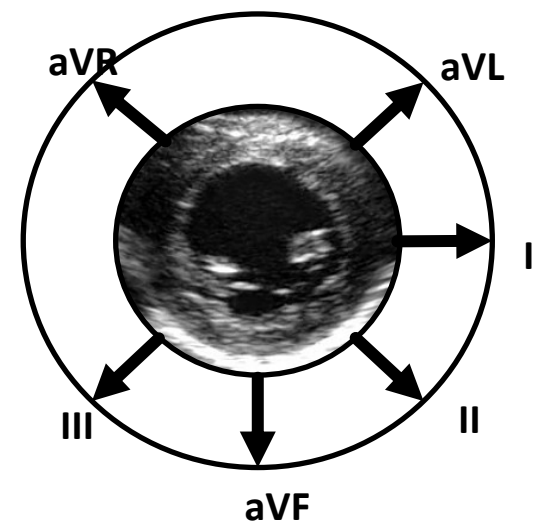
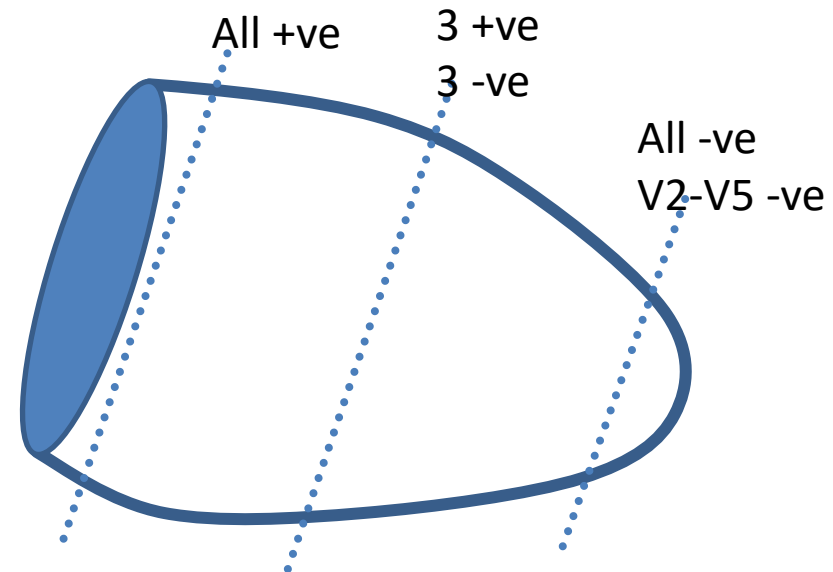
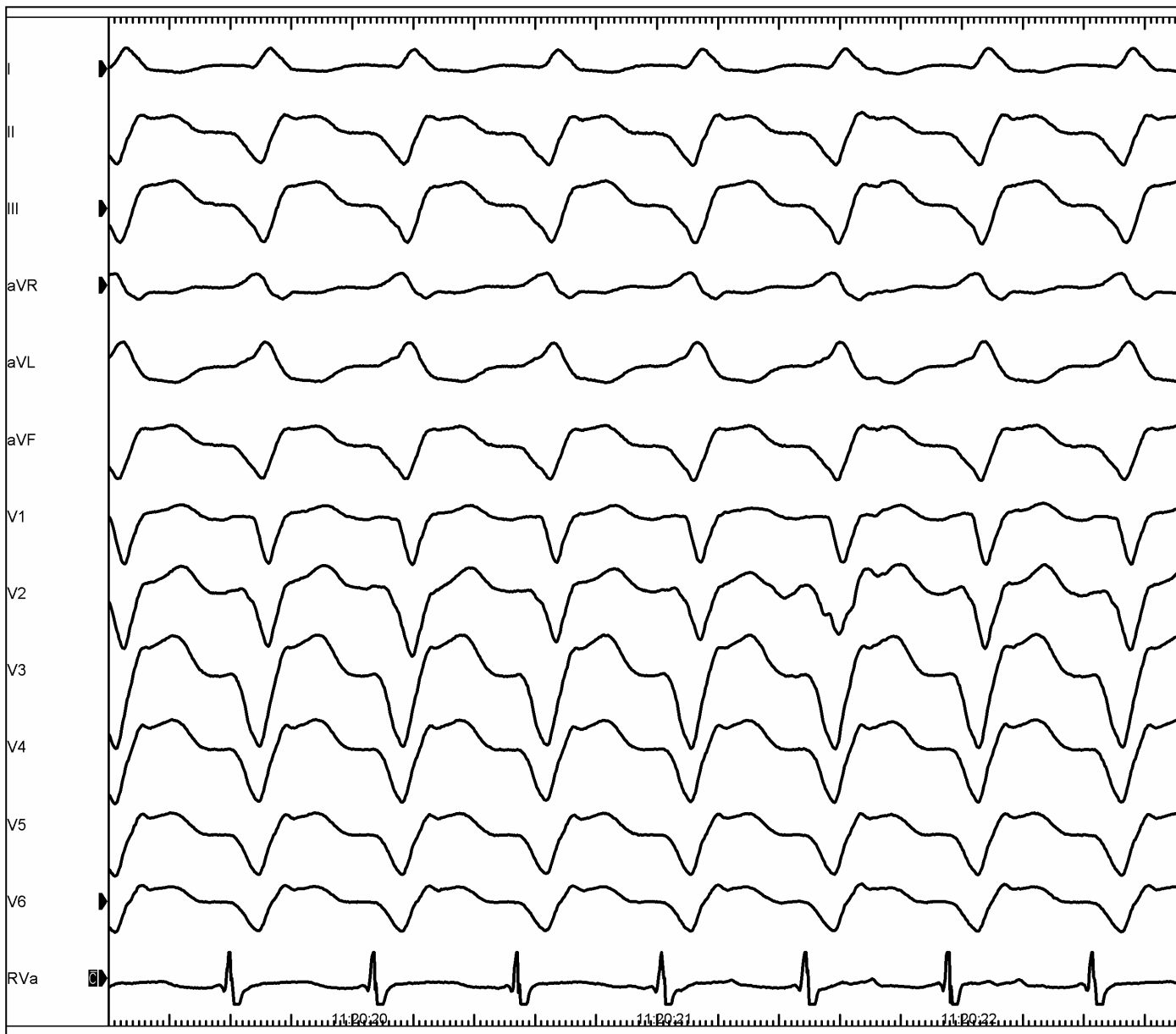
V3

V4

V5

V6

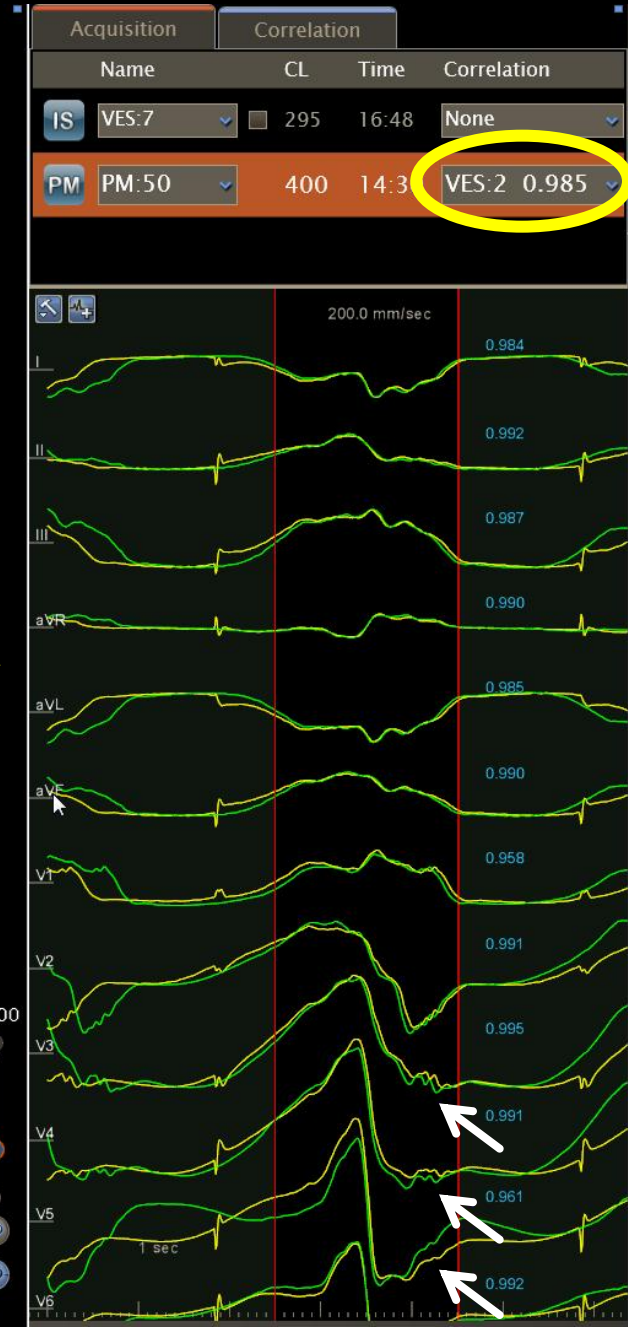
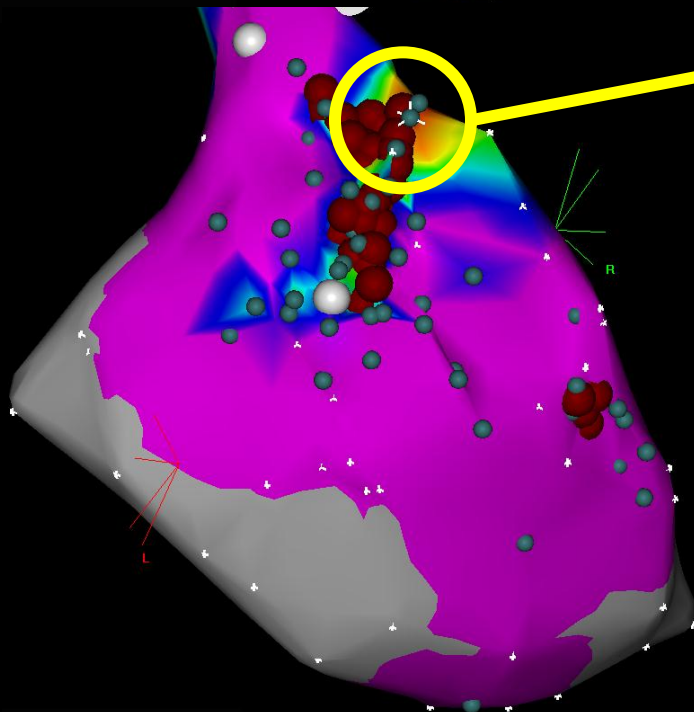


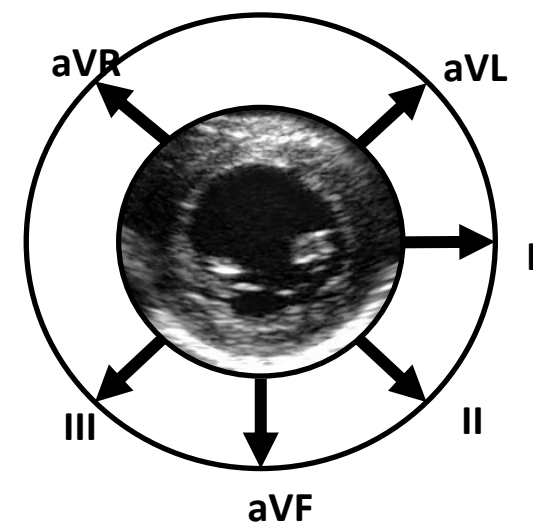
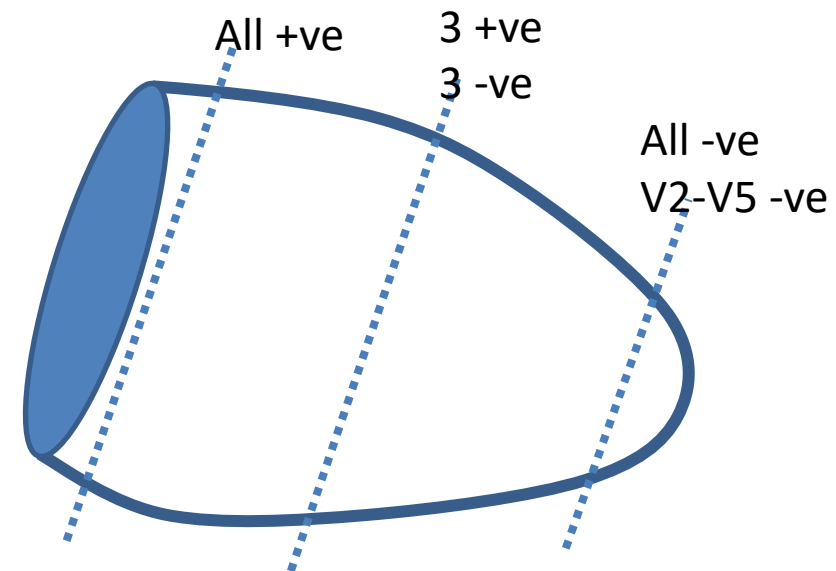
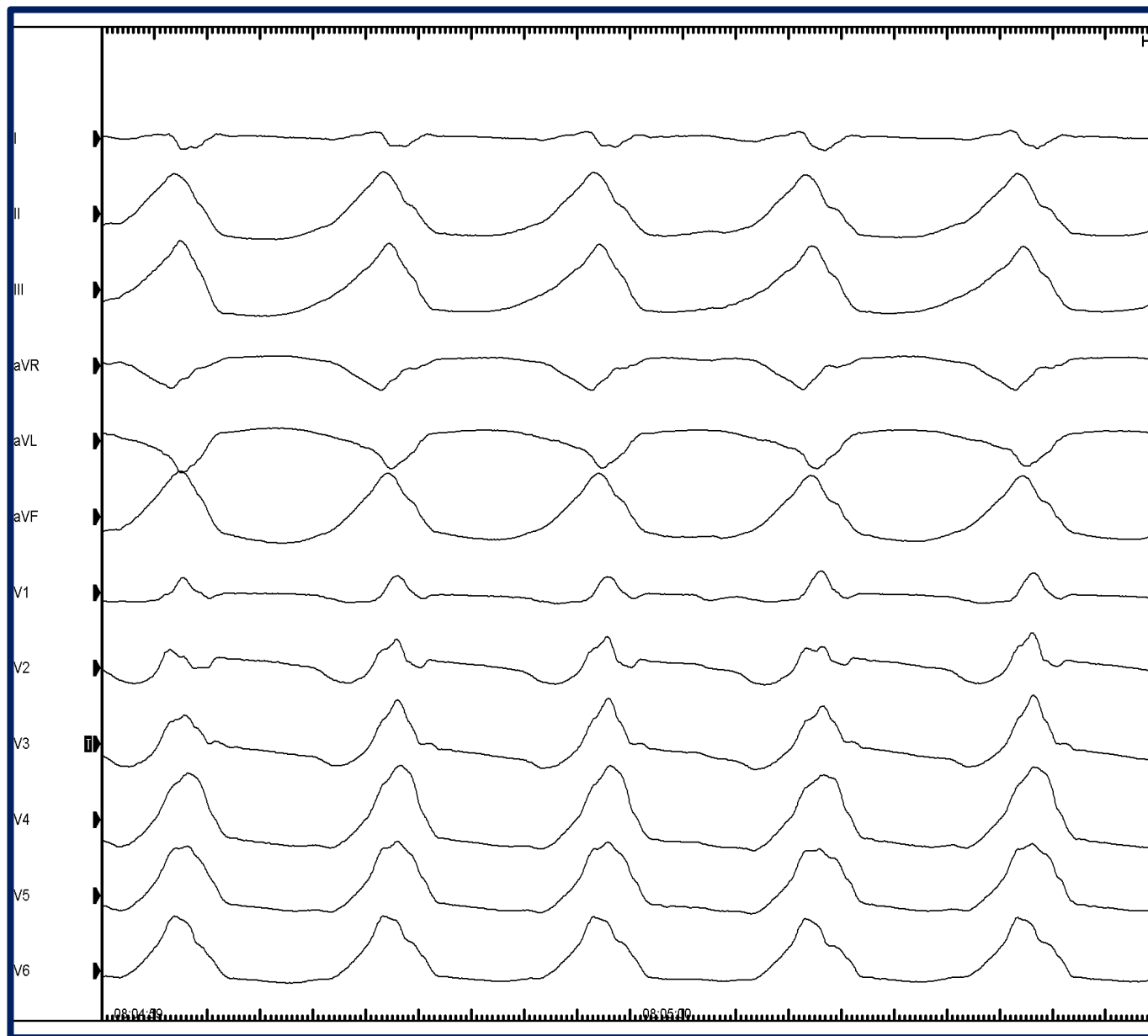


Substrate Mapping



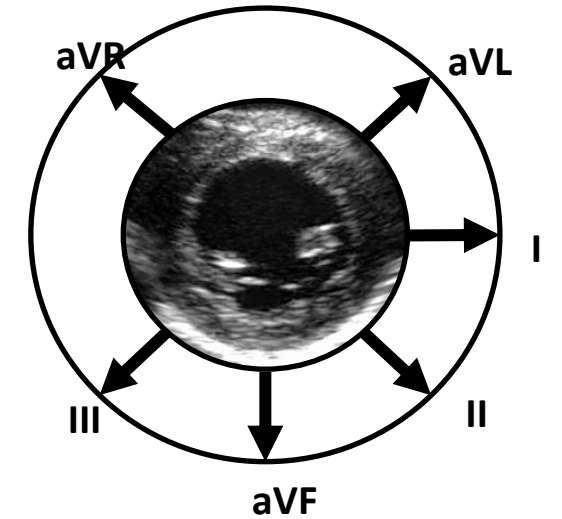
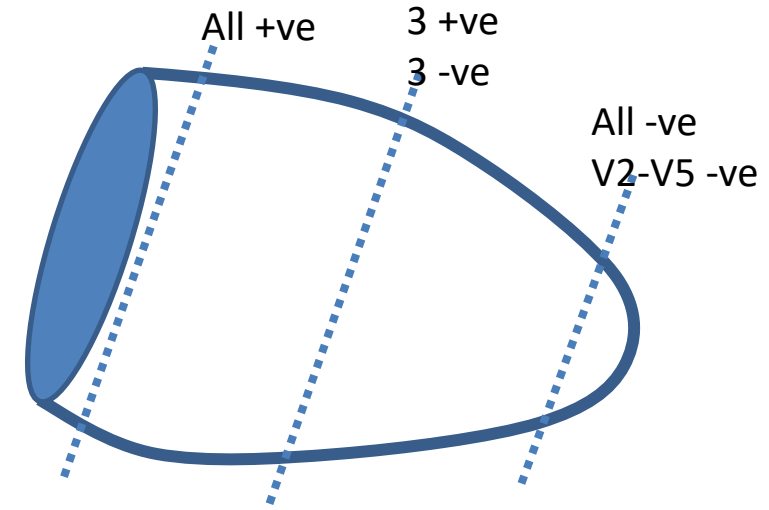
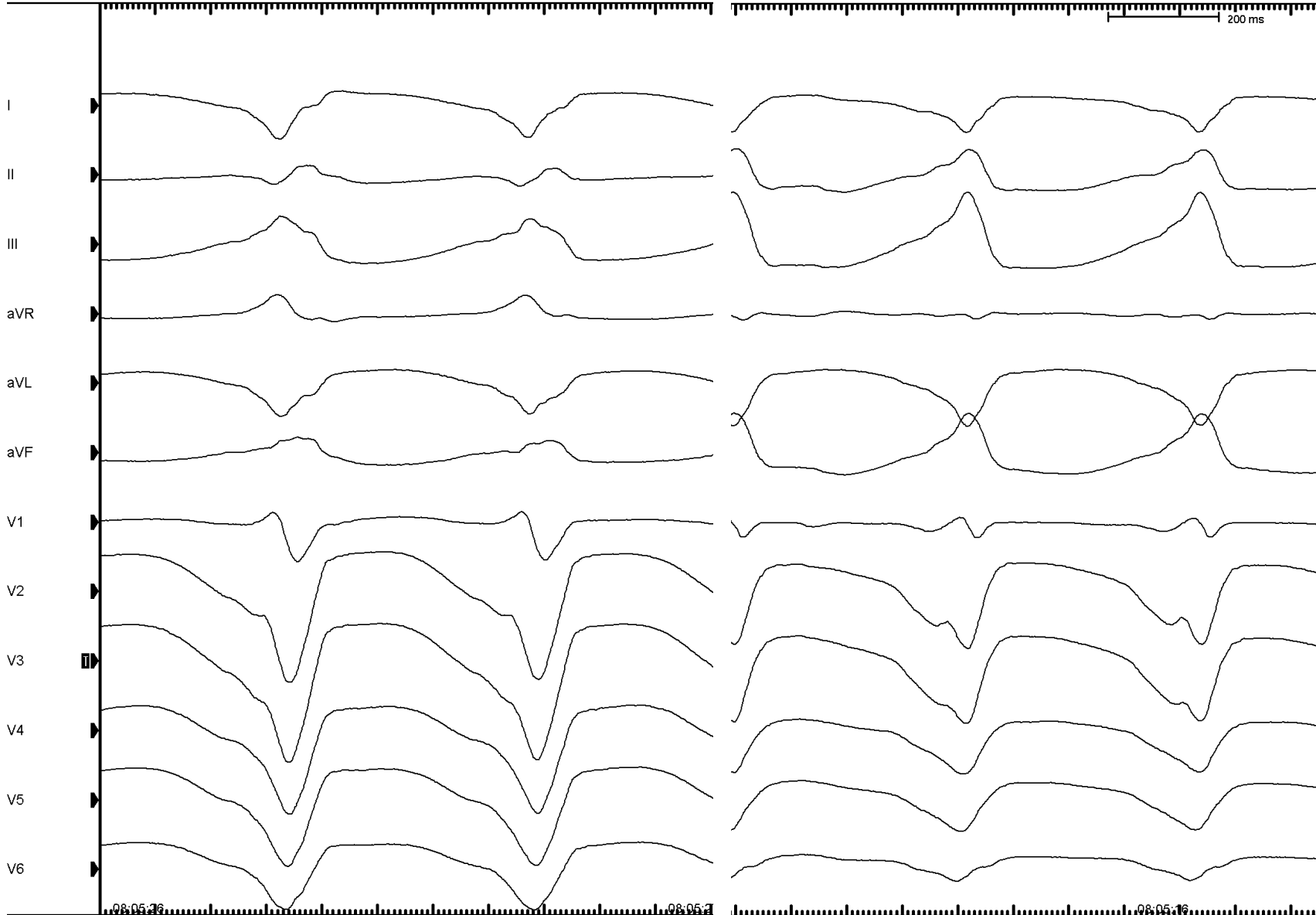
PM Correlation Mapping

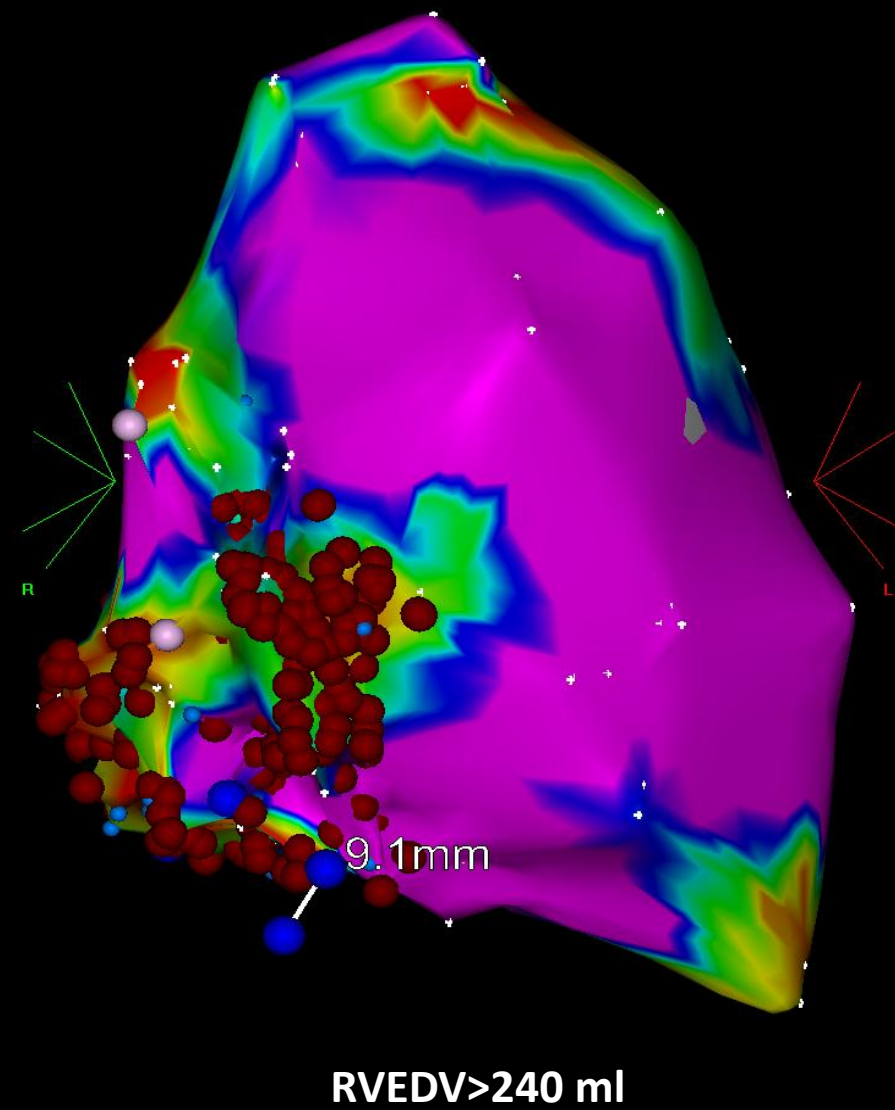
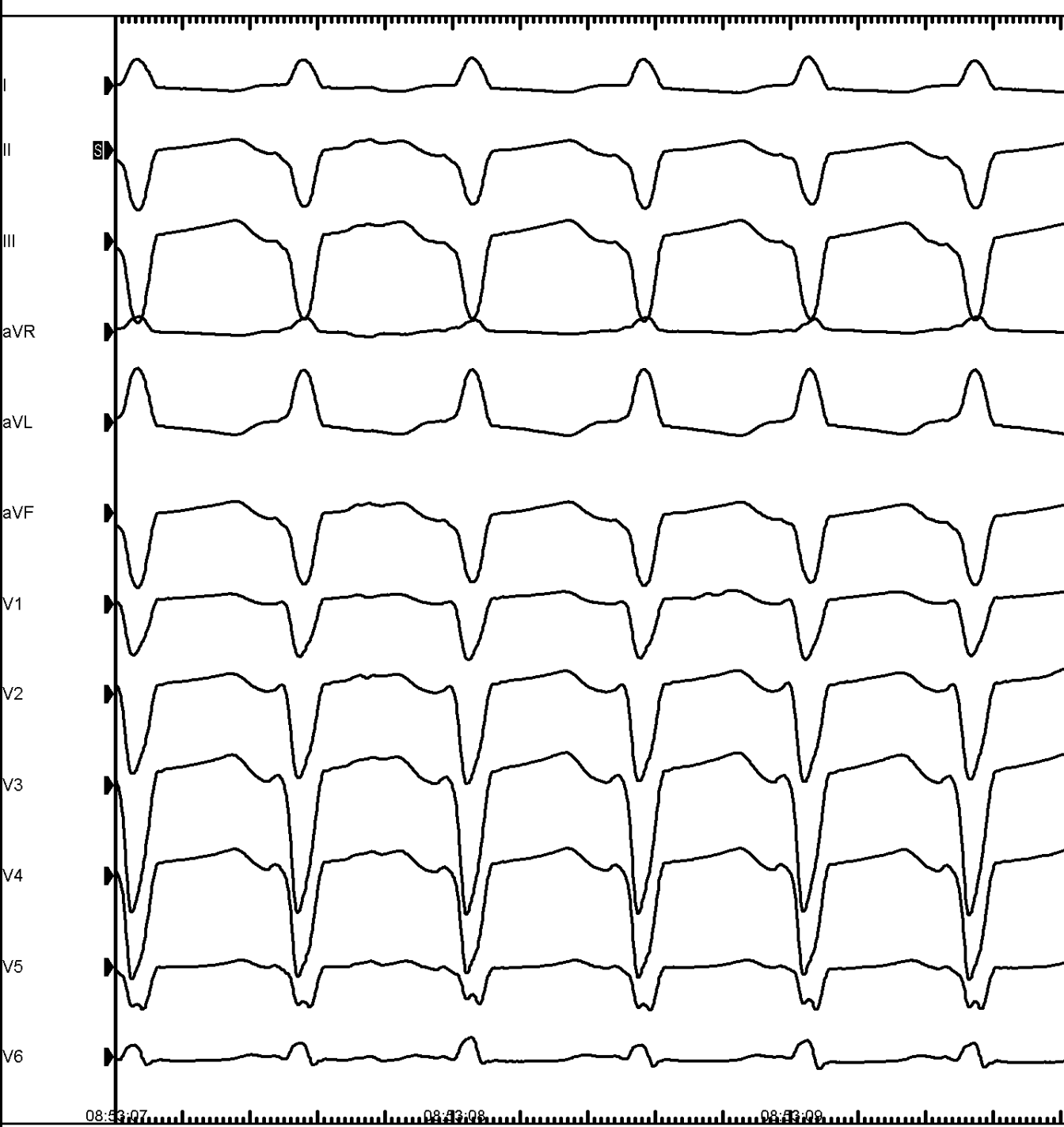


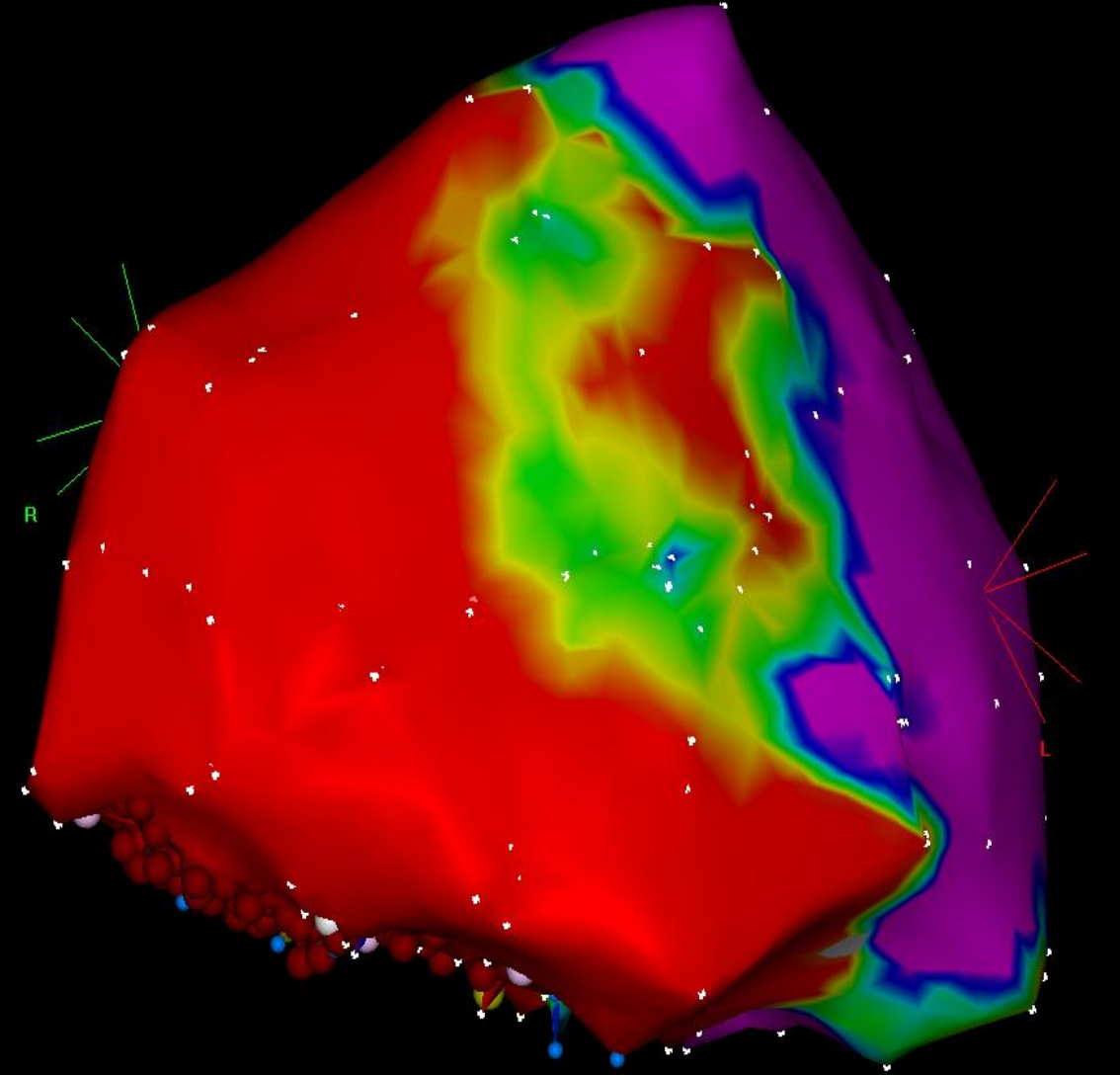
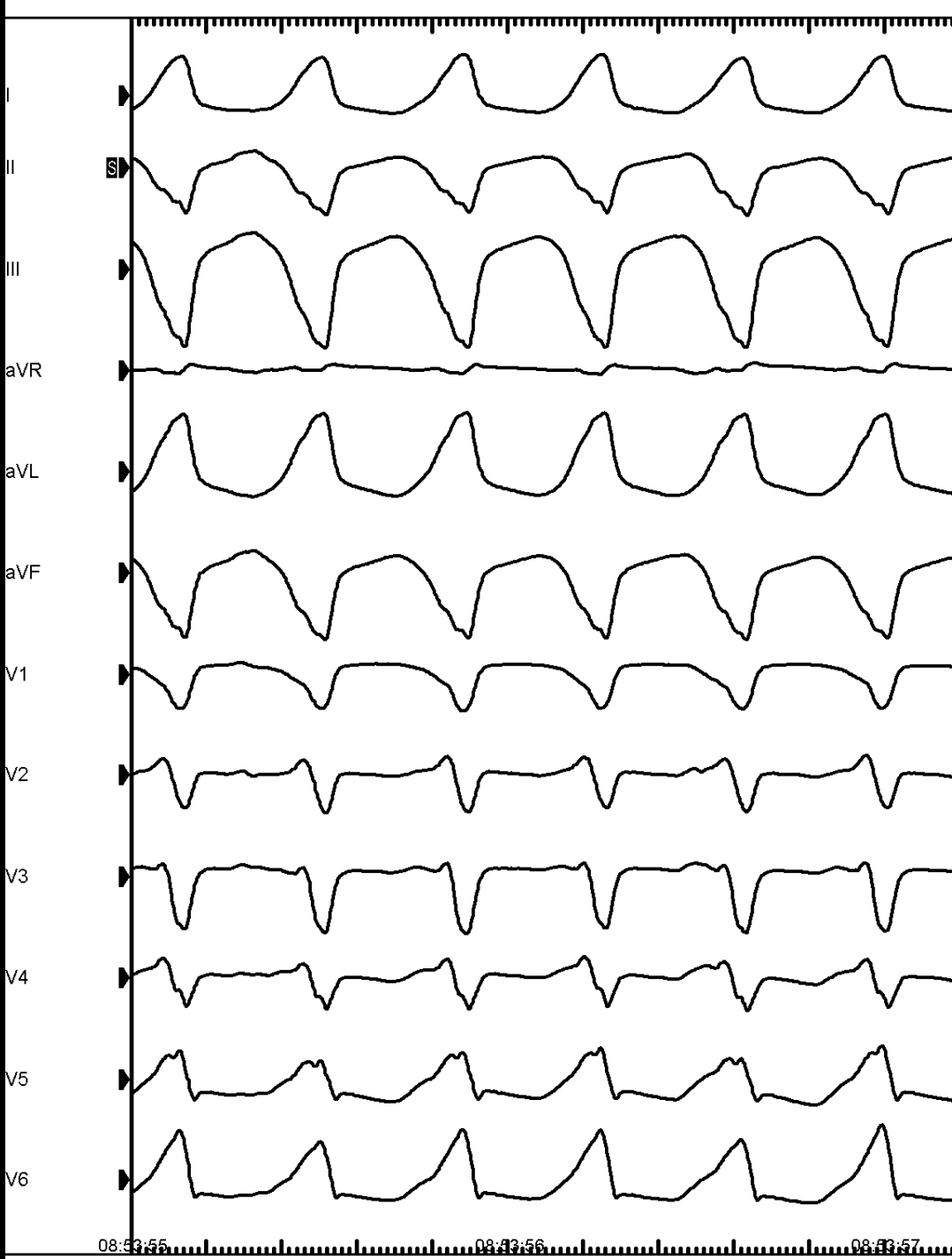


VT1

VT2



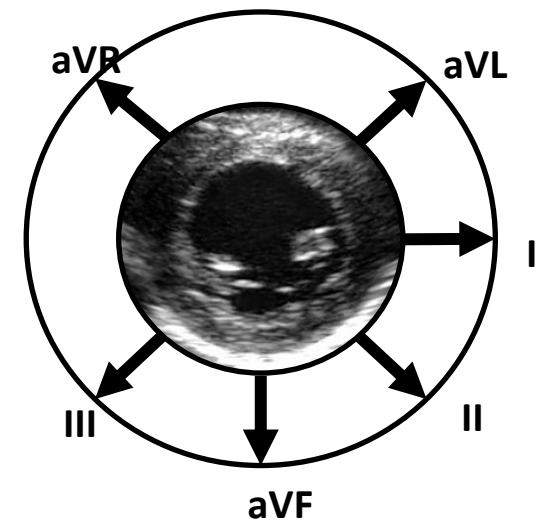
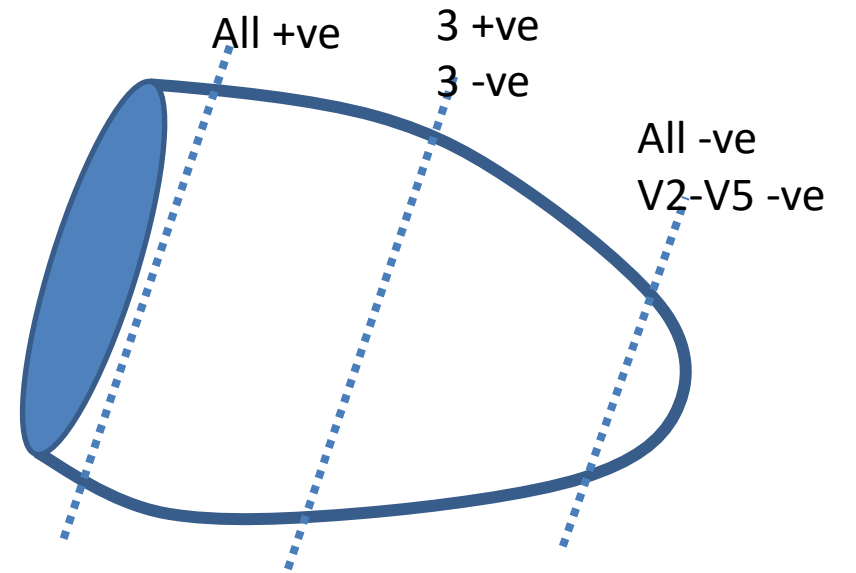
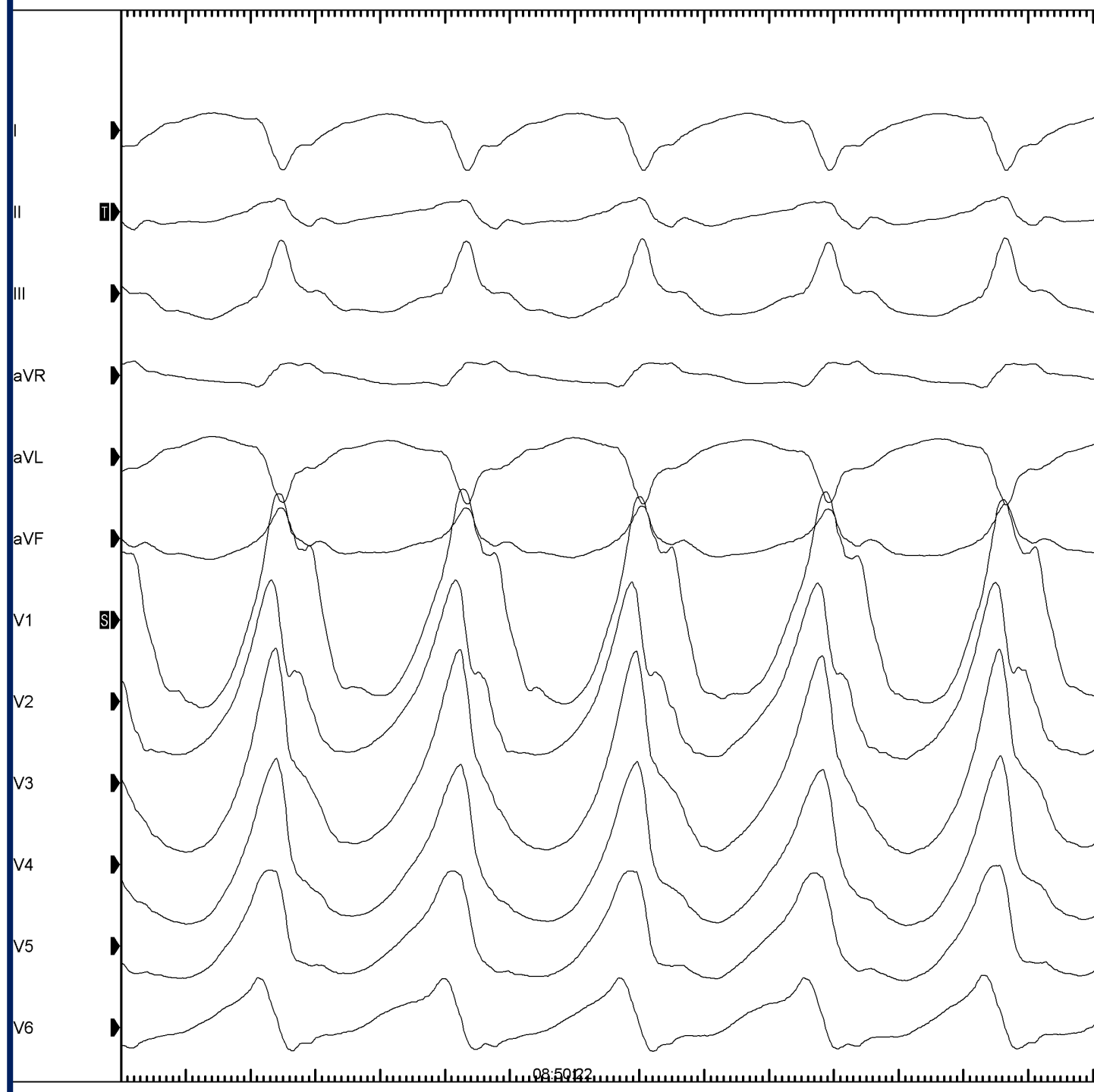




54 years old male patient with palpitation and no syncope were referred to our center for VT ablation

MRT: no scar, LVEF: 54%

CA: Normal coronary arteries



Setup
HW Study Loc. Cath. Map

Mapping

Ablation

PaSo



IS



1-Arash (220, 0)

0.50 mV Bi 1.50 mV

Acquisition

Correlation

PM/IS Correlation Table

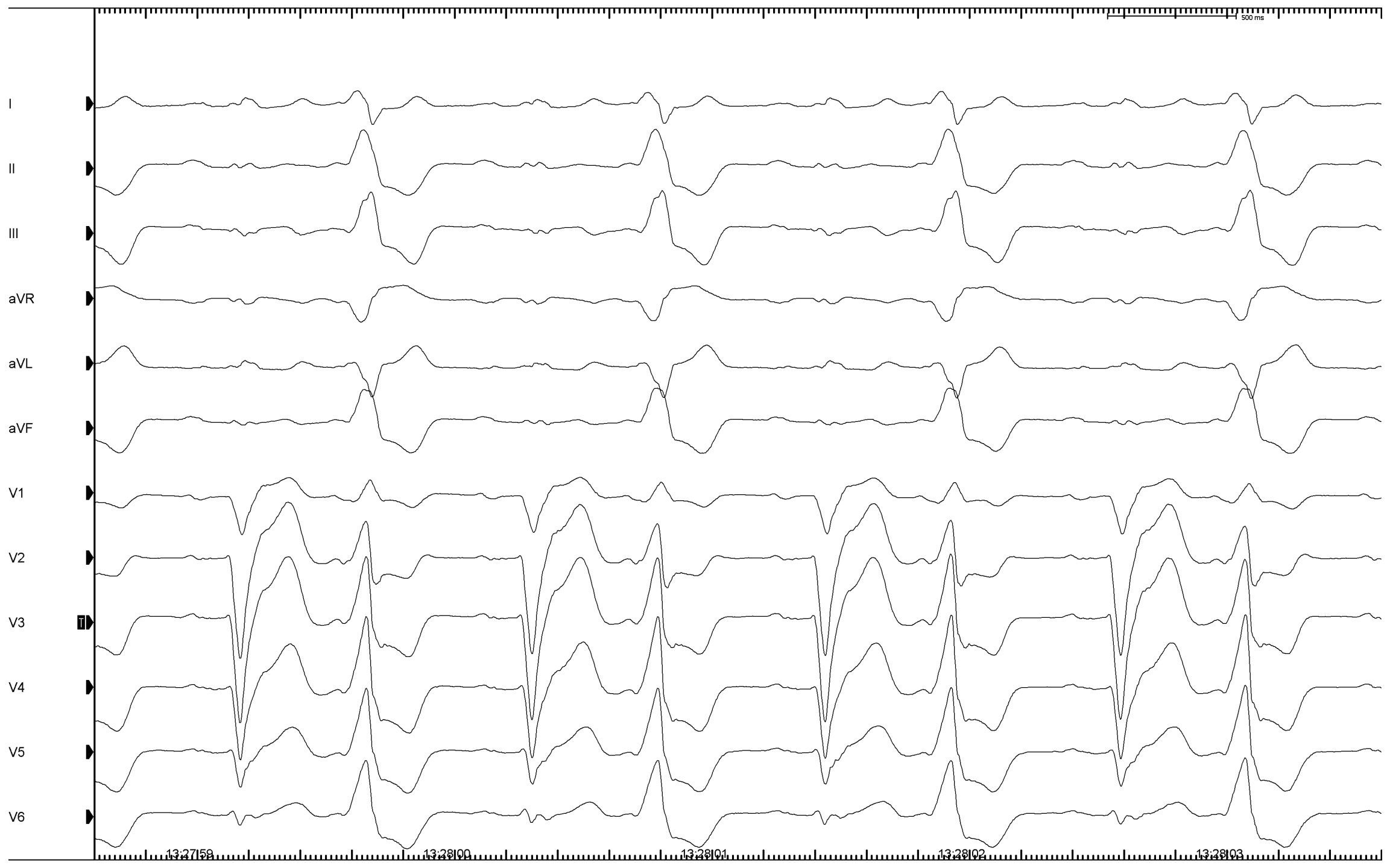
#	PM Name	VTkl:9	VTkb:11
149	PM:38	0.467	0.721
150	PM:39	0.611	0.763
151	PM:40	0.287	0.967
153	PM:41	0.696	0.942

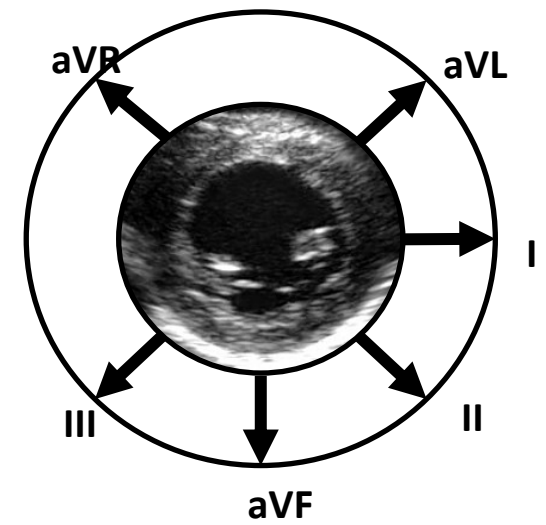
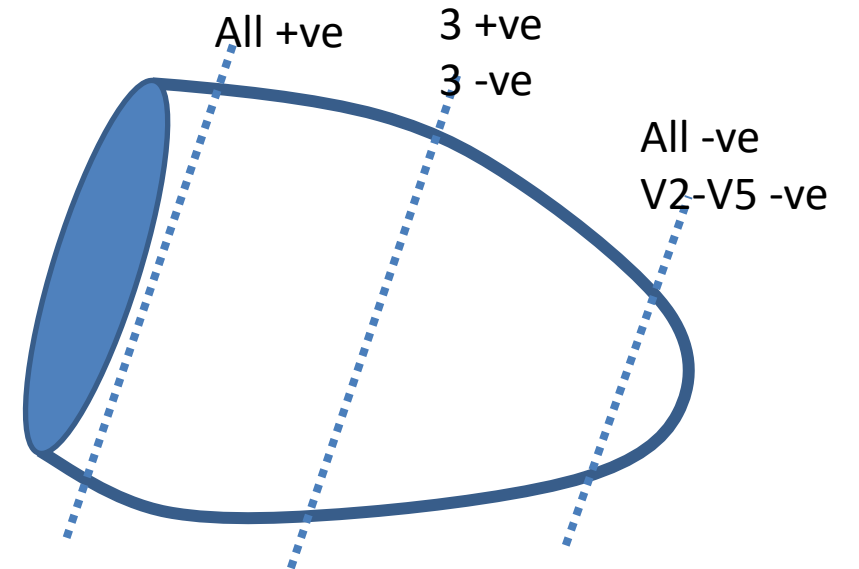
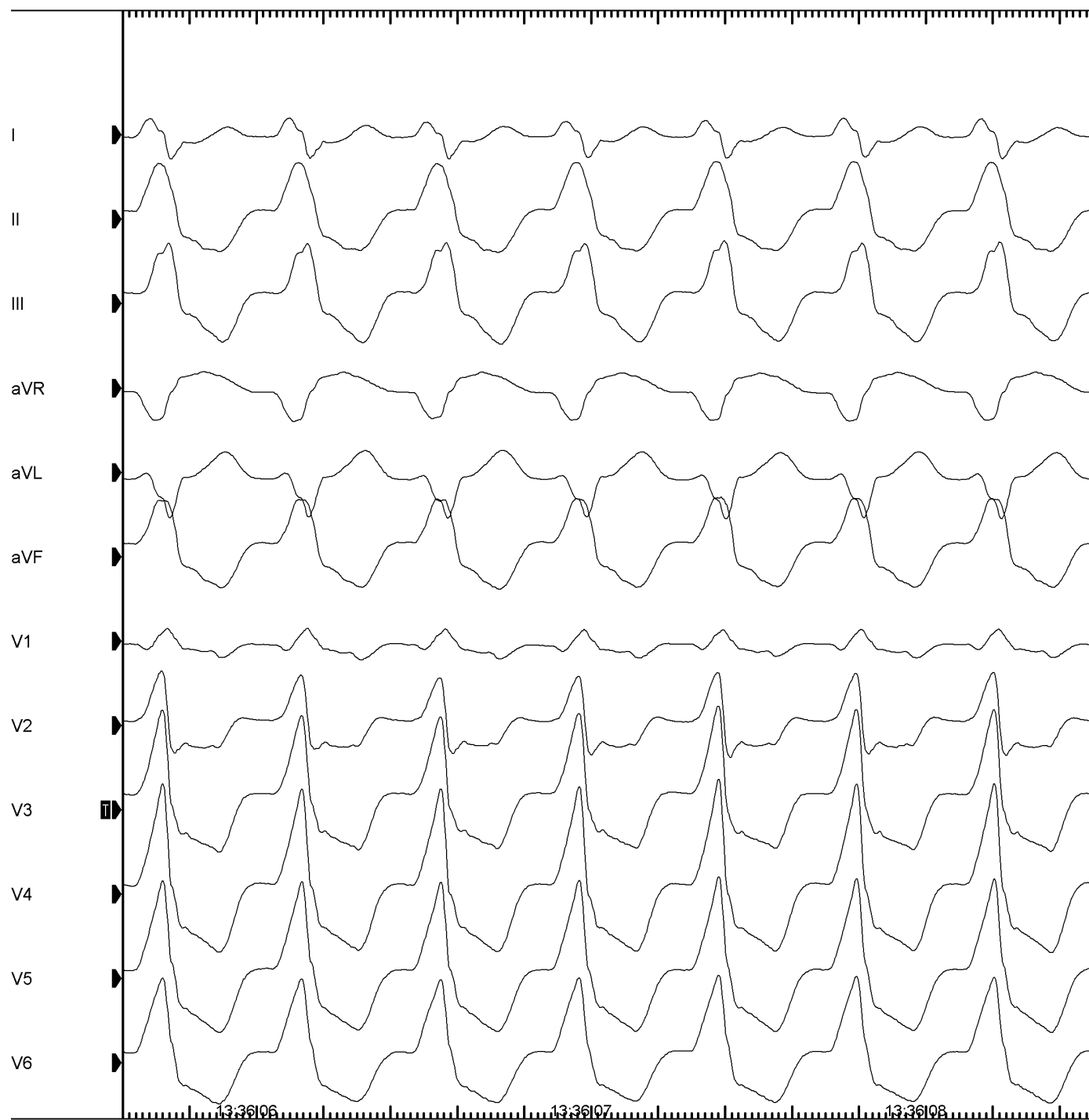


Acquire

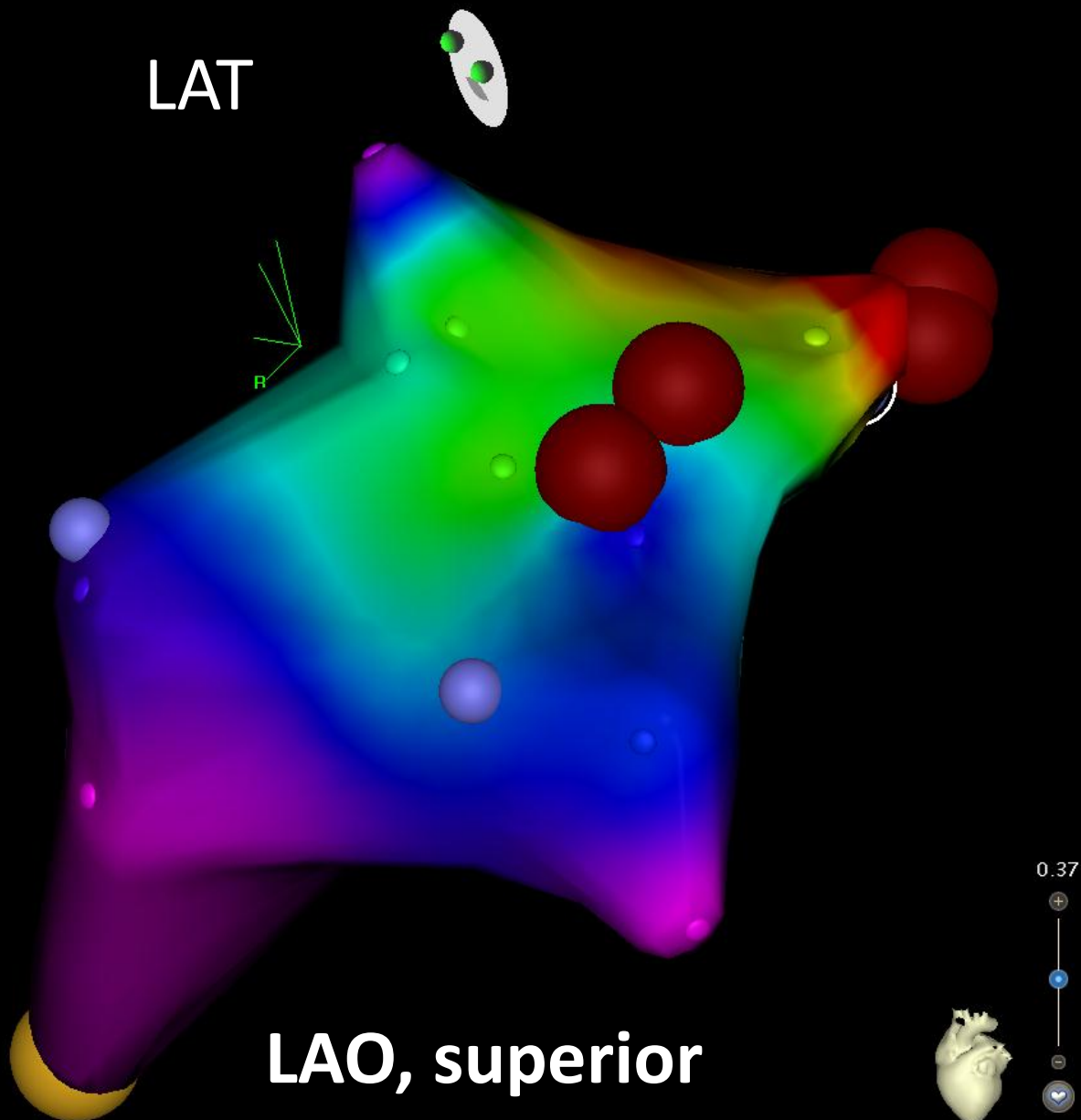
CL LAT Bi Imp

AP PA LAO RAO LL RL INF SUP





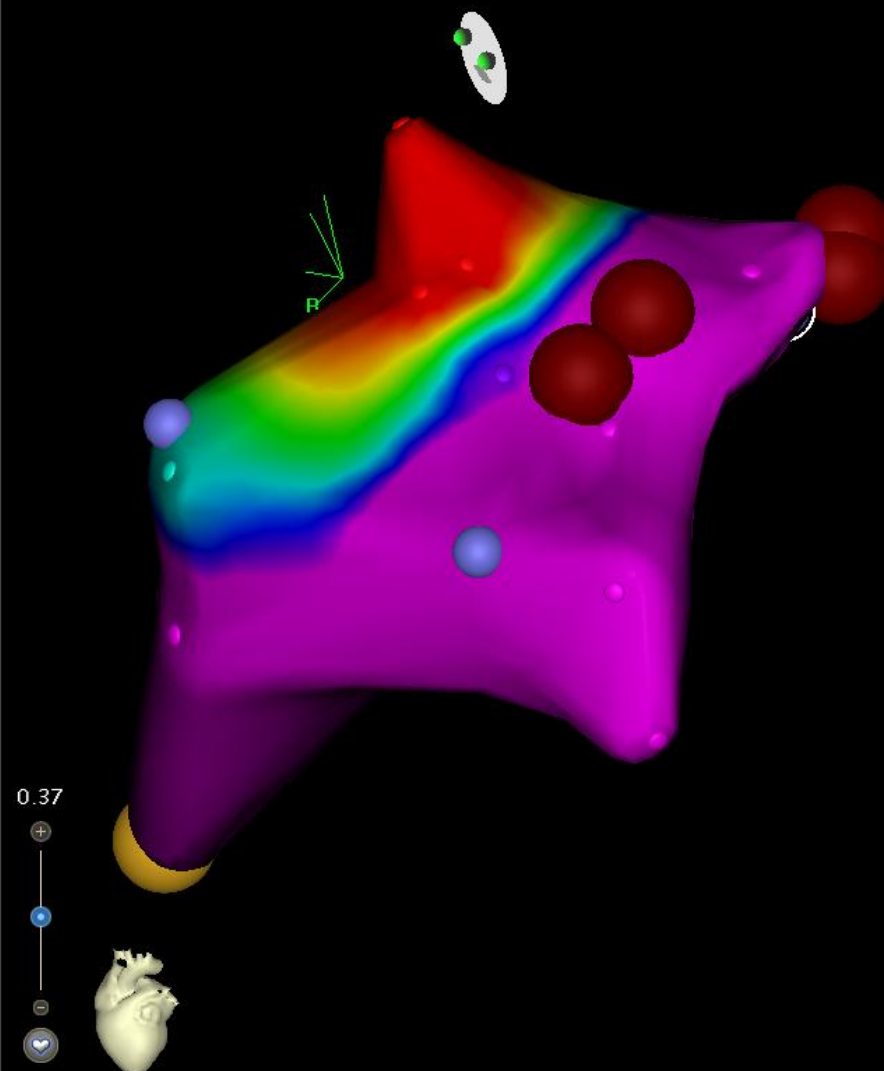
LAT



LAO, superior

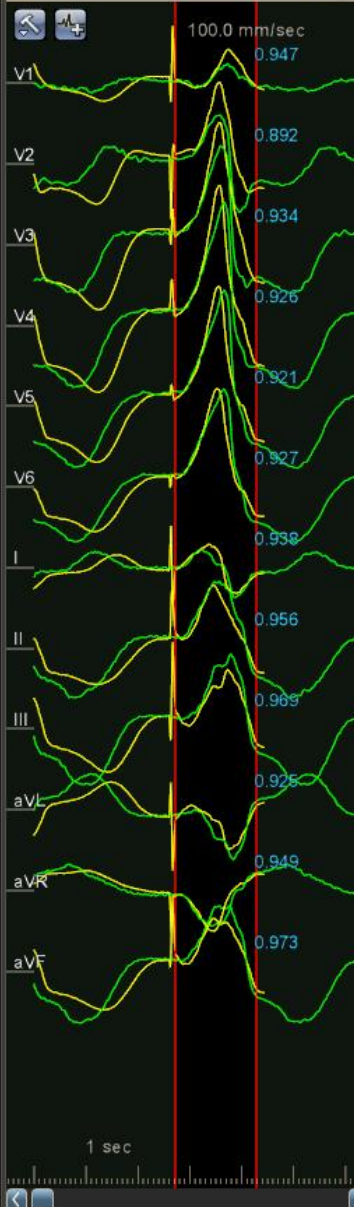
0% AP PA LAO RAO LL RL INF SUP

Bipolar

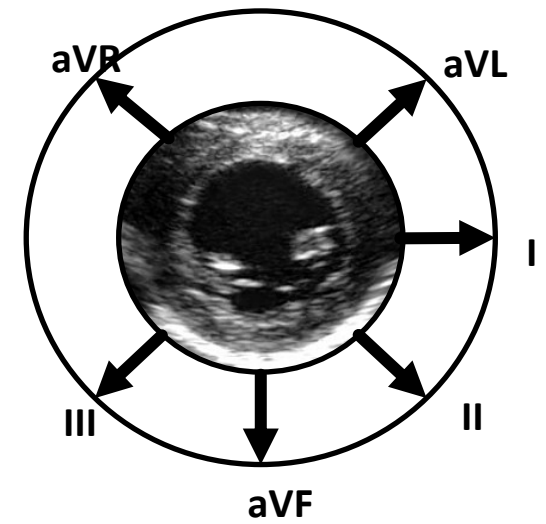
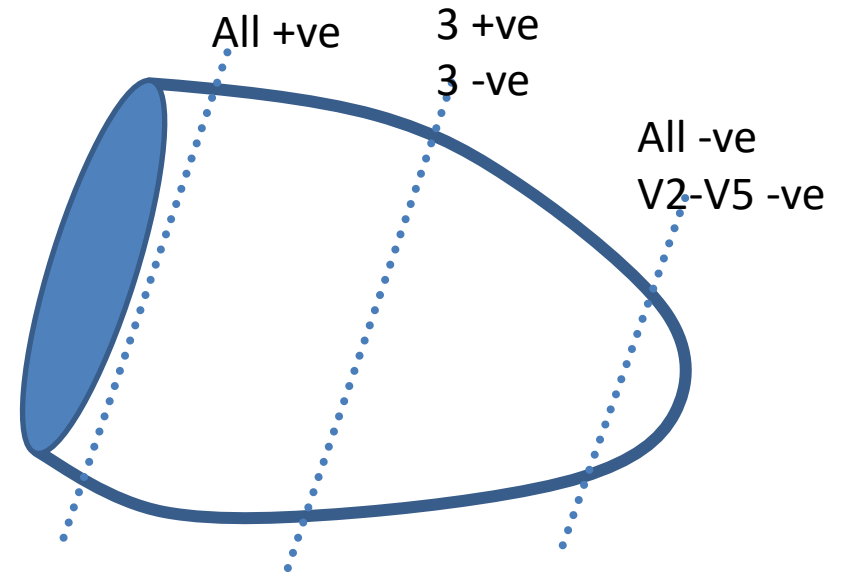
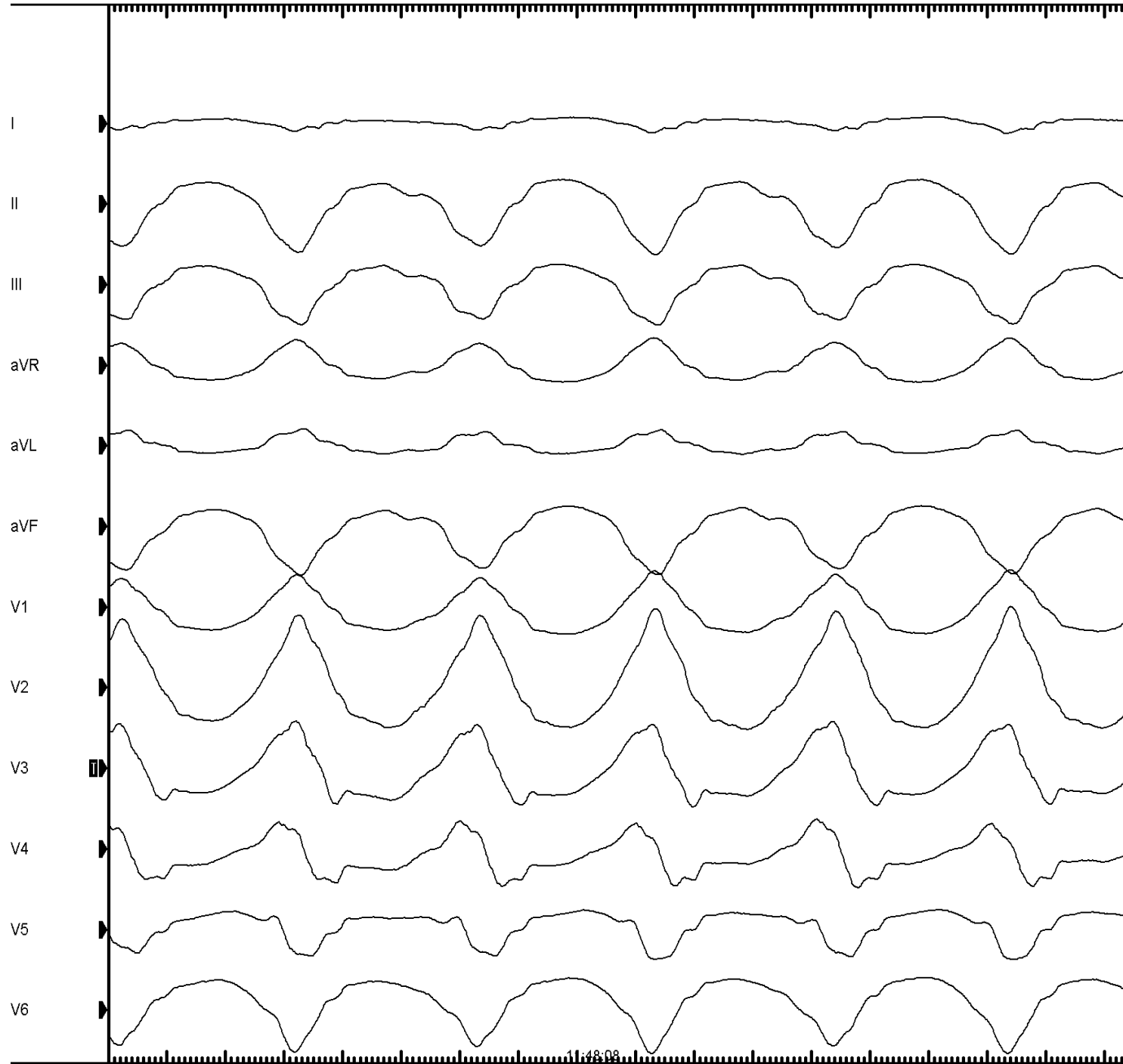


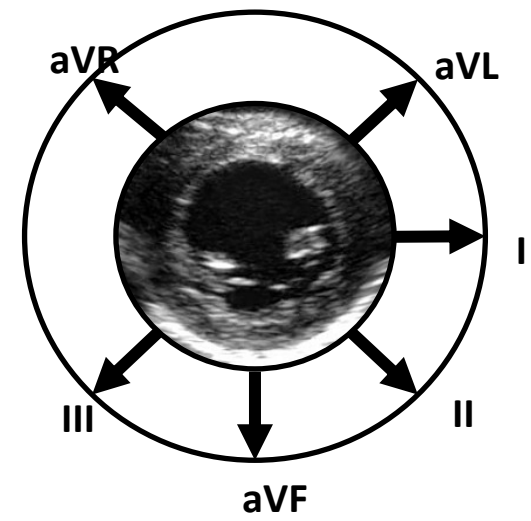
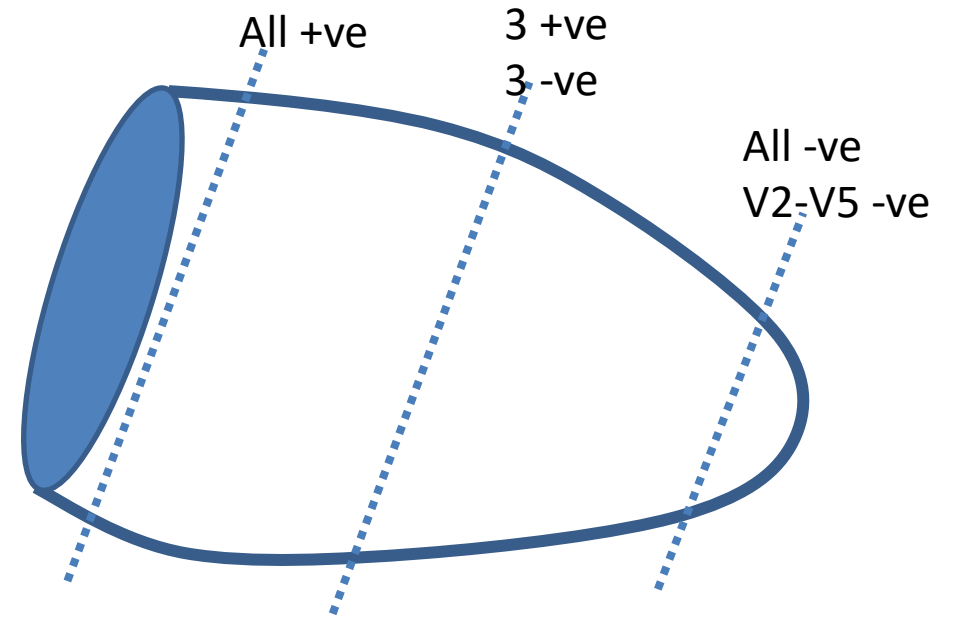
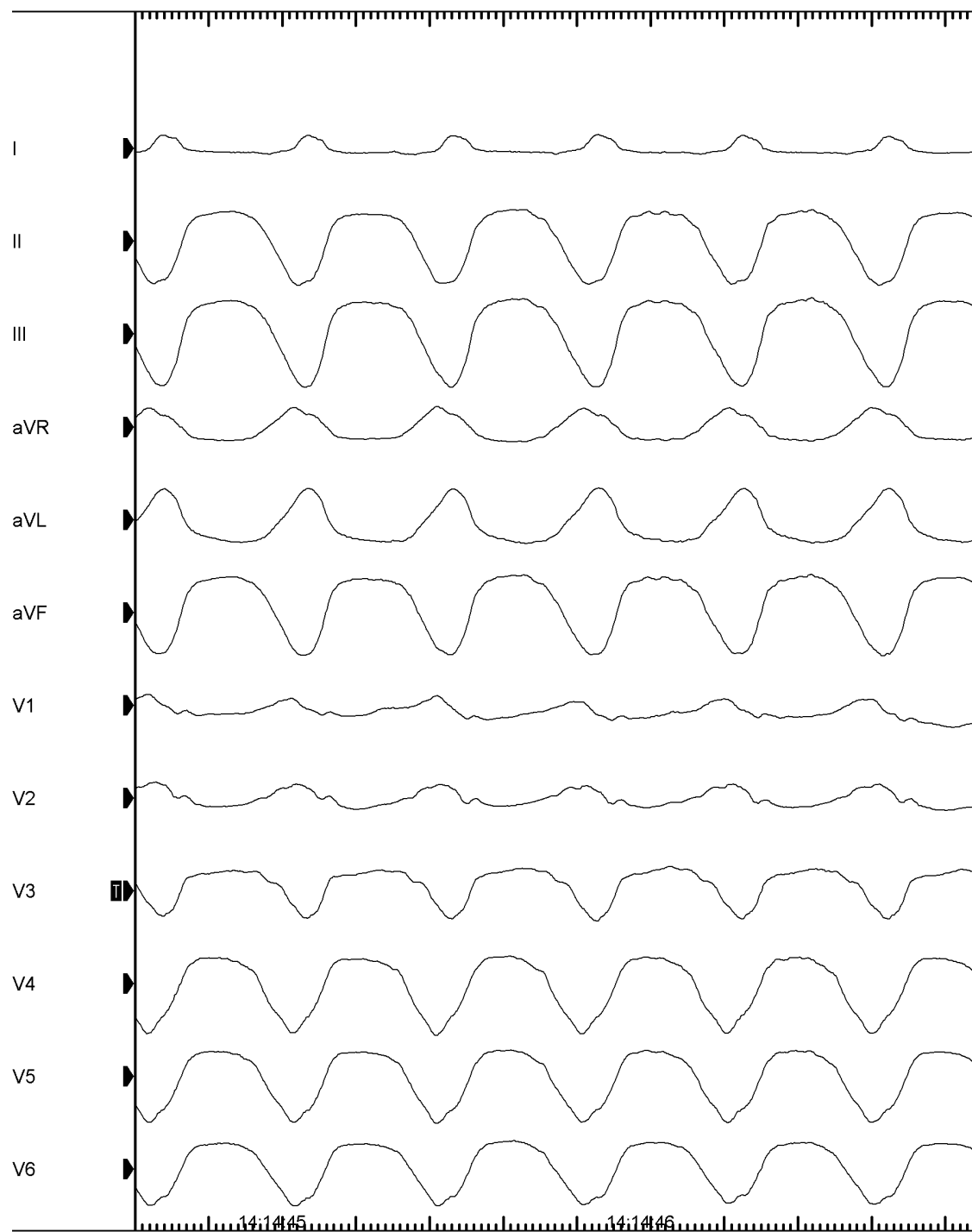
0% AP PA LAO RAO LL RL INF SUP

#	PM Name	VT:1
14	PM:1	0.775
22	PM:3	0.695
23	PM:4	0.938



Sync





The future of ECG: Man versus Machine

The future of ECG

Cardiologist-level arrhythmia detection and classification in ambulatory electrocardiograms using a deep neural network

Awni Y. Hannun^{1,6*}, Pranav Rajpurkar^{1,6}, Masoumeh Haghpanahi^{2,6}, Geoffrey H. Tison^{3,6},
Codie Bourn², Mintu P. Turakhia^{4,5} and Andrew Y. Ng¹

Nature Medicine | VOL 25 | JANUARY 2019 | 65–69 | www.nature.com/naturemedicine

91,232 single-lead ECGs from 53,549 patients who used a single-lead ambulatory ECG monitoring device.

ECG data were recorded by the Zio monitor, which is a Food and Drug Administration (FDA)-cleared, single-lead, patch-based ambulatory ECG monitor that continuously records data from a single vector (modified Lead II) at 200 Hz.

The mean and median wear time of the Zio monitor in our dataset was 10.6 and 13.0 days, respectively.

Table 2 | DNN algorithm and cardiologist sensitivity compared to the cardiologist committee consensus, with specificity fixed at the average specificity level achieved by cardiologists

	Specificity	Average cardiologist sensitivity	DNN algorithm sensitivity
Atrial fibrillation and flutter	0.941	0.710	0.861
AVB	0.981	0.731	0.858
Bigeminy	0.996	0.829	0.921
EAR	0.993	0.380	0.445
IVR	0.991	0.611	0.867
Junctional rhythm	0.984	0.634	0.729
Noise	0.983	0.749	0.803
Sinus rhythm	0.859	0.901	0.950
SVT	0.983	0.408	0.487
Ventricular tachycardia	0.996	0.652	0.702
Wenckebach	0.986	0.541	0.651

The future of ECG

Screening for cardiac contractile dysfunction using an artificial intelligence-enabled electrocardiogram

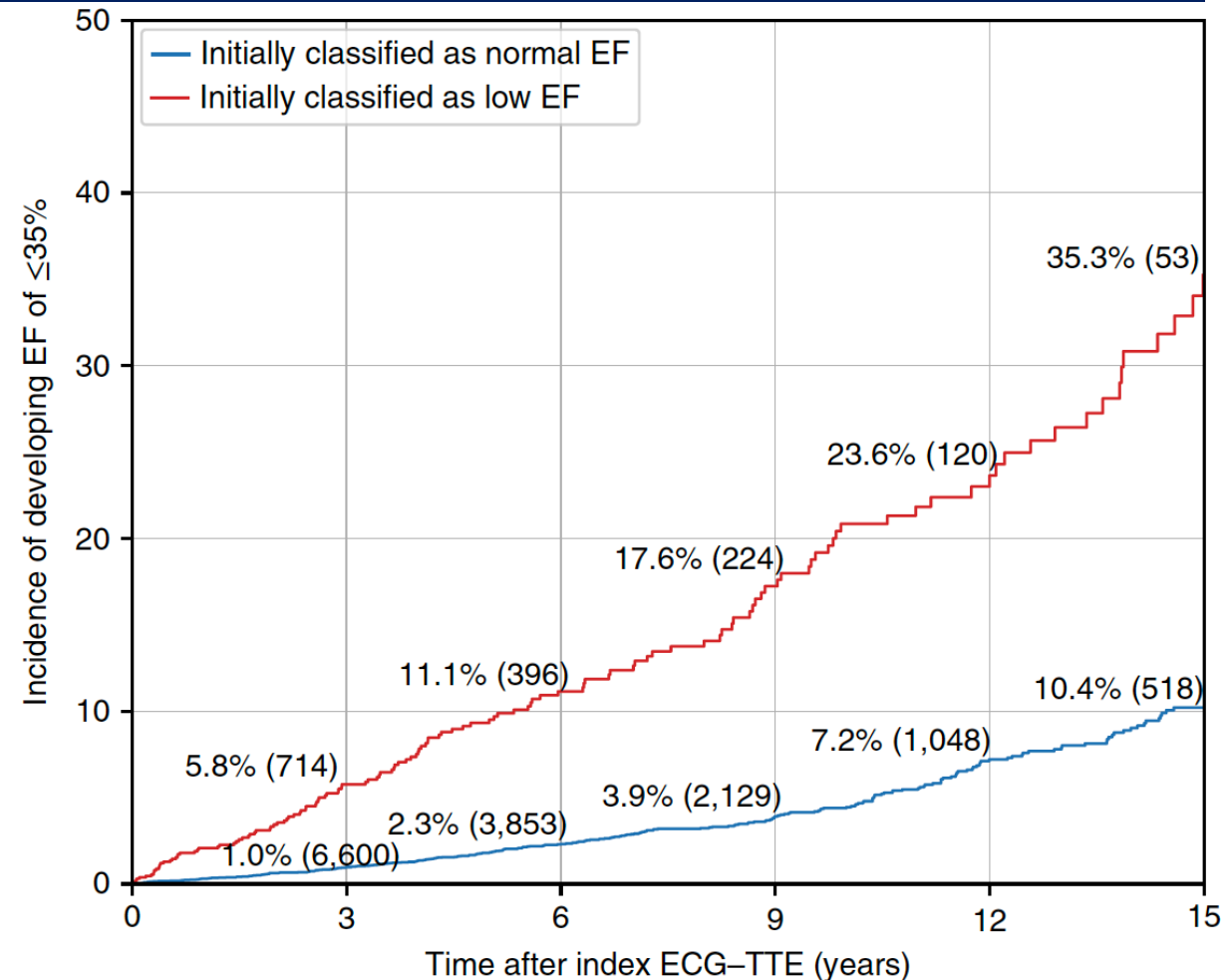
Zachil I. Attia¹, Suraj Kapa¹, Francisco Lopez-Jimenez¹, Paul M. McKie¹, Dorothy J. Ladewig², Gaurav Satam², Patricia A. Pellikka¹, Maurice Enriquez-Sarano¹, Peter A. Noseworthy¹, Thomas M. Munger¹, Samuel J. Asirvatham¹, Christopher G. Scott³, Rickey E. Carter⁴ and Paul A. Friedman^{1*}

Nature Medicine | VOL 25 | 70 JANUARY 2019 | 70–74 | www.nature.com/naturemedicine

Using paired 12-lead ECG and echocardiogram data, including the LVEF, from 44,959 patients at the Mayo Clinic, we trained a convolutional neural network to identify patients with ventricular dysfunction, defined as ejection fraction $\leq 35\%$, using the ECG data alone.

When tested on an independent set of 52,870 patients, the network model yielded values for the area under the curve, sensitivity, specificity, and accuracy of 0.93, 86.3%, 85.7%, and 85.7%, respectively.

In patients without ventricular dysfunction, those with a positive AI screen were at 4 times the risk (hazard ratio, 4.1; 95% confidence interval, 3.3 to 5.0) of developing future ventricular dysfunction compared with those with a negative screen.



Summary



Use of the 12-lead ECG recorded during VT to regionalize its origin was first described by Josephson in 1981.

12-Lead-ECG is a simple ,useful and reliable tool to localize and diagnose the ventricular arrhythmia.

It makes more sense to divide it into no more than 10– 12 approximately equal segments when localizing a region of interest using the 12-lead ECG of the VT to limit overlapping information.